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Titel der Masterarbeit / Title of the Master's Thesis

„Assessing protein-metal-binding using ‘accurate constant via transient incomplete separation’ (ACTIS)“

verfasst von / submitted by

Zorica Eric, BSc

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This work was performed at the Institute of Analytical Chemistry at BOKU in the group of Prof. Stephan Hann, from March to November 2023, under the guidance of Dr. Sven Kochmann and Dr. Anastasiya Tschaikovsky. I want to thank them for guiding me, offering valuable support, and providing helpful feedback throughout my research.

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Abstract (English)

The assessment of biomolecular interactions is one of the main aspects of bioanalytics. All established methods for assessment of protein-compound (PC) binding have inherent sources of inaccuracy. This results in multiple values for the dissociation constant (K_d) differing in few orders of magnitude determined for same model system. Accurate constant via transient incomplete separation (ACTIS) is a recently introduced method, theoretically free from inherent sources of inaccuracy. This method is based on a deterministic process of transient incomplete separation (TIS). The difference in transverse diffusion of free C and PC is the basic for the TIS occurrence. So far ACTIS was only used for assessment of small molecule-protein models. This would be the first protein-metal-binding assessment utilizing ACTIS. To proof our setup, the Humane Serum Albumin (HSA) binding to Fluorescein (FLC) was assessed using ACTIS coupled to fluorescence detector. Furthermore, the compatibility of ACTIS with different detection methods was demonstrated. Our experiments included coupling of ACTIS setup to four different detection methods: fluorescence detection (FLD), time-of-flight mass spectrometry (TOF-MS), inductively coupled plasma mass spectrometry (ICP-MS) and atomic emission spectroscopy (ICP-AES). The binding constant of β -lactoglobulin (BLG) to quercetin-iron (FeQ_2) complex was assessed using ACTIS-TOF-MS. Beside the assessing of K_d , the experiments aiming the improvement of the transient Fe detection with ICP techniques were also conducted. Finally, the impact of the detector configuration, specifically the inner radius of the transfer capillary, was examined *in silico* by employing computer simulations.

Abstract (Deutsch)

Die Bewertung von biomolekularen Interaktionen ist einer der wichtigsten Aspekte der Bioanalytik. Alle etablierten Methoden zur Beurteilung der Bindungsstärke zwischen Protein und einer bindenden Komponente (PC) weisen inhärente Fehlerquellen auf. Dies führt dazu, dass die resultierenden Dissoziationskonstanten (K_d) für dasselbe Modellsystem mehrere Größenordnungen voneinander abweichen. Accurate Constant via Transient Incomplete Separation (ACTIS) ist eine neue Methode zur genauen Bestimmung von K_d , die theoretisch frei von inhärenten Fehlerquellen ist. Diese Methode basiert auf einem deterministischen Prozess der Transient Incomplete Separation (TIS). Die Differenz in der transversalen Diffusion von freiem C und PC ist die Grundlage für das Auftreten von TIS. Bisher wurde ACTIS nur zur Bewertung von Protein-Kleinmolekül-Modellen verwendet. Diese Arbeit stellt den ersten Versuch einer Analyse von Protein-Metall-Bindungen mithilfe von ACTIS dar. Zur Validierung unseres Setups wurde die Bindung von Humanem Serumalbumin (HSA) an Fluorescein (FLC) mithilfe von ACTIS gekoppelt an einem Fluoreszenzdetektor untersucht. Darüber hinaus wurde die Kompatibilität von ACTIS mit verschiedenen Detektionsmethoden demonstriert. Unsere Experimente umfassten die Kopplung des ACTIS-Setups mit vier verschiedenen Detektionsmethoden: Fluoreszenzdetektion (FLD), Flugzeit - Massenspektrometrie (TOF-MS), induktiv gekoppelte Plasma - Massenspektrometrie (ICP-MS) und Atomemissionsspektroskopie (ICP-AES). Die Bindung von Quercetin-Eisen (FeQ_2)-Komplex an β -Lactoglobulin (BLG) wurde mithilfe von ACTIS-TOF-MS untersucht. Neben der K_d - Bestimmung wurden auch Experimente zur Verbesserung der Fe - Detektion mit ICP-Techniken durchgeführt. Abschließend wurde der Einfluss der Detektor-Konfiguration, insbesondere des inneren Radius der Transferkapillare, *in silico* mit Hilfe von Computersimulationen untersucht.

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1 Introduction

Molecular interactions of proteins with other biomolecules are crucial for various biochemical reactions and processes. The association and dissociation of protein-compound complexes determines their functionality [1]. Numerous factors including pH value and temperature, can influence the dissociation of such complexes [2]. Thermodynamic stability, which characterizes the tendency of complexes to exist in equilibrium conditions is quantified through the dissociation constant K_d [3].

Dissociation constant is an important characteristic to be evaluated in the pharmacology for drug discovery and design [4]. For instance, the evaluation of drug-receptor binding strength reveals the drugs efficiency. In material chemistry, the dissociation constant of metal complexes is used to predict its redox potential and catalytic properties [5]. More precisely, the dissociation constant provides insights into the stability of metal complexes, which is linked to their ability to undergo redox reactions and catalyze various chemical processes [6].

1.1 Definition of dissociation constant K_d

A reversible chemical reaction of a compound (C) binding to a protein (P) can be described with the following equation:



At equilibrium, the rates of forward and reverse reactions are equal and all components in the system do not have tendency to change their concentration [7]. Their concentrations at equilibrium define the dissociation constant K_d as follows:

$$K_d = \frac{[P][C]}{[PC]} \quad (2)$$

[C], [P], and [PC] refer to compound, protein, and complex concentrations at equilibrium, respectively. If we know the starting concentrations of P and C ($[P]_0$ and $[C]_0$) and we are able to determine either the [PC] or [C], the K_d value can be calculated by applying formula (2) on previously calculated or determined [P], [C], and [PC].

Conceptually, determining K_d is relatively simple. In practice, however, it is a challenging task. To find K_d (independent of the starting concentrations), wide range of concentration ratios of $[P]_0$ and $[C]_0$ must be evaluated. The assessment of K_d of a specific PC complex typically involves investigating a mixture with a constant $[C]_0$ and gradually increasing $[P]_0$. For each $[P]_0$, the ratio of [PC] to [C] is determined and K_d is found as the inflection point of the corresponding binding isotherm.

1.2 Established methods for finding K_d

Established methods employed for finding K_d of protein-compound complexes predominantly rely on biosensorics and calorimetric methodologies [8]. The accuracy of K_d may have a high impact on the investigated biochemical or catalyst processes. For example, the detection sensitivity of polymerization-based amplification reactions can be precisely predicted with the K_d value [9]. Moreover, an accurate K_d is crucial for the optimization of drug discovery, with a primary focus on the thermodynamics of the drug-receptor binding [10]. Despite the high impact of accurate K_d values for various applications, obtaining of similar values for one complex may be challenging [11–13]. The most commonly used methods for finding K_d are isothermal titration calorimetry and surface plasmon resonance [14].

Isothermal titration calorimetry (ITC) is considered as gold standard for finding K_d [15]. ITC measures the heat flow between a reference and a measurement cell (Figure 1). The reference cell is filled with the solvent. At the beginning, the measurement cell is filled with the protein or compound solution. Subsequently, the solution of the other complex component is added slowly to the measurement cell while the temperature is kept constant. Any release or absorption of heat is recorded. The heat change corresponds to the change of the fraction of bound compound. With increased compound concentration in the titration cell less heat is absorbed or released and signal saturation occurs. Besides finding K_d , ITC provides direct insight into enthalpy and entropy changes caused by molecular interactions as well as the reaction stoichiometry [16]. These thermodynamic parameters can be used to understand the underlying mechanism of the interaction.

ITC is a direct and label free approach but it possesses some inherent sources of inaccuracy. Very weak binding affinities cause minor heat changes that may not be detected due to instrumental signal-to-noise ratio. Furthermore, even a small amount of impurities as well as nonspecific P-P and C-C binding can have a strong impact on the final results and potentially lead to false conclusions [17].

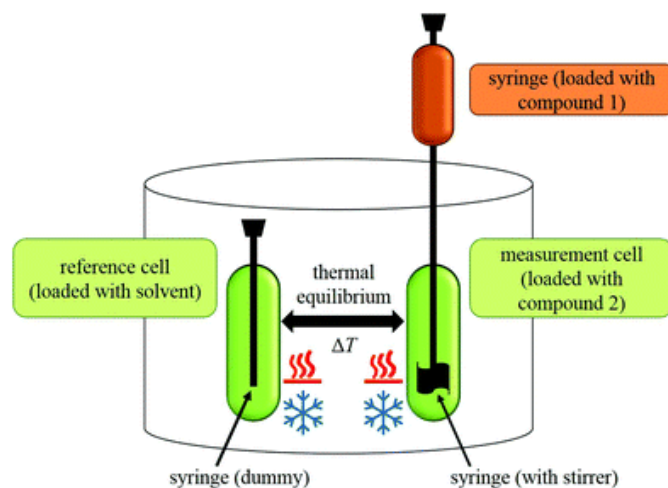


Figure 1: The schematic illustration of ITC. Reproduced from [18] with permission from the Royal Society of Chemistry.

Surface plasmon resonance (SPR) is a biosensorics technique based on a phenomenon known as a surface plasmon resonance [19]. SPR refers to the resonant oscillations of free metal electrons when polarized light strikes a thin metal layer. In SPR protein or compound molecules are immobilized on a thin gold layer fixed on a transparent prism (Figure 2). The thickness of the gold layer is commonly within the range of few hundreds to thousands angstroms (Å) [20]. A microfluidic system is used to continuously propagate the solution of the other complex component on the gold surface and a light source excites the gold from the bottom side. Biomolecular interactions cause the changes in refractive index consequently changing the resonance angle, which is used as SPR signal.

SPR signals can reveal information about binding kinetics and affinity. The main limitation of SPR for finding K_d is its sensitivity. Low mass molecules cause minor changes of the angle of refraction that may not be detectable. The immobilization of biomolecules represents another source of inaccuracy since it can greatly affect the investigated affinity [21].

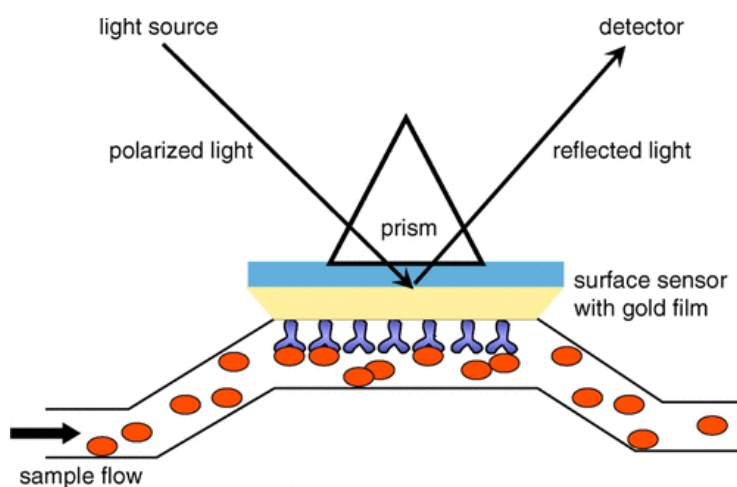


Figure 2: Schematic illustration of SPR. Adapted with permission from [22]. Copyright 2023 American Chemical Society.

Due to such sources of inaccuracies, variations of up to 100-fold in K_d values for the same PC are gained from different determination methods applied by different researchers [23]. Therefore, a new approach with absence of inherent sources of inaccuracy is desired in order to avoid false conclusions caused by unreliable K_d values. A new method that is based on a deterministic phenomenon would have a potential to greatly improve the determination of K_d . Basic advantage of such method would be the possibility to explain and consequently to predict the experimental outcome more reliably. A potential candidate, “Accurate constant via transient incomplete separation” (ACTIS) was introduced as a method based on a deterministic phenomenon and hypothetically free of inherent sources of inaccuracy [24].

1.3 Accurate constant via transient incomplete separation (ACTIS)

ACTIS is a recently introduced method for assessing K_d [24]. Theoretically, this method is free of inherent sources of inaccuracy and thus highly promising to become a reference-standard method for finding K_d values [25].

The principle of transient incomplete separation (TIS) is used in ACTIS to determine unbound C. TIS is a phenomenon that was first described in 1910. [26]. Over the last forty years it was extensively studied in experiments and simulations [27-28]. The concept of TIS is based on a characteristic flow profile of species in laminar pipe flow depending on their transverse diffusion. In a capillary of length l and inner radius r , the liquid is propagated by a pressure gradient between capillary ends. A characteristic parabolic flow profile occurs in this laminar pipe flow [28]. In this flow profile, the maximal velocity lies in the centre of the capillary. With increased distance from the capillary centre, the velocity is reduced gradually until it finally reaches 0 at the capillary walls [29]. Therefore, molecules in the capillary experience a different velocity, depending on their lane as presented in Figure 3.

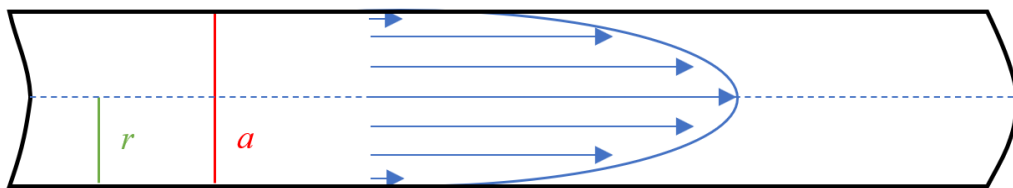


Figure 3: Velocity distribution in parabolic flow profile with r as a variable along the radius a of the capillary, from $r = 0$ to $r = a$

The molecules in the capillary centre, experience the maximal flow velocity $v_{\max}$:

$$v_{\max} = 2 \times v_{\text{mean}} \quad (3)$$

The average velocity of molecules is determined in dependence of flow rate Q and capillary diameter a :

$$v_{mean} = \frac{Q}{\pi \times a^2} \quad (4)$$

The velocity of all molecules as function of r (the distance of the molecule from the centreline) is described with the following formula:

$$v(r) = v_{max} \times \left(1 - \frac{r^2}{a^2}\right) \quad (5)$$

The flow profile of molecules in a capillary is mainly influenced by how they shift lanes while traveling in a straight line. This shifting movement, known as transverse diffusion, affects how quickly molecules can switch between the centre and the walls of a capillary. In general, molecules at the capillary center move faster compared to those near the capillary wall (Figure 3).

When transverse diffusion is low, molecules move slowly between the capillary center and its walls. With time, variations in velocity became more apparent and this results in a flow profile shown in Figure 4A. On the other hand, high transverse diffusion allows molecules to smoothly change positions within the capillary. Therefore, their velocities became more similar with the time resulting in a more evenly balanced flow profile (Figure 4B).

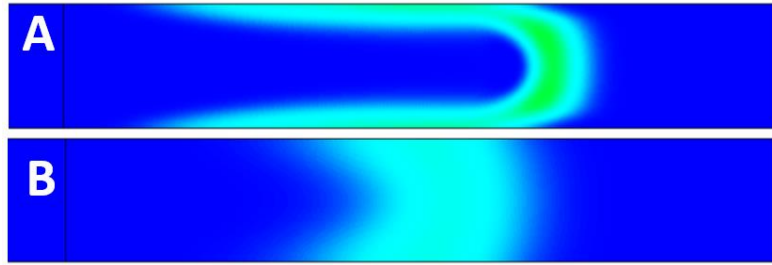


Figure 4: Different flow profiles resulting from different transversal diffusion constants of the molecules. Flow profile of the high (A) and the low (B) diffuse molecules

Different flow profiles caused by difference in a transversal diffusion of molecule species, such as C and PC, result in transient incomplete separation (TIS) [24]. If the difference of transversal diffusions of C and PC is about an order of magnitude, then the propagation of their mixture in a capillary will result in a combination of two different flow profiles. Low transverse diffusion of PC will cause faster propagation around the capillary centre compared to C. C molecules at the capillary centre propagate a bit slower due to a higher rate of transversal position changes. The time point at which the signal of eluted C reaches its maximum is denoted as a characteristic time of transverse diffusion, τ_C . In the short time window around τ_C , denoted as a transitional stage, the small portion of PC moves faster than C molecules while a tail of PC near the capillary walls moves slower than C. As a result, incomplete separation of PC and C occurs, since their concentration profiles overlap (see Figure 5).

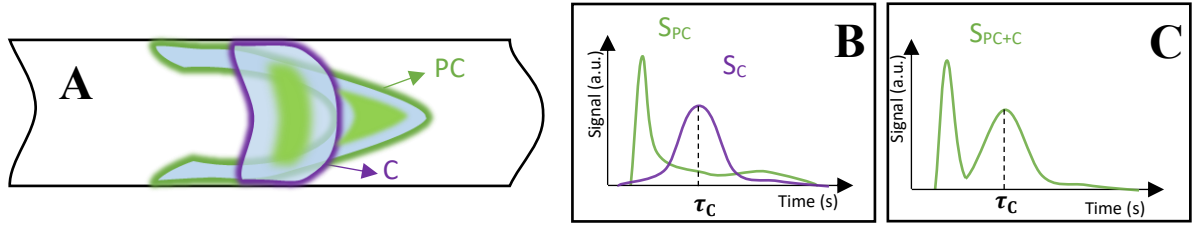


Figure 5: Transitional stage of an equilibrated mixture of P and C propagated through a capillary. Different flow profiles of PC and C fraction occur (A). Overlapping concentration profiles of C from PC and C fractions (B). Resulting cumulative C signal (C).

The diffusion coefficient of C, μ_C and the capillary inner radius r define τ_C as:

$$\tau_C = \frac{r^2}{\mu_C} \quad (6)$$

The flow rate used to propagate the plug of equilibrated mixture of PC, P and C is chosen based on capillary length l and previously calculated τ_C :

$$Q = \frac{l}{\tau_C} \quad (7)$$

At the end of the capillary in which the mixture is propagated, eluted fluid is transferred directly into a detection system, which quantifies the presence of C in it over the time. The resulting signal presents the cumulative C signal of both PC and C fractions. This cumulative C signal over the time is further denoted as a *separagram*. An example of separagram is given in Figure 5C. While separagram includes C signals of the entire ACTIS measurement, the separation peak refers to a segment of the separagram specifically indicating a compound signal during the separation step of the ACTIS measurement.

The following paragraphs describes the application of TIS to assess the K_d of a PC complex in ACTIS. Due to significantly smaller size of C molecules compared to the PC complex, their diffusion is considerably greater, resulting in different flow profiles. Thus, the concept of TIS can be applied to determine the fraction of unbound C in the equilibrium mixture of P, PC, and C. If the initial C and P concentrations are known, the determination of unbound C can be used to find the K_d . The fraction of free C is defined as R :

$$R = \frac{[C]}{[C]_0} \quad (8)$$

Where $[C]$ refers to a concentration of free C molecules in the equilibrium mixture and $[C]_0$ refers to a concentration of C added into the mixture.

When different equilibrated PC mixtures, with constant $[C]_0$ and varying concentration of P added into the mixture ($[P]_0$) are measured, R will also change depending on $[P]_0$ and K_d of PC complex. *Binding isotherm* represents the dependence of R on $[P]_0$ [30]. If we can determine the R values, K_d can be found as the deflection point of the binding isotherm as presented in Figure 6.

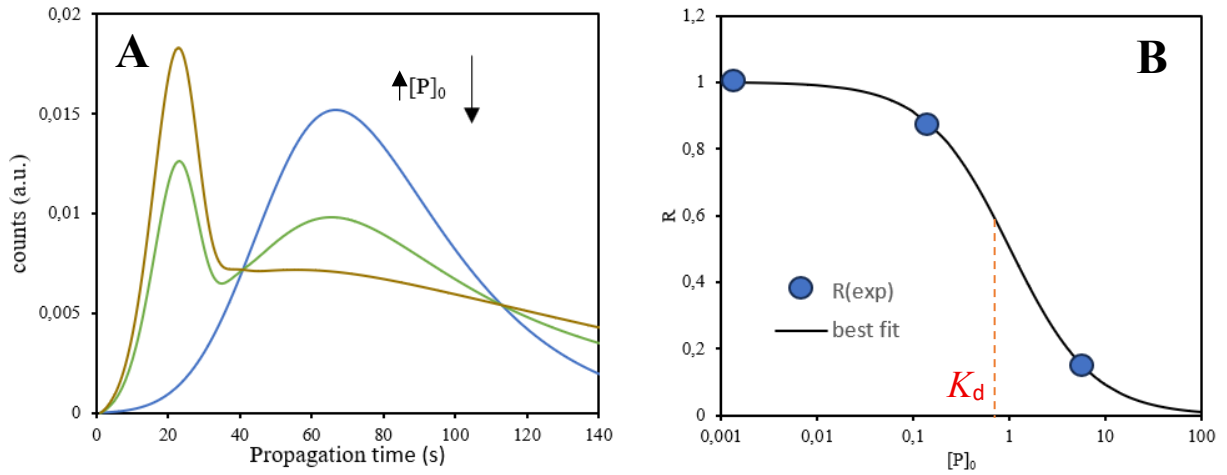


Figure 6: Resulting C signals of three equilibrated mixtures with constant $[C]_0$ and varying $[P]_0$ (A) and the resulting binding isotherm (B).

The cumulative signal of C, S , is calculated from R as follows:

$$S = S_C \times R + S_{PC} \times (1 - R) \quad (9)$$

where S_C corresponds to pure compound signal and S_{PC} represents the signal of the pure PC complex.

The transformation of equation 9 gives the formula for calculation of experimental R , R_{exp} from the corresponding C signals:

$$R_{exp} = \frac{S - S_{PC}}{S_C - S_{PC}} \quad (10)$$

At very high $[P]_0$ added into a mixture, we assume that nearly all the C molecules are incorporated into the PC complex. Therefore, the compound signal at very high protein concentrations $S_{[P]_0 \gg K_d}$ is approximately equal to the S_{PC} . Analogous to that, compound signal at very low protein concentrations, $S_{[P]_0 \ll K_d}$ is approximately equal to the S_C .

If we measure PC mixtures with constant $[C]_0$ and following $[P]_0$ variations: $[P]_0 \gg K_d$, $[P]_0 \ll K_d$ and an arbitrary $[P]_0$, the equation 10 can be written as:

$$R_{exp} \approx \frac{S_{[P]_0} - S_{[P]_0 \gg K_d}}{S_{[P]_0 \ll K_d} - S_{[P]_0 \gg K_d}} \quad (11)$$

where $S_{[P]_0}$ refers to a S resulting from measurement of an equilibrated mixture with an arbitrary $[P]_0$ added into it.

Finally, a theoretical R_{theo} function is used to fit the experimental data R_{exp} . The R_{theo} values are calculated by applying following formula in which an arbitrary value is used for K_d as a starting value.

$$R_{theo} = -\frac{K_d + [P]_0 - [C]_0}{2[C]_0} + \sqrt{\left(\frac{K_d + [P]_0 - [C]_0}{2[C]_0}\right)^2 + \frac{K_d}{[C]_0}} \quad (10)$$

Two essential conditions must be met to achieve accurate K_d values: the reaction should be at equilibrium and the experiment must be done in the so-called binding regime [31-32]. More precisely, the $[C]_0$ is the limiting component and if it is similar to the K_d value, the resulting K_d will be affected by titration. Therefore, the ratio $[C]_0/K_d$ should be optimally 1/100.

Since the TIS relies on a deterministic process, it can be accurately described by using a differential equation system and without empirical coefficients known. Consequently, ACTIS separagrams can be computer-simulated allowing a comprehensive in-silico evaluation of ACTIS performance, including its accuracy [33].

Finally, let's briefly look at the experimental implementation of ACTIS. After a system consisting of P and C is selected for assessment, an appropriate detection system needs to be chosen. The choice of the detection system depends on the PC properties and detection system limitations. If the K_d of the PC is unknown, computer simulations or preliminary experiments can be used to estimate the K_d value. Based on the estimated K_d , the maximum $[C]_0$ can be determined. Subsequently, the mixtures of PC with constant $[C]_0$ and varying $[P]_0$ are prepared. After the equilibration of the PC mixtures, the actual ACTIS experiment is performed. One ACTIS experiment refers to a set of measurements of prepared PC mixtures. Typically, ten PC mixtures are prepared for a single ACTIS experiment. Each prepared mixture has multiple replicates, and each replicate is denoted as an ACTIS run. One run typically lasts about four minutes. In standard experiments, six replicates of each equilibrated mixture are performed. Including the time required for sample changing, the overall time for one whole ACTIS experiment is approximately four hours.

1.4 Thesis scope

ACTIS was firstly introduced in 2019 bringing a significant improvement to analytical methods for finding K_d [34]. Since then, various model systems have been evaluated using ACTIS. Using the fluorescence detector coupled to ACTIS, K_d for bovine serum albumin and fluorescein was determined to be $28 \pm 6 \mu\text{mol L}^{-1}$. By using MS as the detector, the K_d value for the same model system was found to be $31 \pm 6 \mu\text{mol L}^{-1}$ [24]. ACTIS coupled with MS as the detector assessed K_d of $1.4 \pm 0.2 \mu\text{mol L}^{-1}$ for the alpha-1-acidglycoprotein - alprenolol model system [24]. In further experiment, the investigations of binding of similar-sized molecules were performed. More specifically, K_d value of 0.12 nmol L^{-1} for the Mut-S binding aptamer model system was found [30]. Simultaneously, the computer simulations were investigated and Python script for evaluation was developed. The brief overview of already performed ACTIS investigations is given in Table 1.

Table 1: The overview of reported ACTIS experiments up until now

Protein	Compound	Detection	K_d	Reference
BSA	Fluorescein	Fluorescence	$22 \pm 2 \mu\text{mol L}^{-1}$	[24]
BSA	Fluorescein	Mass spectrometry	$31 \pm 4 \mu\text{mol L}^{-1}$	[24]
AGP ¹	Alprenolol	Mass spectrometry	$1.4 \pm 0.2 \mu\text{mol L}^{-1}$	[24]
Mut-S protein ²	Aptamer	Mass spectrometry	0.12 nmol L^{-1}	[30]

¹ α -1-acid glyco protein, ²His-tagged recombinant *Thermus aquaticus* Mut-S protein

Despite the broad range of ACTIS experiments, no experiments have been reported for the assessment of protein-metal binding. Therefore, this work was intended to further explore ACTIS applicability to these systems. This includes the following points:

- The building up and the evaluation of ACTIS setup functionality
- The evaluation of feasibility of selected protein-metal model system for ACTIS experiments
- The actual assessment of K_d of selected protein-metal model system employing ACTIS

The first stage of this work includes establishing an ACTIS setup since no ACTIS instrument existed at BOKU at the start of this project. Notably, ACTIS setup is not commercially available. It is crucial to detailly test the setup's stability and to find optimal solutions for maintaining constant and reproducible flow rates. Moreover, the optimal duration of individual run steps should be determined.

In the next stage, the functionality of the ACTIS setup must be evaluated in terms of actual K_d assessment. To achieve this, experiments using a relatively simple model system, preferably one previously investigated with ACTIS, will be conducted. The similarity of the results with prior ACTIS experiments will serve as a clear indicator of the instrumentation's suitability for further studies.

The selected protein-metal model system should be explored regarding protein and compound stability, solubility, and signal intensity in the chosen detection system. This step also includes first ACTIS experiment on this system in order to further explore its feasibility. Furthermore, the optimal $[C]_0$ for working solution for actual ACTIS experiment will be determined in this step.

Then, all the findings and results from the previously described points should be considered to enable successful assessment of K_d of a protein-metal complex. To the best of our knowledge, this would be the first protein-metal-binding assessment utilizing ACTIS. In addition to the main goal, several additional tasks need be done to enhance ACTIS as a method. In order to improve assessment of protein-metal systems, different detection systems need to be evaluated. In particular, detection methods which enable direct precise metal determination should be explored. Potential issues will be investigated, documented, and assessed with experimental and computational tools.

The possibility of assessing K_d of metal-protein complexes via ACTIS would be a significant extension of the application range. More metal detection systems with even lower LOQs, LODs, and signal-to-noise ratios could be coupled with ACTIS. Lower LOQ, LOD, and signal-to-noise would increase the range of accessible K_d values and, in turn, the range of investigated complexes.

2 Materials and methods

2.1 Model systems

In this work the assessing of K_d of two different model systems was done. The binding pairs: human serum albumin (HSA) and fluorescein (FLC) as well as β -lactoglobulin (BLG), quercetin (Q) and iron (Fe) were investigated by coupling ACTIS to different detection systems. The HSA-FLC system has many benefits regarding the application of ACTIS. Firstly, FLC is fluorometric active, which enables using the fluorescence detector (FLD) as a detection system. Both substances (HAS, FLC) are cost-effective and have great solubility in aqueous solutions [35-36]. Since a similar protein-compound system has already been investigated using ACTIS, our main consideration was to validate our ACTIS instrumentation and detection methods by comparing the results with literature values and our previous experiments.

Compared to HSA-FLC, BLG-FeQ₂ is a more complex system (Figure 7). In this model system the FeQ₂ is the compound in the BLG-FeQ₂ complex. Iron binds to quercetin with very high affinity at a physiologic pH of 7.4 [37-38]. The binding of FeQ₂ complex to BLG was recently investigated in terms of its antiallergenic potential [39]. It was found that the BLG-FeQ₂ complex plays an important role in preventing milk allergies. This study reveals previous unrecognized immune-regulatory effects of BLG-FeQ₂ complex. Additionally, it was found that the affinity of BLG binding to the FeQ₂ is in nmol L⁻¹ range. Theoretically, this system is adaptable for various detection systems. This represents a significant advantage for studying the potential of ACTIS by exploring its compatibility to other detection systems. The fluorescence of Q enables the employment of the fluorescence detector. Organic MS methods could be used to detect FeQ₂. Finally, the precise Fe detection over time can be done by applying element analytic methods, such as inductively coupled plasma mass spectrometry (ICP-MS) and atomic emission spectroscopy (ICP-AES).

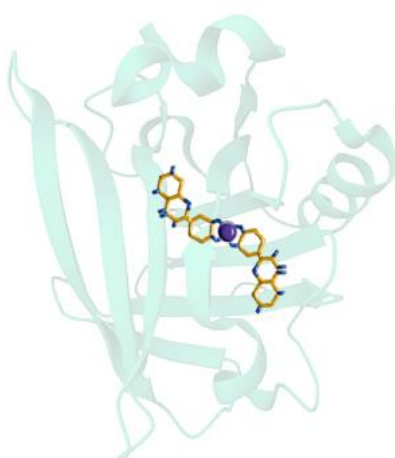


Figure 7: Bovine β -lactoglobulin complex with quercetin and iron

2.2 Reagents and solutions

Following solutions were used in our ACTIS experiments:

stock solutions – concentrated solution of a specific substance used to prepare working solutions;

working solutions – mixture of a specified amount of protein and a compound of investigated model system, measured in ACTIS experiments;

ACTIS running solution (ASR) – used as a background solution to prefill the ACTIS setup and to propagate the sample plug through it.

2.2.1 HSA-FLD solutions

Albumin from human serum (HSA) and fluorescein were purchased from Sigma Aldrich. All solutions were made by using 30 mmol L⁻¹ ammonium acetate (NH₄Ac) as a solvent with pH=7.2. NH₄Ac was prepared by weighing 1.2 g of ammonium acetate purchased from Thermo Fisher and dissolving it in 500 mL MQ-H₂O. 1 mol L⁻¹ NaOH solution, purchased from Thermo Fisher, was used to adjust the pH of the NH₄Ac to 7.2. The working solutions of HSA and fluorescein prepared with corresponding final concentrations are shown in the Table 2. The HSA-FLC mixtures were prepared by mixing the corresponding amounts of HSA and FLC working solutions as shown in Table 3 and Table 4. The mixtures were incubated for 2 h at room temperature of 22 °C before measurements. Each experiment took two days and the mixtures were measured in increasing protein concentrations. Working solutions were stored in the fridge at 4 °C.

Table 2: HSA-FLC stock solutions

Stock solution	Mass of component	Added NH ₄ Ac volume	Final concentration
HSA I	208.0 mg	4 mL	7.8×10^{-1} mmol L ⁻¹
HSA II	400.0 mg	3 mL	2.0 mmol L ⁻¹
FLC I	3.3 mg	10 mL	1.0 mmol L ⁻¹
HSA III	1:100 dilution of HSA I with NH ₄ Ac solution		7.8×10^{-3} mmol L ⁻¹
HSA IV	1:100 dilution of HSA II with NH ₄ Ac solution		2.0×10^{-2} mmol L ⁻¹
FLC II	1:100 dilution of FLC I with NH ₄ Ac solution		1.0×10^{-2} mmol L ⁻¹

Table 3: Table of HSA-FLC solutions made for the first ACTIS-FLD experiment

Nr.	Final HSA concentration ($\mu\text{mol L}^{-1}$)	HSA stock solution	Volume of HSA stock solution added (μL)	FLC stock solution	Volume of FLC stock solution added (μL)	Added NH_4Ac volume (μL)
1	700.00	HSA I	895	FLC II	5	100
2	496.80	HSA I	635	FLC II	5	360
3	101.70	HSA I	130	FLC II	5	865
4	50.00	HSA I	64	FLC II	5	931
5	10.00	HSA I	13	FLC II	5	982
6	5.00	HSA III	639	FLC II	5	360
7	1.00	HSA III	128	FLC II	5	865
8	0.50	HSA III	64	FLC II	5	931
9	0.25	HSA III	32	FLC II	5	963
10	0.10	HSA III	13	FLC II	5	982

Table 4: Table of HSA-FLC solutions made for the second ACTIS-FLD experiment

Nr.	Final HSA concentration ($\mu\text{mol L}^{-1}$)	HSA stock solution	Volume of HSA stock solution added (μL)	FLC stock solution	Volume of FLC stock solution added (μL)	Added NH_4Ac volume (μL)
1	1800.0	HSA II	900	FLC II	5	95
2	1200.0	HSA II	600	FLC II	5	395
3	1000.0	HSA II	500	FLC II	5	495
4	700.0	HSA II	350	FLC II	5	645
5	500.0	HSA II	250	FLC II	5	745
6	250.0	HSA II	125	FLC II	5	870
7	100.0	HSA II	50	FLC II	5	945
8	50.0	HSA II	25	FLC II	5	970
9	10.0	HSA IV	500	FLC II	5	495
10	5.0	HSA IV	250	FLC II	5	745

2.2.2 BLG-FeQ₂ solutions

β -lactoglobulin from bovine milk and quercetin were purchased from Sigma Aldrich. Iron (III) chloride hexahydrate was purchased from PanReach AppliChem. NH₄Ac was prepared by weighing 1.2 g of ammonium acetate purchased from Thermo Fisher and dissolving it in 500 mL MQ-H₂O following by adjusting the pH to 7.2 with 1 mol L⁻¹ NaOH. The solubility of BLG and FeCl₃ × 6H₂O in NH₄Ac was very good and all the working solutions were made easily as described in the Table 5. However, the quercetin solubility at pH 7.2 was low. The first quercetin working solution was made by dissolving 17.81 g in 27.960 mL of NH₄Ac followed by homogenization for 10 minutes in an ultrasonic bath. After first FLD measurements of pure quercetin solutions, the yellow solid residuals were observed on the connection part of the syringe and the capillary. The poor repeatability of fluorescence signals implicated that injected quercetin concentration varied. After closer inspection, we noticed that quercetin was not completely dissolved in the solution. The increasing of the pH of the NH₄Ac was found to be an important factor to improve the quercetin solubility. Therefore, a small amount of 1 mol L⁻¹ NaOH solution was added to the stock solution, as described in the Table 5.

Table 5 shows the processes of making BLG, Q and Fe stock solutions that were used later to prepare working solutions for ACTIS experiments.

Table 5: Stock solutions used for making BLG-FeQ₂ working solutions for ACTIS measurements

Stock solution	Added mass	Added NH ₄ Ac volume	Final concentration
BLG I	92.1 mg	2.00 mL	2.5 mmol L ⁻¹
Q I	17.8 mg	27.96 mL	2.0 mmol L ⁻¹
Fe I	38.3 mg	14.20 mL	10.0 mmol L ⁻¹
BLG II	1:10 dilution of BLG I with NH ₄ Ac solution		2.5 × 10 ⁻¹ mmol L ⁻¹
BLG III	1:10 dilution of BLG II with NH ₄ Ac solution		2.5 × 10 ⁻² mmol L ⁻¹
BLG IV	1:100 dilution of BLG II with NH ₄ Ac solution		2.5 × 10 ⁻³ mmol L ⁻¹
BLG V	1:10 dilution of BLG IV with NH ₄ Ac solution		2.5 × 10 ⁻⁴ mmol L ⁻¹
BLG VI	1:10 dilution of BLG V with NH ₄ Ac solution		2.5 × 10 ⁻⁵ mmol L ⁻¹
Q II	1:2 dilution of Q I with NH ₄ Ac solution with 200 μ L of 1M NaOH per 5 mL solution		1.0 mmol L ⁻¹
Q III	1:1000 dilution of Q II with NH ₄ Ac solution		1.0 × 10 ⁻³ mmol L ⁻¹
Q IV	1:5 dilution of Q III with NH ₄ Ac solution		2.0 × 10 ⁻⁴ mmol L ⁻¹
Q V	1:50 dilution of Q II with NH ₄ Ac solution		2.0 × 10 ⁻² mmol L ⁻¹
Fe II	1:20 dilution of Fe I with NH ₄ Ac solution		1.0 × 10 ⁻² mmol L ⁻¹
Fe III	1:1000 dilution of Fe II with NH ₄ Ac solution		5.0 × 10 ⁻⁴ mmol L ⁻¹

Fe IV	1:5 dilution of Fe III with NH ₄ Ac solution	$1.0 \times 10^{-4} \text{ mmol L}^{-1}$
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One set of BLG-FeQ₂ mixtures was measured with ACTIS-FLD, ACTIS-TOF-MS, and ACTIS-AES. Three runs for each mixture were carried out using ACTIS-FLD. In both ACTIS-TOF-MS experiments, six replicates were conducted. Only one run per mixture was performed using ACTIS-AES. The preparation of all the working solutions is shown in the Tables 6-10. Note that in the preparation procedure, the initial mixing of Q and Fe was followed by 15-minutes of incubation at room temperature of 23 °C. After incubation the proper amount of NH₄Ac and BLG stock solutions were added. The concentration of compound, in this case the FeQ₂ complex, is constant in each solution from one experiment while the protein concentration was varied.

Table 6: BLG-FeQ₂ working solutions prepared for ACTIS-FLD experiment

No.	Final [BLG] ($\mu\text{mol L}^{-1}$) ¹⁾	BLG stock solution	Added volume of BLG stock solution (μL)	Q stock solution	Added volume of Q stock solution (μL)	Fe stock solution	Added volume of Fe stock solution (μL)	Added NH₄Ac volume (μL)
1	750.0	BLG I	450	Q II	150	Fe III	150	750
2	500.0	BLG I	300	Q II	150	Fe III	150	900
3	250.0	BLG I	150	Q II	150	Fe III	150	1050
4	100.0	BLG I	60	Q II	150	Fe III	150	1140
5	50.0	BLG II	300	Q II	150	Fe III	150	900
6	10.0	BLG II	60	Q II	150	Fe III	150	1140
7	5.0	BLG III	300	Q II	150	Fe III	150	900
8	1.0	BLG III	60	Q II	150	Fe III	150	1140
9	0.1	BLG IV	60	Q II	150	Fe III	150	1140
10	0.01	BLG V	60	Q II	150	Fe III	150	1140

Table 7: BLG-FeQ₂ working solutions prepared for the first ACTIS-TOF-MS experiment

No.	Final [BLG] ($\mu\text{mol L}^{-1}$)	BLG stock solution	Added volume of BLG stock solution (μL)	Q stock solution	Added volume of Q stock solution (μL)	Fe stock solution	Added volume of Fe stock solution (μL)	Added NH ₄ Ac volume (μL)
1	1000	BLG IV	800	Q IV	100	Fe IV	100	1000
2	750.0	BLG IV	600	Q IV	100	Fe IV	100	1200
3	500.0	BLG IV	400	Q IV	100	Fe IV	100	1400
4	250.0	BLG IV	200	Q IV	100	Fe IV	100	1600
5	100.0	BLG IV	80	Q IV	100	Fe IV	100	1720
6	50.0	BLG IV	40	Q IV	100	Fe IV	100	1760
7	25.0	BLG V	200	Q IV	100	Fe IV	100	1600
8	10.0	BLG V	80	Q IV	100	Fe IV	100	1720
9	5.0	BLG VI	400	Q IV	100	Fe IV	100	1400
10	1.0	BLG VI	80	Q IV	100	Fe IV	100	1720

Table 8: BLG-FeQ₂ working solutions prepared for the second ACTIS-TOF-MS experiment

No.	Final [BLG] (nmol L^{-1})	BLG stock solution	Added volume of BLG stock solution (μL)	Q stock solution	Added volume of Q stock solution (μL)	Fe stock solution	Added volume of Fe stock solution (μL)	Added NH ₄ Ac volume (μL)
1	250.0	BLG IV	200	Q IV	100	Fe IV	100	1600
2	100.0	BLG IV	80	Q IV	100	Fe IV	100	1720
3	75.0	BLG IV	60	Q IV	100	Fe IV	100	1740
4	50.0	BLG IV	40	Q IV	100	Fe IV	100	1760
5	35.0	BLG IV	28	Q IV	100	Fe IV	100	1772
6	25.0	BLG V	200	Q IV	100	Fe IV	100	1600
7	15.0	BLG V	120	Q IV	100	Fe IV	100	1680
8	10.0	BLG V	80	Q IV	100	Fe IV	100	1720
9	5.0	BLG VI	400	Q IV	100	Fe IV	100	1400
10	1.0	BLG VI	80	Q IV	100	Fe IV	100	1720

Table 9: BLG-FeQ₂ Solutions made for the ACTIS-ICP-AES experiment

No.	Final [BLG] ($\mu\text{mol L}^{-1}$) ¹⁾	BLG stock solution	Added volume of BLG stock solution (μL)	Q stock solution	Added volume of Q stock solution (μL)	Fe stock solution	Added volume of Fe stock solution (μL)	Added NH ₄ Ac volume (μL)
1	1000	BLG I	80	Q V	20	Fe II	20	80
2	500.0	BLG I	40	Q V	20	Fe II	20	120
3	100.0	BLG II	80	Q V	20	Fe II	20	80
4	50.0	BLG II	40	Q V	20	Fe II	20	120
5	10.0	BLG III	80	Q V	20	Fe II	20	80
6	5.0	BLG III	40	Q V	20	Fe II	20	120
7	1.0	BLG IV	80	Q V	20	Fe II	20	80
8	0.5	BLG IV	40	Q V	20	Fe II	20	120
9	0.25	BLG IV	20	Q V	20	Fe II	20	140
10	0.1	BLG V	80	Q V	20	Fe II	20	80

Table 10: Protein concentration ranges and compound concentrations in measured samples for each detection method utilized for assessing K_d of BLG-FeQ₂ model system

Detection method	FLD	TOF-MS		AES
		1 st experiment	2 nd experiment	
[BLG] ₀	750.0 – 1.0×10^{-2} $\mu\text{mol L}^{-1}$	1.0×10^3 - 1.0 nmol L^{-1}	2.5×10^2 – 1.0 nmol L^{-1}	1000 – 0.1 $\mu\text{mol L}^{-1}$
[FeQ ₂]	50.0 $\mu\text{mol L}^{-1}$	5.0×10^{-3} $\mu\text{mol L}^{-1}$	5.0×10^{-3} $\mu\text{mol L}^{-1}$	1.0 $\mu\text{mol L}^{-1}$

No K_d assessment was performed using ACTIS-ICP-MS. This technique was evaluated by measuring Fe solutions. The overview of injected solutions with corresponding preparation recipes are given in the Table 11.

Table 11: The Fe solutions prepared for testing of ACTIS-ICP-MS

[Fe] ₀	Stock solution used for preparation	The solvent used to dilute the stock solution
5.0 $\mu\text{mol L}^{-1}$	Fe II	30.0 mmol L^{-1} NH ₄ Ac (pH=7.2)

5.0 $\mu\text{mol L}^{-1}$	1000 ng g ⁻¹ Fe solution in 2% HNO ₃ and 30.0 mmol L ⁻¹ NH ₄ Ac (pH=7.2) 0.1% HCl
5.0 $\mu\text{mol L}^{-1}$	1000 ng g ⁻¹ Fe solution in 2% HNO ₃ and Sub-boiled H ₂ O 0.1% HCl

2.3 ACTIS setup

The ACTIS setup consisted of a pump, valve, flow sensor, and five capillaries. The setup scheme is presented in Figure 8. The pump was used to propagate the ACTIS running solution (ARS) and the sample plug through the capillaries. ARS refers to the solution used to prefill the ACTIS setup and to propagate the sample plug through it. The 30 mmol L⁻¹ NH₄Ac solution with pH=7.2 was used as ARS in ACTIS experiments in this work. Three pumps were tested for the application in our ACTIS setup. The overview of tested pumps is given at the end of this section. Liquid flow sensor SLF3S-0600F produced by Sensorion and purchased from Bartels Mikrotechnik was used to monitor the flow rate. 10-port valve Cheminert C2H-2340D, produced by VICI Valco Instruments, was used to enable the smooth loading of the sample while maintaining constant flow rate. The capillary in which the TIS takes place is referred as a separation capillary. In this setup, a separation capillary with length of 60 cm and an inner diameter of 254 μm was used. The injection capillary was prefilled with sample and later connected via the valve to the separation capillary to load the sample into it. The injection capillary was 15.6 cm long with an inner diameter of 102 μm . Besides separation and injection capillaries, ACTIS setup also had two waste and one sample introduction capillary. Both waste capillaries have inner diameter of 50.8 mm. The sample introduction capillary was connected to a syringe filled with sample solution.

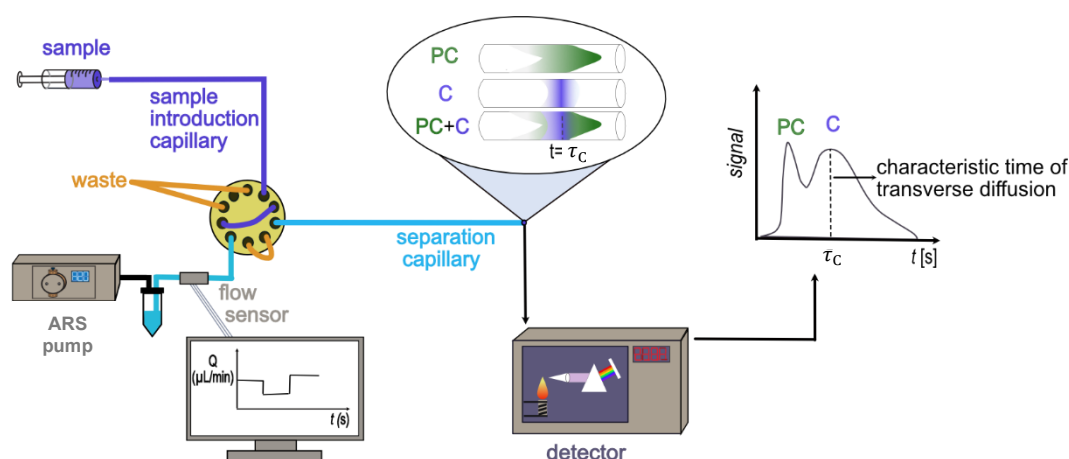


Figure 8: The scheme of ACTIS setup

The following paragraphs provide the explanation of a single ACTIS run. One ACTIS run consists of four steps: 1) sample injection, 2) sample loading, 3) separation, and 4) purge step. A scheme of different valve positions and the flow of ARS and a sample in them is given in appendix, section 1.

For sample injection (step 1) the starting valve position is the position A. In this position, the injection capillary is connected to the waste, while the ARS is directed into the separation capillary. The sample is introduced manually into the injection capillary with a 1 mL syringe (produced by Rays). Simultaneously, the pump fills ARS into the separation capillary at flow rate matching the flow rate used in a separation step, Q_{sep} .

After the injection capillary is purged and filled with the sample, sample loading (step 2) begins by switching the vent to the B position. In the B position the ARS is pumped directly into the injection capillary which is now connected to the separation capillary. At injection flow rate, Q_{inj} the sample is slowly transferred from injection into the separation capillary. This step ensures that the whole sample plug volume is pushed into the separation capillary.

After sample loading step, the flow rate is increased to Q_{sep} . To begin the separation (step 3), the flow rate of the sample plug through the separation capillary is chosen to ensure that TIS occurs at the end of the capillary. As already mentioned, the choice of the duration time and flow rates of single steps plays a crucial role in one ACTIS run. The injection step was performed at flow rate of $20 \mu\text{L min}^{-1}$ for 20 s. The volume of the injection capillary V_{inj} can be calculated as follows:

$$V_{inj} = \pi \times r^2 \times l \quad (11)$$

The r is the inner radius of injection capillary ($51 \mu\text{m}$) and l refers to its length (15.6 cm). Inserting these values in the formula results in V_{inj} of $1.2 \mu\text{L}$. At the flow rate of $20 \mu\text{L min}^{-1}$ the time needed to push this volume twice through the injection capillary is:

$$t_{inj} = \frac{3 \times 1.2 \mu\text{L}}{15 \mu\text{L min}^{-1}} = 0.24 \text{ min} = 14.4 \text{ s} \quad (12)$$

In order to simplify the automatization of the valve and the pump switch, the duration of the sample loading step was set to 15 s.

The duration of the separation step was set twice as long as the characteristic transverse diffusion time of compound, τ_C . By setting the duration of separation step longer we are able to see the full peaks. As described in introduction part, the τ_C is calculated from the inner radius r , and diffusion constant of the compound, μ_C (see equation 6). We estimated diffusion constant of the FeQ_2 complex, μ_{FeQ_2} , to be similar to the Fe (III) diffusion constant of $0.604 \times 10^{-9} \text{ m}^2 \text{ s}^{-1}$ [40]. The calculation of the flow rate in the separation step, Q_{sep} is given in the equation 7. Here, τ_{FeQ_2} was 26.7 s and l was 60 cm, and Q_{sep} amounted $68 \mu\text{L min}^{-1}$, respectively. Same values of Q_{sep} and t_{inj} were applied in measurements of both

model systems to keep processes consistent. On the other hand, the acquisition time was much longer than the estimated τ_C and the evaluation included finding the maximum of diffusion peak. Since the Q_{inj} and the Q_{sep} varied depending on the used pump during the ACTIS run and the delay of valve switching affected the timing, we determined the real τ_C during the evaluation.

In the last step, high flow rates ($Q_{purge} > 100 \mu\text{L min}^{-1}$) were used to purge the setup with ARS. For this purpose, the pressure on the ARS pump was set to 2 bar and the valve position was switched every 3 seconds for 10 times. Switching of valve positions allowed the effective purge of potential sample residuals out of the valve.

Table 12 provides an overview of the ACTIS measurement steps with respective valve positions and the applied flow rates.

Table 12: Brief overview of ACTIS run steps

Measurement step	Short description	Flow rate	Valve position	Duration
Sample injection	Transfer of sample from syringe into injection capillary;	manually	A	20 s
	Simultaneously filling the separation capillary with the ARS	$68 \mu\text{L min}^{-1}$		
Sample loading	Transfer of sample plug from injection into separation capillary	$20 \mu\text{L min}^{-1}$	B	20 s
Separation	Propagation of sample plug through the separation capillary	$68 \mu\text{L min}^{-1}$	A	120 s
Purge	Purge the capillaries at high flow rates by switching the valve position	100-500 $\mu\text{L min}^{-1}$	both	60 s

The duration time and respective flow rates of each step in one ACTIS run are presented in Figure 9.

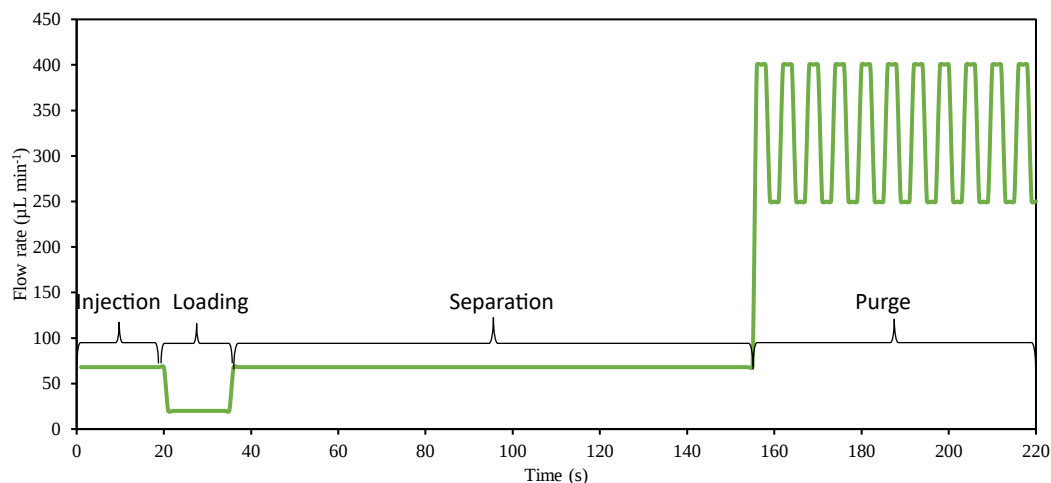


Figure 9: The duration and flow rates of respective steps in one ACTIS run

Even with subsequent τ_C determination, the Q_{inj} and Q_{sep} had to be maintained as constant as possible, because variations would have led to plug distortion.

It is challenging to find a pump that is able to produce constant low flow rates of 20 and 68 $\mu\text{L min}^{-1}$ during separation and valve switching. Three pumps were tested for this purpose: a syringe pump 704806 from Harvard Apparatus, a piezoelectric pump - mp6 liq (Bartels, microfluidic), and a pressure pump - Cobalt (Elveflow). The piezoelectric pump showed the highest flow rate variations. Syringe pump suffered from massive problems caused by air bubbles introduction into the capillary. We found that the most suitable pump for our setup is the pressure pump. The stability of the flow rate was good and the contactless pumping of ARS was also a beneficial characteristic.

However, we found additional concerns that should also be addressed. Namely, the position of the pressure pump relative to the detector position affected its performance due to syphon effects. Because of that, the pressure set on the pump produced different flow rates depending of the pump position. Because of the nebulizer gas flow in the ICP-MS device, the flow rate of the ARS was higher than needed, even with the pump switched off. In order to solve this issue, a 15 cm long capillary with 102 μm inner radius was attached between the flow rate sensor and the valve. This set up modification was applied only to the coupling ACTIS with ICP-MS.

To ensure consistent and repeatable measurements, it is necessary to switch the valve and change the flow rate at predefined time points for each measurement step as described above. At the beginning of the separation step these changes have to be done simultaneously. It is possible for one person to conduct the measurements and manually switch the valve and the pressure. Due to practical precision problems, shifts on the time axis are possible. For the ACTIS-AES measurements of BLG-FeQ₂ model and ACTIS-FLD measurements of HSA-FLC model, manual switching was performed. For all other measurements, a small Python program named *automACTIS*, implemented with the help of Dr. Sven

Kochmann was implemented. This program enabled synchronization of the pump, the valve, and in the case of FLD, also the detector. The source code can be found in the appendix, section 2.

2.4 Detection methods

The ACTIS setup was coupled to four different detectors by directly connecting the separation capillary: fluorescence detection (FLD), time-of-flight mass spectrometry (TOF-MS), inductively coupled plasma mass spectrometry (ICP-MS) and atomic emission spectroscopy (AES). Two of them, FLD and TOF-MS have suitable capillary connection, while ICP-MS and AES required an additional capillary connector. However, very robust and stable coupling with ACTIS characterises all four methods.

The FLD detector UltiMate 3000 by Dionex with a flow cell of 8 μL volume was used. The ACTIS-FLD is the only technique which was employed for both investigated model systems. For the HSA-FLC system measurements the excitation wavelength was set to 300 nm and emission wavelength to 350 nm. The acquisition was performed with a sensitivity of 1. For the BLG-FeQ₂ system measurements excitation wavelength was 423 nm, emission 515 nm, and sensitivity was set to 4. The flow cell temperature was set to 25 °C and the lamp mode to long life lamp for both systems. The overview of FLD parameters applied for HSA-FLC and BLG-FeQ₂ experiments is given in Table 13. ACTIS-FLD coupling is presented in Figure 10.

Table 13: The overview of FLD parameters

Parameter	HSA-FLC experiments	BLG-FeQ ₂ experiments
Excitation wavelength (nm)	300	423
Emission wavelength (nm)	350	515
Sensitivity	1	4
Flow Cell Temperature (°C)	25	25
Lamp Mode	Long Life Mode	Long Life Mode

The main advantages of FLD as an ACTIS detector include high sensitivity and specificity due to high extinction coefficient of fluorophore. On the other hand, FLD can only be applied on PC systems with a fluorescent compound. This serious limitation did not have an impact in this study since both compounds, FLC and FeQ₂ are fluorophores. [41-42]

Our FLD device had an integrated flow cell of 8 μL volume with a small detection window. If the separation flow rate for our systems is 68 $\mu\text{L min}^{-1}$, the flow cell content will be completely replaced in about 7 s. That implies that the detected signal at a specific time point represents a cumulative signal of the past 7 s. This results in signal overlapping, which impacts its resolution and intensity.

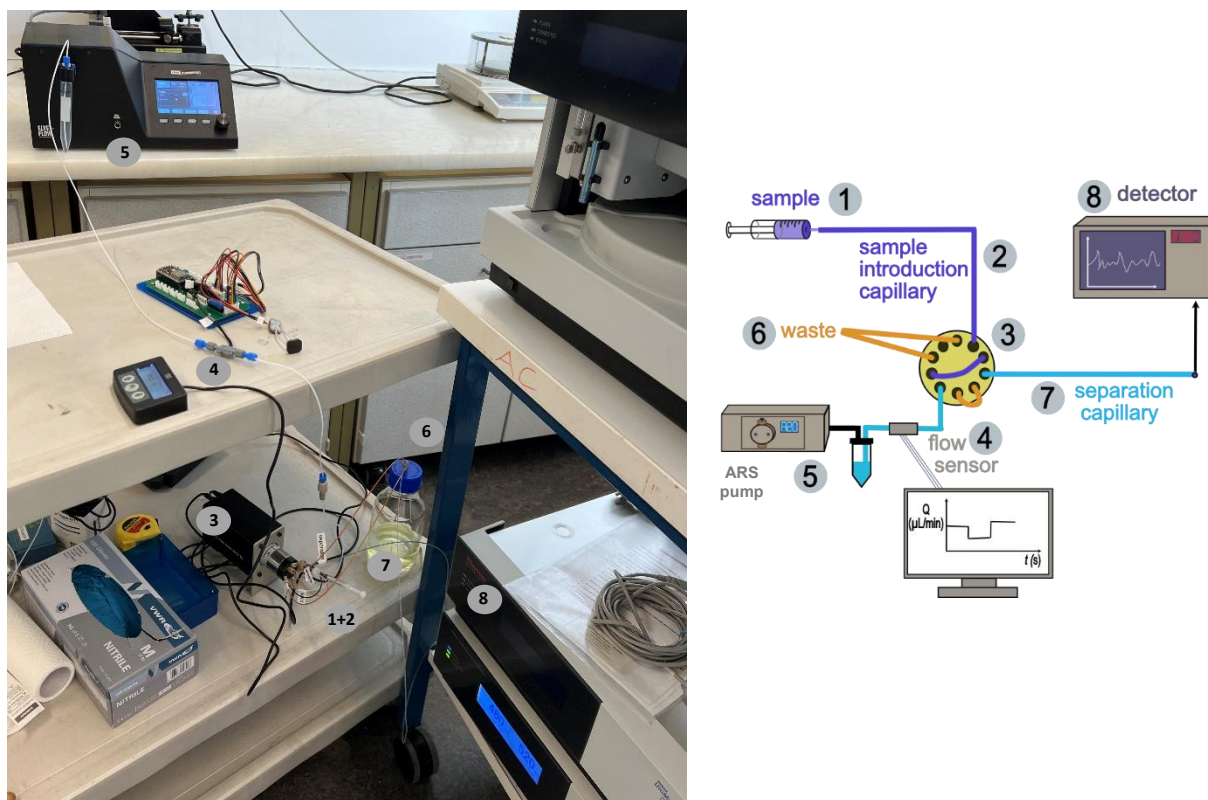


Figure 10: ACTIS setup coupled to FLD

An Agilent 6230 LC TOF MS was used with electrospray ionisation (ESI), as the organic MS detector. The instrument and scan source parameters parameter applied for all ACTIS-TOF-MS measurements are presented in Table 14. The ACTIS experiments were performed in positive mode. According to the molecular structure of quercetin, we assumed that the TOF-MS acquisition in negative mode would be more successful. However, the total ion content was very low in negative mode and no specific quercetin peaks could be determined in this mode. Therefore, the positive mode was selected for actual ACTIS experiments. The ACTIS-TOF-MS coupling is shown in Figure 11.

Table 14: Overview of TOF-MS method parameters

Instrument parameters		Scan Source Parameter	
Gas temperature (°C)	120	Nozzle voltage (V)	1000
Gas flow (L min ⁻¹)	10	Fragmentor voltage (V)	120
Nebulizer (psig)	35	Skimmer1 voltage (V)	60
Sheath Gas temperature	350	Octopole RF Peak (V)	750
Sheath Gas flow	11	Average Scans	1
Source Voltage (V)	+3500	Detection Window (ppm)	100
		Min Height (counts)	100

Compared to FLD, TOF-MS has a higher acquisition speed since the capillary content comes straight to ESI source. The wide m/z range of TOF-MS is beneficial for the application as ACTIS detector since it allows the observation of protein signals in theory.

After measurements of pure Q and FeQ_2 solutions in the concentration range of prepared BLG- FeQ_2 mixtures, the qualitative data analysis in MS Dial was done. This analysis yielded a list of relevant m/z values, associated with FeQ_2 complex. These m/z values were later used in MS Qual to extract the ion chromatograms out of total ion chromatograms originated from ACTIS measurements.

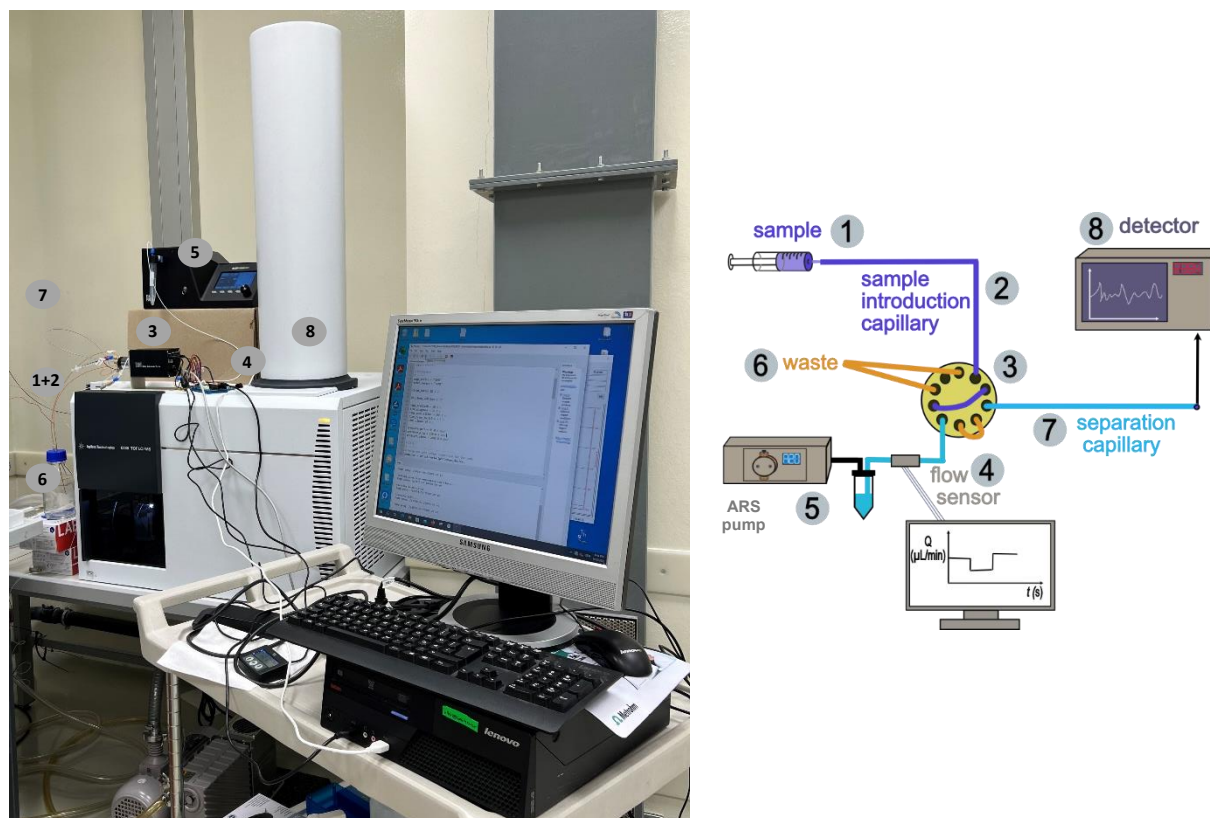


Figure 11: ACTIS-TOF-MS

An ICP-MS with collision/reaction cell (NexION 2000 from PerkinElmer) was utilized as an elemental detector. The acquisitions were performed in kinetic energy discrimination (KED) mode with He as collision gas with cell flow of 7 mL min^{-1} . The Rpq parameter was set to 0.4. The method optimization was performed by using a quality control solution containing 10 ng g^{-1} Fe in 2% HNO_3 . The perfluoroalkoxy (PFA) micro flow nebulizer ST-5898 from Perkin Elmer was used to convert the liquid sample into an aerosol, which was further introduced into the ICP-MS. Before each first measurement after device started up, plasma was warmed up for 15 minutes. All ACTIS-ICP-MS measurements were carried out in a clean room laboratory (ISO class 7) with the setup shown in Figure 12.

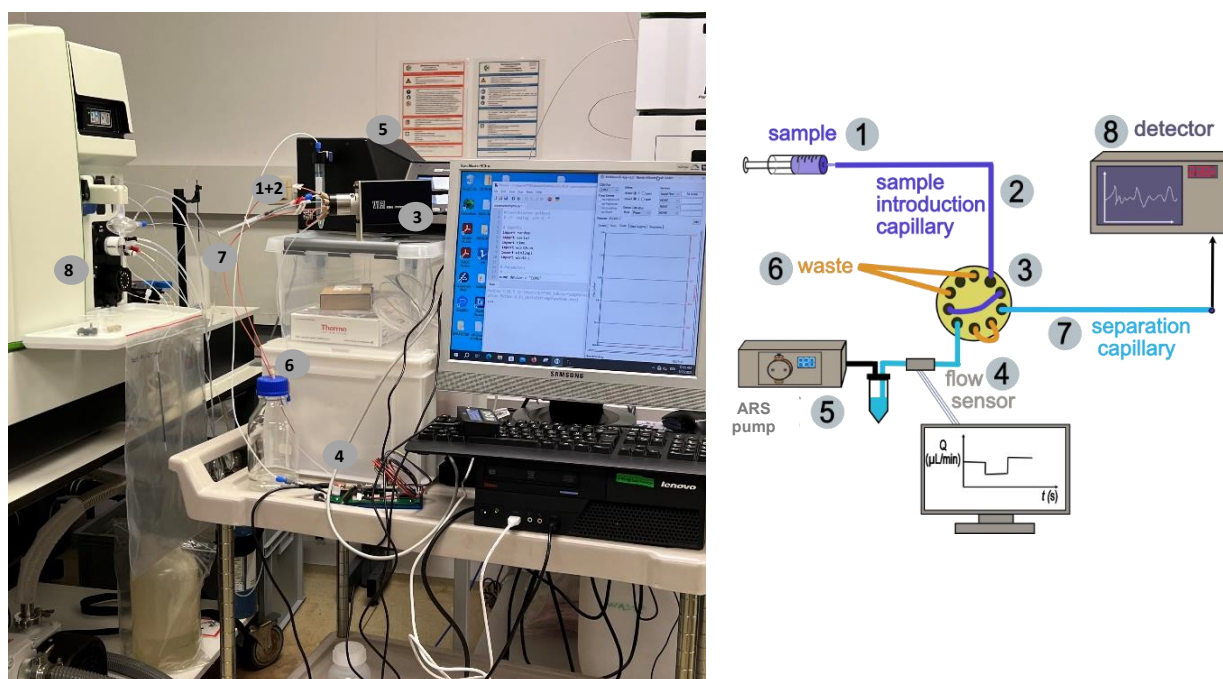


Figure 12: ACTIS-ICP-MS

The last detection method evaluated in this work was ICP-AES, for which the device AVIO 220Max from Perkin Elmer was used. The separation capillary was connected to a ST-9400 PFA microflow nebulizer from Perkin Elmer. The wavelength was set to 238.204 nm for Fe. Before each first measurement after device started up, plasma was warmed up for 10 minutes.

Since this ICP-AES was not designed for transient measurements, direct signal extraction over time was not possible in its software. Therefore, an additional PowerShell “hack” script was needed to copy the signal values and save them in separate text file. This “hack” script is given in the appendix, section 3.

2.5 Data evaluation

One ACTIS run result in a separagram. Depending on the employed detector, the intensity of compound signal as well as acquisition rate can vary. It is imperative that properties of the detector remain consistent for one ACTIS experiment. In the evaluation process the relative signal intensities among the mixtures are used to find K_d based on the principles explained in section 1.3.

The data evaluation can be performed in a calculation program such as Microsoft Excel. Alternatively, automated evaluation is possible by applying the prACTISed workflow; prACTISed is a collection of Python scripts which is designed for the analysis of ACTIS experimental data. [44]

In order to validate the prACTISed workflow results, we performed the data evaluation of initial experiments in Excel. The raw data was imported into Excel and replicates of one PC working solution were organized within one Excel sheet. Subsequently, individual diagrams were generated for each

mixture separately. These diagrams aided in selecting the appropriate cutting points to extract the compound peak for each measurement. It was required to adjust the peaks positions slightly, if the measurements were performed without using automACTIS. The adjustment involved the removing of datapoints prior the non-diffusive peak, to ensure that all the peaks have the same starting timepoint. When applying automACTIS, only slightly shifted peaks positions were observed due to minor changes of flow rates. In this case no peak time corrections were applied. Note that this might have introduced small errors in subsequent evaluation steps.

All peaks were cut and aligned, and the background was removed by subtracting the absolute intensity value at the starting region of each separagram. The next step involved the peak normalization to unity which was followed by averaging over all separagrams (from the same $[P]_0$). The averaged separagrams were used for further analysis. Initially, the τ_C was found as the time point where the mixture with lowest protein concentration reached its maximum. The signal value at determined τ_C were further used to find R_{exp} values, as shown in Equation (). The signals at the $t = \tau_C$ in other separagrams were used to find corresponding R_{exp} values. This resulted in one R_{exp} value for each measured working solution. The R_{exp} values were used to fit R_{theo} of each mixture by applying the Equation (10). Finally, the K_d value was determined as the fitting parameter of R_{theo} .

The described data evaluation workflow is time-consuming and prone to errors, particularly when handling larger data sets. The prACTISed workflow represents the set of open-source Python scripts which enable automated ACTIS data evaluation [44]. Raw separagrams were stored in .csv or .txt formats depending on the detector used. The data had to be compiled into an Excel input file consisting of a data worksheet for each working solution as well as a specific worksheet with experimental parameters such as flow rate and capillary dimensions. In this work, the aligned separagrams used for evaluation in Excel were copied into this input file. The width of the window for detection the corresponding signals at τ_C was set to 2%. For the data resulting from ACTIS-TOF-MS experiments, compensation procedure was applied. The compensation procedure refers to signal-unmasking of the compound which either can be suppressed or increased in the presence of protein.

The analysis of 60 separagrams took about 10 seconds using prACTISed. The output resulted in .xlsx working file containing all analysed separagrams, as well as graphical representation of separagrams and binding isotherm as PNG-files. The example of separagrams and corresponding binding isotherm is given in Figure 13.

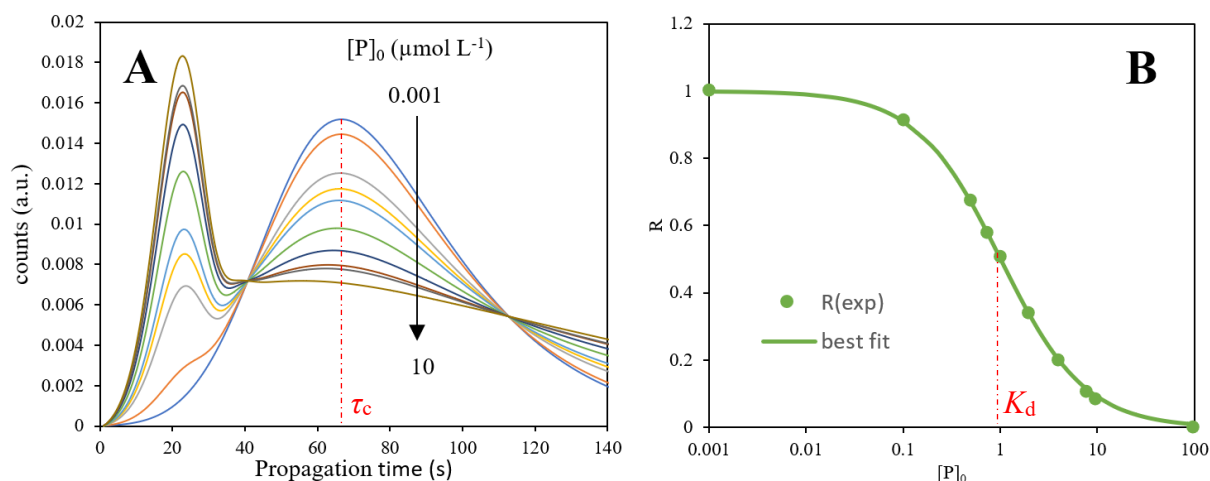


Figure 13: Example of resulting separagrams (A) and binding isotherm (B)

2.6 Computer simulations

To test the impact of the transfer capillary (nebulizer capillary) on the assessed K_d , the computer simulations were performed. For this purpose, the ElmerGUI program using Elmer FEM software for simulations of multi-physics problems was used [45]. The geometry of separation capillary connected to a transfer capillary was submitted as text file and the corresponding 2D mesh was constructed using gmsh.exe program. The example of geometry text file is given in appendix, section 4.

The radius (r_1) and the length (l_1) of the separation capillary and the radius (r_2) and length (l_2) of transfer capillary were selected to align with the real characteristics. In this work, one set of ACTIS virtual experiments was conducted with the variations of r_2 in the range of 50 - 1250 μm . In all virtual experiments, the inflow velocity (v) of sample plug was set to 0.029, the sample plug length (l_{sp}) corresponds to 10 % of l_1 . All input values were given in arbitrary units. The diffusivity of the compound (μ_c) was established at 5×10^4 , which corresponds to $500 \mu\text{m s}^{-1}$. The protein's diffusivity (μ_p) was set to 5×10^3 , which corresponds to $50 \mu\text{m s}^{-1}$. Experimental and simulation parameters are given in Table 15. We decided to exclude steady state in these simulations. The dimensions were scaled in x-direction (along the capillary) in order to save simulation time and to improve convergence.

Table 15: Real and simulated ACTIS – detector characteristics

characteristics	experimental	unscaled	simulation (scaled)
l_1	600 mm	600	3
r_1	0.25 mm	0.25	0.25
l_2	80 mm	80	0.8
r_2	0.05 mm	0.05 - 1.250	0.05 - 1.250
l_{sp}	5 mm	5	0.1

ν	346 mm min ⁻¹	346	0.029
μ_C	500 $\mu\text{m s}^{-1}$	500	5×10^4
μ_P	50 $\mu\text{m s}^{-1}$	50	5×10^3
Mesh size	-	-	0.01
Timestep interval	-	-	300
Timestep sizes	-	-	1

The geometry of the separation and transfer capillary with their mesh is presented in Figure 14.

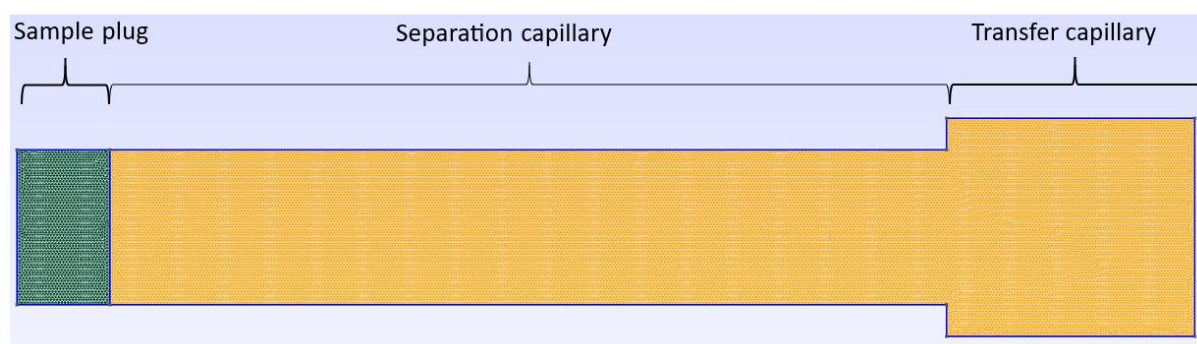


Figure 14: The geometry of separation and transfer capillary with integrated mesh used for computer simulations

Two simulations were carried out for each compound and the protein for every value of r_2 . This resulted in total of 20 simulations. Each simulation resulted in time-based compound concentration.

The evaluation of computer simulations involved following steps: 1) normalisation of the functions; 2) calculation of [PC], [P], and [C] for 10 different $[P]_0$ values; 3) calculation of coefficients for compound and protein functions for each $[P]_0$; 4) calculation of resulting functions of low and high diffuse functions by multiplication of normalized functions with respective coefficients; and 5) finding the K_d value by applying prACTISed algorithm. The evaluation resulted in 10 K_d values, for each r_2 value. For the calculation of [PC], [P], and [C], beside the 10 specified $[P]_0$ values, the value for $[C]_0$ and arbitrary K_d are also required. When selecting these values it is important to consider the criteria for $K_d/[C]_0$ to accurately assess K_d [31]. K_d was set to 1000 nmol L⁻¹ and the $[C]_0$ to 10 nmol L⁻¹. The range of $[P]_0$ included 10 concentrations from 1 to 2000 nmol L⁻¹.

3 Results and discussion

3.1 Validating ACTIS-setup with HSA-FLC model system

The initial experiments aimed at the validation of our ACTIS setup, testing its functionality, and its ability to accurately determine K_d value of a protein-metal complex. The functionality of the setup includes different aspects. First we wanted to ensure the absence of leaks in the valve, especially during experimental runs. Besides that, we wanted to achieve reproducible flow stability and sample transfer. We implemented data logging of the flow rate over time to assess the repeatability of ARS pump's performance and flow rate stability. In the context of ACTIS-FLD experiments, we considered consistent peak form during the separation step as an indicator of proper sample loading and transfer. Furthermore, the performance of the detector was evaluated based on the repeatability and reproducibility of the separation peaks in terms of their form and intensity. Finally, we confirmed the suitability of our setup for further experiments by K_d assessment of a model system comparable to one that had previously been investigated using ACTIS.

We chose HSA-FLC model system and FLD as appropriate detection method for evaluating our ACTIS setup. This decision was inspired by a similar ACTIS experiment, which was reported previously. Namely, a study which assessed bovine serum albumin (BSA) binding to FLC using ACTIS-FLD method yielded K_d of $28 \pm 6 \mu\text{mol L}^{-1}$ [31]. Since BSA and HSA are similar in terms of their binding affinities [46], we consider the comparison of the obtained results to be reasonable. An additional advantage of HSA-FLC model system is a relatively high expected K_d value (in $\mu\text{mol L}^{-1}$ range). Higher K_d allows higher $[C]_0$ in working solutions which improves the quantification with chosen detection method and the accuracy [47]. On the other hand, K_d in $\mu\text{mol L}^{-1}$ range refers to unspecific molecular binding. Therefore, deviations of observed K_d values are more likely compared to ones observed in highly specific molecular binding ($\text{pmol L}^{-1} - \text{nmol L}^{-1}$ range).

First experiment conducted aiming at the validation of our ACTIS setup included ACTIS-FLD measurements of pure FLC solutions. We prepared six solutions with [FLC] in range of $0.025 - 0.5 \mu\text{mol L}^{-1}$ and measured six runs per solution. Due to high fluorescence of FLC and good sensitivity of used FLD, intense signals were obtained in separation step of each run. Average maximal signals with corresponding standard deviations are given in Table 16. The corresponding standard deviations reveal excellent repeatability of peak intensity, particularly for [FLC] within the range of $0.025 - 0.1 \mu\text{mol L}^{-1}$.

Table 16: Average Peak Maximums and Standard Deviation of FLC measurements using ACTIS-FLD

[FLC] ($\mu\text{mol L}^{-1}$)	Average peak maximum (a.u.)	Relative standard deviation (%)
0.025	$8.6 \times 10^6 \pm 5.8 \times 10^5$	0.067
0.075	$2.4 \times 10^7 \pm 1.4 \times 10^6$	0.058

0.050	$1.6 \times 10^7 \pm 9.7 \times 10^5$	0.060
0.100	$3.4 \times 10^7 \pm 3.1 \times 10^6$	0.091
0.230	$7.5 \times 10^7 \pm 1.0 \times 10^7$	0.133
0.500	$1.1 \times 10^8 \pm 6.3 \times 10^5$	0.005

The calibration curve of fluorescein measured using ACTIS-FLD setup is illustrated in Figure 15. Considering the wide range of [FLC] measured and injection via ACTIS setup, we consider $R^2 > 0.9$ as acceptable. The resulting R^2 value of 0.9474 demonstrates a good level of linearity in this experiment. The FLC concentration of $0.05 \mu\text{mol L}^{-1}$ for HSA-FLC working solutions was selected for ACTIS setup evaluation.

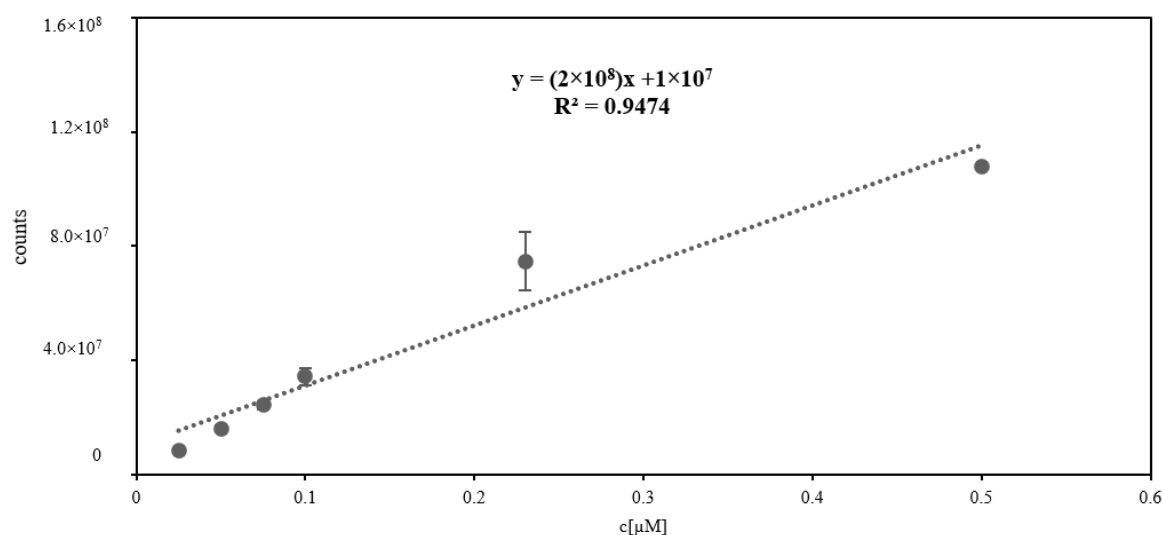


Figure 15: FLC calibration curve

After positive evaluation of the ACTIS-FLD instrumentation for measuring the FLC, the first ACTIS experiment was conducted. The primary objective was to determine if the measurements of HSA-FLC would mirror those of pure FLC from previous assessments. Therefore, only three runs per working solution were performed. In section 2.2.1, the preparation process of all mixtures analysed in the first ACTIS-FLD experiment is given.

Separation peaks cut from normalized average separagrams, as well as resulting binding isotherm are presented in Figure 16A and 16B. Since this was the first ACTIS experiment conducted in this work, we conducted the evaluation using both Excel and the prACTISed script. The evaluation using Microsoft Excel revealed a K_d value of $93.7 \pm 34.3 \mu\text{mol L}^{-1}$. The evaluation with prACTISed revealed a K_d value of $97.3 \pm 22.2 \mu\text{mol L}^{-1}$. Evaluated K_d value aligns with the one reported in the literature for BSA-FLC model system.

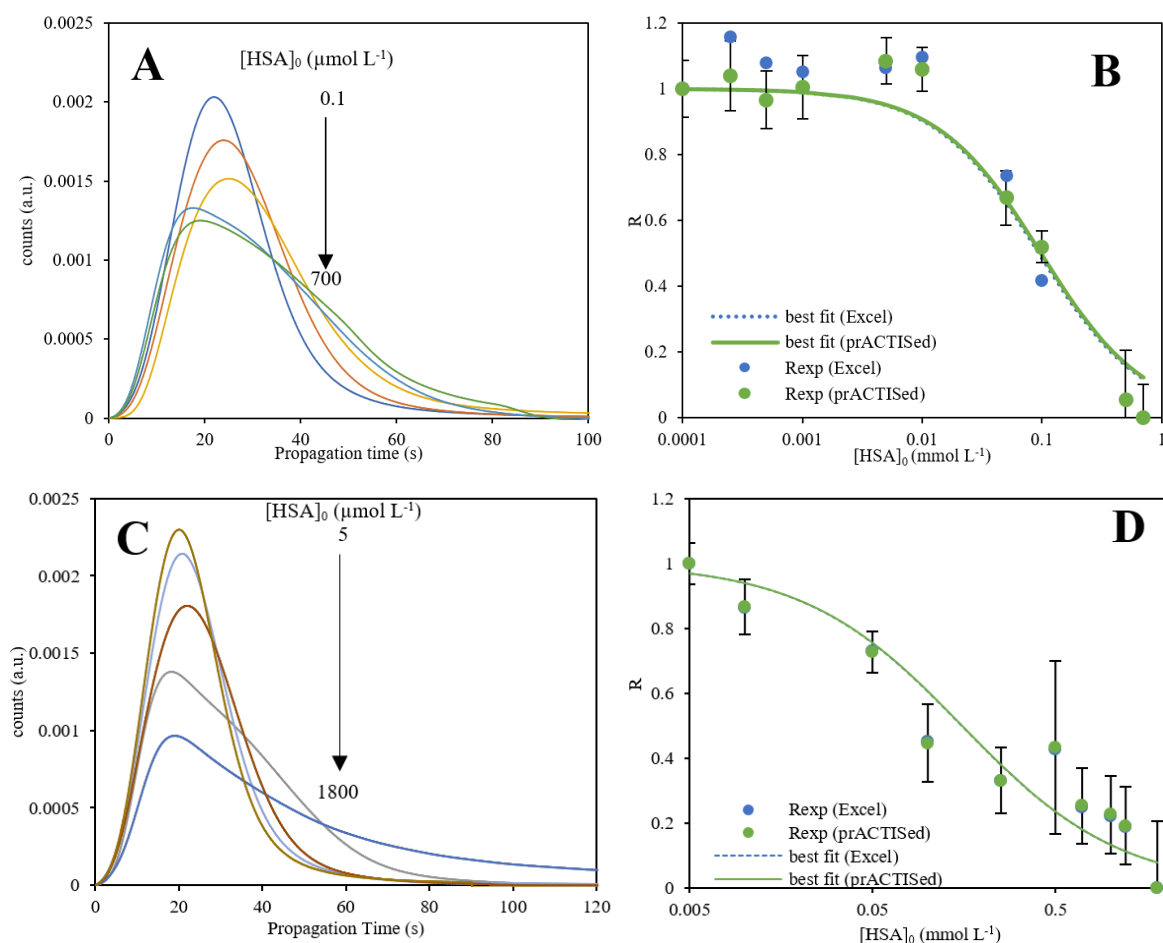


Figure 16: Separation peaks of five HSA-FLC working solution measured in the first ACTIS-FLD experiment (A) and the corresponding binding isotherm (B); Separation peaks (C) and binding isotherm (D) resulted from second ACTIS-FLD experiment of HAS-FLC.

The initial ACTIS-FLD experiment demonstrated good repeatability. As expected, with increased $[HSA]_0$, the form and intensity of the separation peak changed. The intensity of diffuse peak decreased and the frontal part of the peak enhanced with rising $[HSA]_0$ and constant $[FLC]_0$. This appearance validates the fundamental thesis of TIS. However, to determine K_d value of this system more precisely using ACTIS-FLD, a second experiment was conducted with an adjusted range of $[HSA]_0$.

Evaluation of second experiment (Figure 14C and 14D) using Excel gained K_d value of $153.4 \pm 40.2 \mu\text{mol L}^{-1}$ while prACTISed yielded K_d of $154.6 \pm 33.8 \mu\text{mol L}^{-1}$. Increasing of $[HSA]_0$ in working solutions affected the shift of binding isotherm and its deflection point to higher $[HSA]_0$. Consequently, we observed higher K_d value compared to first experiment.

Now let's discuss the differences of Excel and prACTISed evaluation approaches. The greatest difference between those two evaluation approaches lies in the width of the data points range used to determine τ_C . In Excel, only one data point was used to find R_{exp} . On the other hand, prACTISed found the R_{exp} as average from the data range of 2% width around the τ_C . Additionally, the calculation of the

standard deviation was also different. In Excel, the standard deviation values were found for each data point for each working solution separately. The gained standard deviation values were further used to find maximal and minimal K_d values. This calculation was performed analogously to the calculation of K_d value. Finally, the standard deviation of K_d was found as a difference between maximal and minimal K_d values. In prACTISed, the given standard deviation refers to the the precision of the linear regression fitting.

We are uncertain about which values are more in agreement with the real K_d value, but the wider window for signal detection applied in prACTISed might be advantageous comparing to picking a single value. With wider window, the average value is calculated and thus the eventual detection system fluctuations can be diminished. Taking into account all the differences in described evaluation approaches, we consider the gained K_d values similar. Therefore, to simplify and to speed up the evaluation process we decided to exclusively use prACTISed for assessing further experiments.

Both obtained K_d values in ACTIS-FLD experiments performed are in similar range of values compared to the reported value for BSA-FLC. As already mentioned, the dissociation constant in $\mu\text{mol L}^{-1}$ range indicates unspecific binding [46]. Additionally, the previously discussed (Section 2.4) flow cell volume of FLD has also negatively affected the precision of the gained results. Therefore, the obtained values are in agreement with reported value of $K_d = 28 \pm 35.8 \mu\text{mol L}^{-1}$ for BSA-FLC model system. We consider the conducted experiments validated the capability of our setup to conduct ACTIS-Experiments. The evaluation data resulting from both experiments is given in appendix, section 5.

3.2 Assessing the feasibility of BLG-FeQ₂ model system for ACTIS experiments

After successful evaluation of the ACTIS setup, we wanted to evaluate its applicability on a metal-protein model system. More specifically, this experiment was conducted to explore the fluorescence intensity, solubility, and stability of the selected model system within the evaluated ACTIS setup.

Our assumption was that the BLG-FeQ₂ is suitable for ACTIS-FLD assessment of K_d due to quercetin fluorescence. It is known that no fluorescence emission of quercetin in aqueous solutions occurs due to intermolecular interaction of quercetin polar groups with H₂O molecules [42]. However, binding to proteins leads to strong quercetin fluorescence. After testing different excitation and emission wavelengths, we found that the excitation at 423 nm and emission at 515 nm resulted in reproducible fluorescence signals.

After initial ACTIS-FLD measurements of $100 \mu\text{mol L}^{-1}$ quercetin solution in 30 mmol L^{-1} NH₄Ac, we observed insufficient solubility of the quercetin. Consequently, this led to nonrepeatable fluorescence intensity. After closer inspection of the injection capillary and connector, we noticed solid quercetin residuals. These residuals impacted the variations of the amount of quercetin injected. To address this

issue, varying amounts of NaOH solution were added to equal quercetin aliquots, aiming to determine the minimum NaOH concentration required for complete quercetin dissolution. We found that by adding 200 μL of the 1 M NaOH into 4.8 mL of 1 mM Q in 30 mmol L^{-1} solution, the complete dissolving of the quercetin occurs.

After solving the quercetin solubility issue, the preparation of the working solutions was done. According to the literature, K_d value of BLG-FeQ₂ system is approximately 0.11 $\mu\text{mol L}^{-1}$ [39]. For K_d value in this range, the ligand concentration should ideally be maximal 0.01 $\mu\text{mol L}^{-1}$. However, due to low fluorescence of quercetin, $[\text{FeQ}_2]_0$ of 50 $\mu\text{mol L}^{-1}$ was chosen for ACTIS experiments. The high component concentration implies that the conducted experiment was more similar to a titration, which means that the determined K_d will be close to $[\text{FeQ}_2]_0$ [32]. Nevertheless, since the primary goal of this experiment was to explore the properties of the BLG-FeQ₂ system and its suitability for ACTIS experiments, we ignored the unsuitable component concentration at this stage. The results of ACTIS-FLD measurements of BLG-FeQ₂ system are shown in Figure 17.

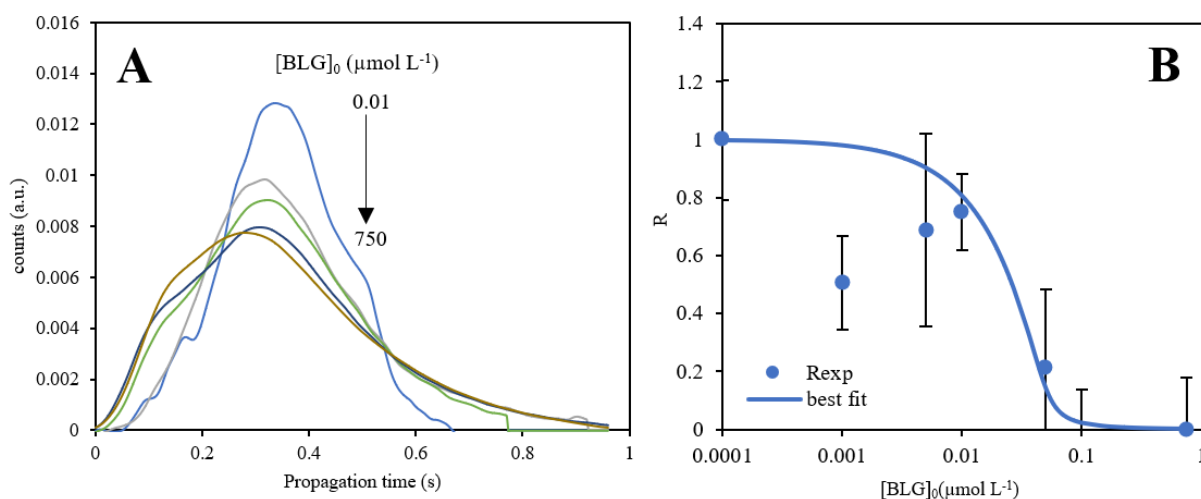


Figure 17: ACTIS-FLD measurements of BLG-FeQ₂ model system

The evaluation of the data yielded a K_d of $1.15 \pm 4.14 \mu\text{mol L}^{-1}$. The FeQ₂ concentration was constant in all measured working solutions. However, the signal intensity increased with increased $[\text{BLG}]_0$. This observation is in agreement with the previously discussed changes of quercetin's fluorescence depending on the binding state. Beside the inappropriate FeQ₂ concentration, this has also contributed to the high standard deviation. Evaluation data from this experiment is given in appendix, section 6.

Despite the high signal increase and consequently high standard deviation, the changed peak form with higher $[\text{BLG}]_0$ implies that the ACTIS assessment of K_d of BLG-FeQ₂ is possible. However, we expected that coupling ACTIS to another detector with higher sensitivity and specificity for FeQ₂ to be more successful.

3.3 Assessing K_d of the BLG-FeQ₂ model system

TOF-MS was selected as the detection method for the assessment of K_d of the BLG-FeQ₂ model system by ACTIS. A more precise and more sensitive technique compared to FLD should allow the assessing of accurate K_d value. Same as FLD detection, the TOF-MS compound detection is based on the quercetin signal. The unbounded Fe can not be directly detected with an organic MS method such as TOF-MS, since their m/z exceeds the lower limit of detectable m/z values of TOF-MS [47]. Additionally, the ESI source leads to soft ionisation and iron may not be completely ionised with it. However, we expected TOF-MS to detect FeQ₂ as an intact molecule or to find its fragments [48].

For the BLG-FeQ₂ model system, TOF-MS seems to be an excellent detector choice due to its low LOQ and LOD values. It is important to note that assessing of another metal-protein systems, with no organic molecule incorporated in the complex component, may not be possible by employing organic MS.

The reported m/z value for intact Fe(III)Q₂ complex obtained from ESI-TOF-MS analysis is 658.0049 [49]. According to molecular mass, this m/z value corresponds to [(2Q-H)Fe]⁺ ion. According to the same study references [49], depending on further quercetin fragmentation more m/z values are possible, such as: 640, 612, 602, 584, and 465. Notable, this study had different methodology. The FeQ₂ complex was dissolved in methanol to final concentration of 10 $\mu\text{mol L}^{-1}$. In our work, the relatively high concentration of NH₄Ac and BLG in the working solutions may complicate the identification of 658.0049 m/z value. To be more specific, the presence of multiple positive charges on the [(2Q-H)Fe]⁺ ion, or its association with NH₄⁺ and/or H₃O⁺ ions, can result in another more relevant m/z values for the specific FeQ₂ signal.

BLG-FeQ₂ working solutions were prepared with [FeQ₂] of 5.0×10^{-3} $\mu\text{mol L}^{-1}$ for both experiments. We considered this concentration accessible for TOF-MS measurements and optimal for assessment of K_d . After measurements of pure Q and FeQ₂ solutions in concentration range of prepared BLG-FeQ₂ working solutions, the qualitative data analysis in MS DIAL was done. We applied this algorithm on pure ARS and pure FeQ₂ measurements, aiming to identify the specific m/z for FeQ₂ complex. This analysis in MS DIAL yielded a list of relevant m/z values associated with FeQ₂ complex: 590.9913, 508.9935, 426.9877, 344.9857, 262.9821, 180.9781, 158.9960, and 140.0014. The listed m/z values were used later to extract the ion chromatograms out of total ion chromatograms originated from ACTIS measurements.

Two ACTIS-TOF-MS experiments were carried out on the BLG-FeQ₂ system. The change of total ion content (TIC) during one run indicated if the injection of the sample was done properly. The TIC variations correspond to respective ACTIS steps, as showed in Figure 18.

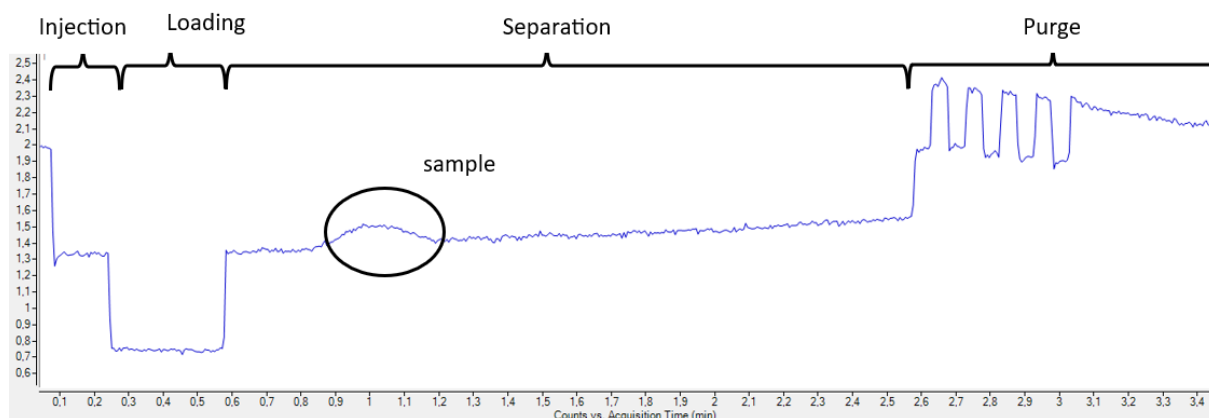


Figure 18: Total ion content (TIC) of one ACTIS-TOF-MS run

The separagrams were gained by extracting ion chromatograms from the TIC for each run. As previously mentioned, eight ions were selected for this purpose.

First experiment resulted in the separagrams and corresponding binding isotherm presented in Figure 19. In contrast to ACTIS-FLD, in ACTIS-TOF-MS signals of FeQ_2 decrease with increasing $[\text{BLG}]_0$. The reason for this appearance is the “masking effect” caused by increasing protein concentration. One possible explanation for the occurrence of the “masking effect” is that an increased production of protein fragment ions masks the relevant ions for ion extraction. Therefore, in the evaluation process using prACTISed, the compensation procedure was applied. For this procedure, the computer-simulated separagram of pure protein was necessary.

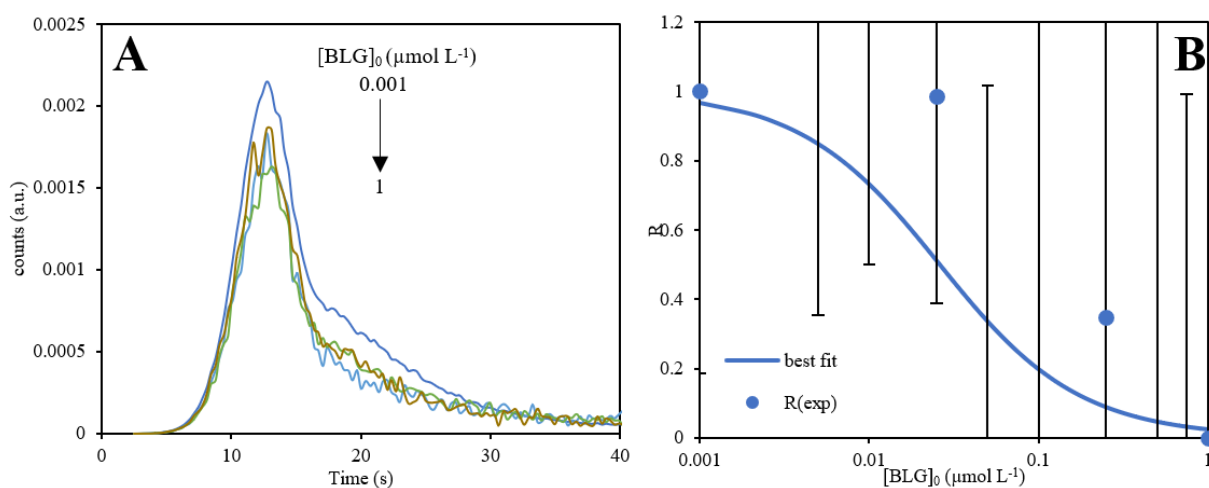


Figure 19: The results of the first ACTIS-TOF-MS experiment. A) The average separagrams of measured mixtures with different $[\text{BLG}]_0$; B) The resulting binding isotherm

Even though the compensation procedure proved to be an effective tool to reduce the “masking effect”, we decide to change the range of $[\text{BLG}]_0$ for the second experiment. The main motivation was to check if this effect will be the same and to test if the precision can be improved. The second ACTIS-TOF-MS

experiment yielded separagrams and binding isotherm presented in Figure 20. Evaluation data from both ACTIS-TOF-MS experiments are given in appendix, sections 7 and 8.

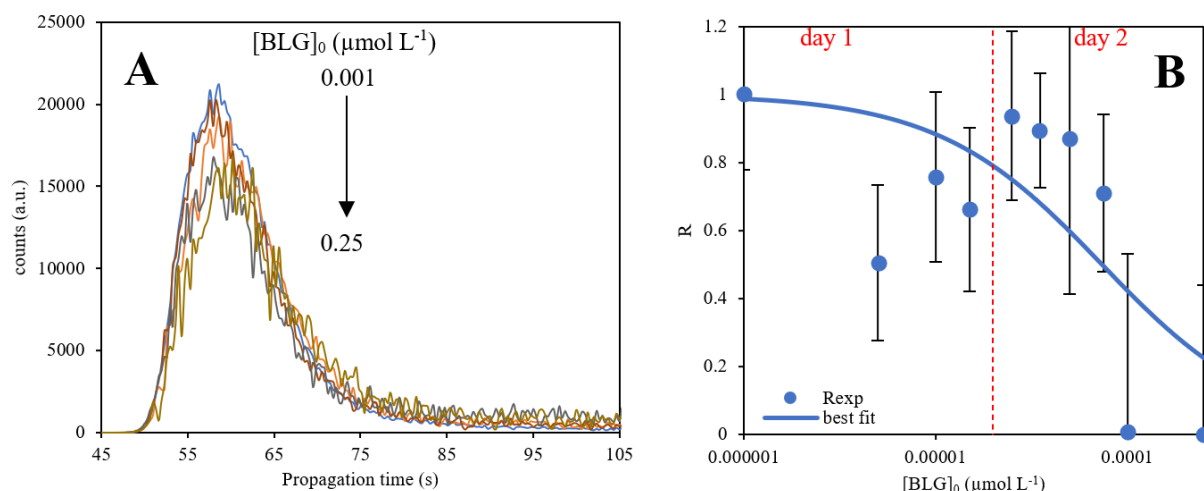


Figure 20: The results of the second ACTIS - MS -TOF experiment. The average separagrams of measured mixtures with different $[BLG]_0$ (A); The resulting binding isotherm (B).

K_d value assessed in the first experiment was $0.0235 \pm 0.0037 \mu\text{mol L}^{-1}$. The K_d value observed in the second experiment was $0.0709 \pm 0.0034 \mu\text{mol L}^{-1}$. The reduction of $[BLG]_0$ for the second experiment resulted in a higher K_d value. Closer inspection of the separagrams revealed that the separation peak intensity of the mixtures with the same initial $[BLG]_0$ is higher in the second experiment. For instance, the separagram of $[BLG]_0 = 0.05 \mu\text{mol L}^{-1}$ solution reaches its maximum at about 3,000 counts in the first and 18,000 counts in the second experiment. The similar trend is evident for all mixtures with the same $[BLG]_0$ measured in both experiments. Since the device tuning was performed between first and second experiments, this may have caused significant variations. However, since the normalization of the separagrams was done before the actual evaluation, this should not have significantly impacted the assessed K_d values.

Since the resulted distribution of the R values (Figure 18B) in second experiment was inconsistent, the fit of binding isotherm was predictably poor. Consequently, the standard deviation was high compared to gained K_d value. The measurements were performed over two days, namely four working solutions with lowest $[BLG]_0$ on the first and remaining solutions on the second day. The unusual R over $[BLG]_0$ distribution appears to be linked to changes in the day of measurement. Therefore, our assumption was that the TOF-MS conditions were different on each measurement day.

If this assumption is true, this inconsistency of R distribution would be the same for each m/z . Therefore, we checked each EIC for each m/z and found the same unusual R distribution. This distribution was independent of the normalization on the reference 922.0098 m/z . We did not apply

the compensation procedure during the evaluation to exclude the impact of simulated separagram. Resulting K_d values of corresponding m/z used for extraction are presented in Table 17 and Figure 19.

Table 17: K_d values gained by extraction of TICs after corresponding m/z value

m/z	590.9913	508.9935	426.9877	344.9857	262.9821	180.9781	158.9960	140.0014
K_d	0.0140	0.0153	0.0211	0.0213	0.0191	0.0171	0.0111	0.0224
Std. dev.	0.0088	0.0091	0.0111	0.0124	0.0111	0.0102	0.0076	0.0108

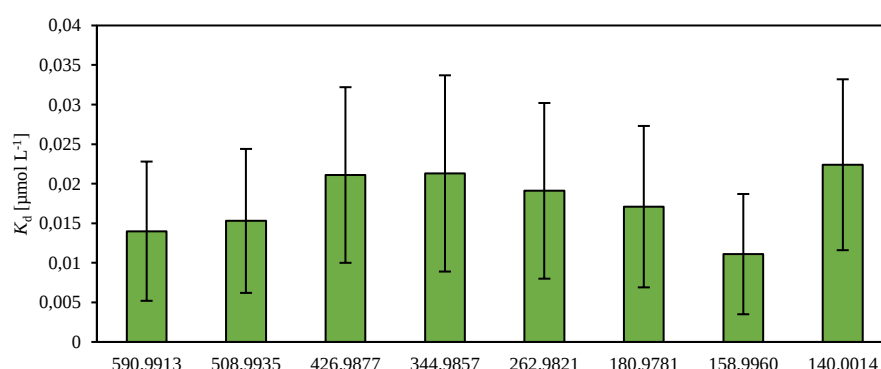


Figure 21: K_d values gained by extraction of TICs after corresponding m/z value

Resulting binding isotherms of all selected m/z values have similar R over $[BLG]_0$ distribution. Figure 21 represents binding isotherms of 140.0014 and 590.9913 m/z.

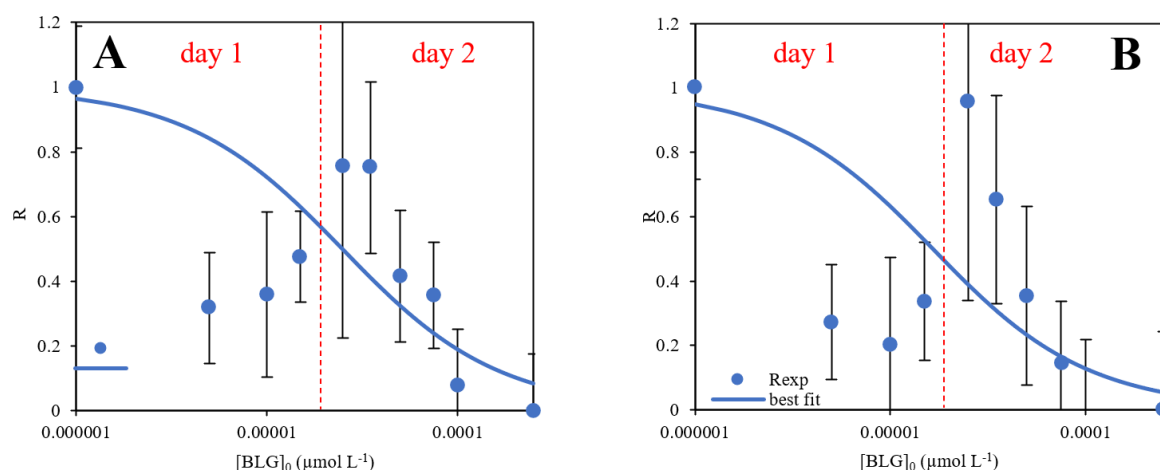


Figure 21: Binding isotherms resulted from TICs extractions after m/z = 140.0014 (A) and 590.9913 (B)

The reason for this unusual R distribution may lie in a device problem but more likely it is caused due to different measurement days and possible calibration of the device in between. To avoid this issue in the future, all measurement in frame of one ACTIS experiment should be performed on the same day in one session.

Despite many challenges in terms of precision and concentration limits, to the best of our knowledge, K_d values obtained with the ACTIS-TOF-MS technique represent the lowest values found for BLG-FeQ₂ complex. These values highlight the advantages and potentials of the ACTIS method. However, the determination of accurate K_d requires systematic studies and method optimization, which were beyond the scope of this work.

3.4 Exploring the application of ICP detection methods for ACTIS

ICP based detection methods are promising techniques for elemental analysis in combination with ACTIS. Particularly the assessment of the metal-protein binding may be achieved by metal detection over the time. ICP is widely used as ionization source in ICP-MS and as excitation source in ICP-AES [50]. The main advantages of ICP based detection techniques are high sensitivity and possibility to couple the instrument with ACTIS setup. These properties may play a crucial role in accurate assessment of K_d .

However, some ICP methods are not intended to perform transient measurements. For instance, sensitivity of ICP-AES and ICP-MS are related to area-based evaluation of the time-dependent signal. This represents a disadvantage for the application as an ACTIS detector because the transient evaluation is a crucial requirement for ACTIS. On the other hand, the optimization of measurement parameters may improve its ability to measure transient signals more precisely.

To explore the applicability of ICP-MS and ICP-AES for ACTIS experiments, we used the BLG-FeQ₂ model system. In contrast to previously performed ACTIS-FLD and ACTIS-TOF-MS, the detection of the compound was based on Fe detection here. The main goal of these experiments was to assess the compatibility of the specified detection methods with ACTIS. In addition to this, the optimal Fe concentration for ACTIS working solutions which can be accurately detected with these techniques should be estimated. Furthermore, the evaluation of impact of Fe binding to Q and to BLG on the Fe signal is also a part of these experiments.

ACTIS-ICP-MS

To test the background of Fe, the ARS (30 mmol L⁻¹ NH₄Ac; pH=7.2) was prefilled in ACTIS setup and injected as a sample. In addition to this, the same ARS was also directly injected into the ICP-MS. The average of three measurements each showed similar noise level calculated as $3.5 \times \text{Std. dev.}$, as well as similar intensity of about 150 counts. These results are given in appendix, section 9.

When we directly injected pure 5 $\mu\text{mol L}^{-1}$ Fe solution, made by diluting the Fe II stock solution with ARS, unusual peaks appeared. We observed signal fluctuations and many spikes up to 2×10^5 counts. Results of three measurements are presented in Figure 22A. Our initial assumption was that the iron may not remain stable at the pH of 7.2 and the precipitation in solution causes huge signal fluctuations.

However, no precipitation was observed in either the stock solution or any of the analysed solutions. Very high noise level and considerable signal fluctuations indicated that the solution may have an issue.

To test this assumption, we prepared another $5 \mu\text{mol L}^{-1}$ Fe solution analogously to previous one. However, a different stock solution was used for the preparation in this case. The key difference of this stock solution compared to Fe II stock solution, was in its preparation - diluting Fe in sub-boiled H_2O with 2% HNO_3 and 0.1% HCl . This stock solution is further denoted as “new stock solution”. The signals obtained after direct injection of this $5 \mu\text{mol L}^{-1}$ Fe solution showed reduced signal fluctuations (Figure 22B). This led us to conclusion that the solvent used to prepare the stock solution play a crucial role in the Fe measurement with ICP-MS.

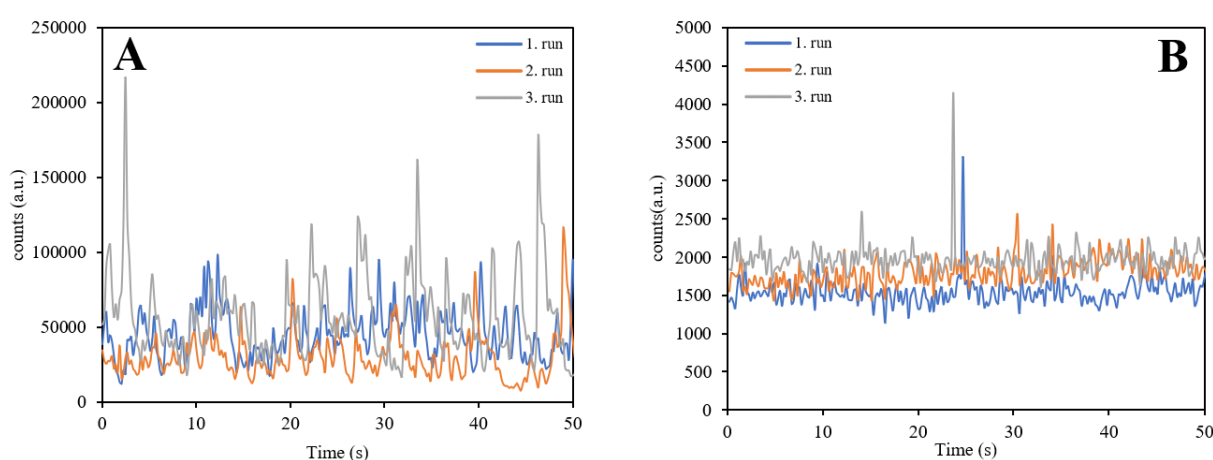


Figure 22: Three direct injections of $5 \mu\text{mol L}^{-1}$ Fe solution made by dilution of Fe II stock solution with 30 mmol L^{-1} NH_4Ac solution with $\text{pH} = 7.2$ (A); Three direct injections of $5 \mu\text{mol L}^{-1}$ Fe solution made by dilution of 1000 ng g^{-1} Fe stock solution with 30 mmol L^{-1} NH_4Ac solution with $\text{pH} = 7.2$ (B). The stock solution was prepared in sub-boiled H_2O with 2% HNO_3 and 0.1 % HCl .

The possible explanation for these differences might be the pH value. It is known that iron hydrolysis occurs in the aqueous solution depending on the pH value [51]. At higher pH, the hydrolysis process is more pronounced due to higher availability of OH^- ions. The hydrolysed Fe species can aggregate and especially at higher pH form various polynuclear complex polymers. The presence of Fe aggregates might explain the spikes observed during the measurements of Fe solutions made from stock solution with NH_4Ac . The lower pH and high concentration of NH_4Ac might result in dissolved polynuclear complexes.

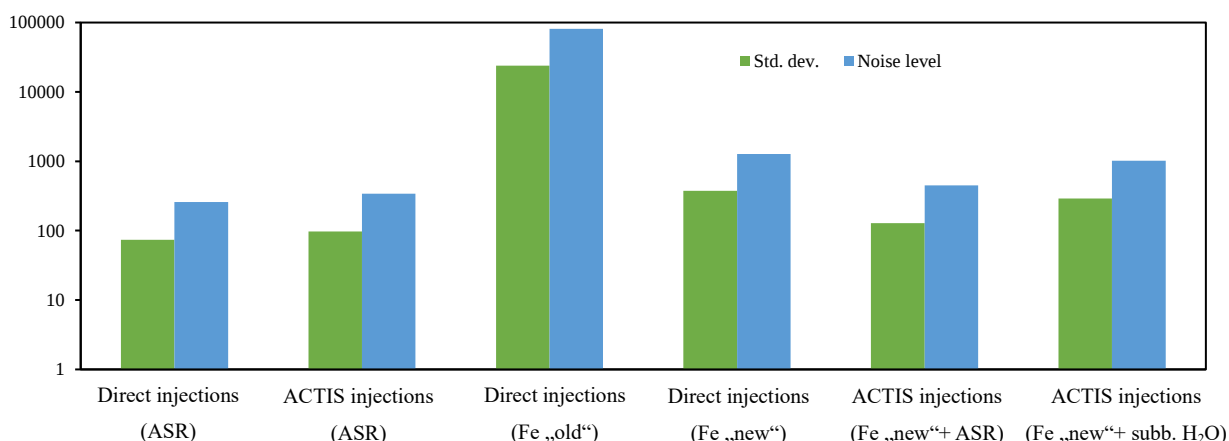


Figure 24: Standard deviations and noise calculated for different direct and ACTIS injections of NH_4Ac and Fe solutions. “Old” refers to Fe solution made by diluting Fe II stock solution and “new” refers to 1000 ng g^{-1} Fe stock solution made by diluting Fe in the 2% HNO_3 and 0.1 % HCl. The number values are given in appendix, section 9.

The standard deviations and noise calculated for different injection of NH_4Ac and Fe solutions are presented in Figure 24. The noise of the measurements of NH_4Ac injected directly or via ACTIS is comparable. The 1.3 times higher noise in the NH_4Ac signals when injected through ACTIS is caused due to longer time for transfer to ICP-MS through ACTIS setup compared to direct injections through autosampler needle. As discussed before, solutions of same [Fe] cause different noise levels depending on solution used in preparation of stock solutions. 30 mmol L^{-1} NH_4Ac with $\text{pH}=7.2$ in stock solution cause 60-times higher noise level comparing to sub-boiled H_2O with 2% HNO_3 and 0.1% HCl.

Iron is a one of the most abundant metals found in fine atmospheric particles [52]. The valve itself contains iron internally. Additionally, polyatomic interferences such as $^{40}\text{Ar}^{16}\text{O}^+$ and $^{40}\text{Ca}^{16}\text{O}^+$ can increase the background signals despite the KED mode applied [53]. Based on this data, we consider a background signal of around 150 counts without Fe in NH_4Ac solution added, acceptable.

Even though the $5 \text{ } \mu\text{mol L}^{-1}$ Fe solution made from stock solution with sub-boiled H_2O with 2% HNO_3 and 0.1% HCl is theoretically not suitable for our working solutions for assessment of BLG- FeQ_2 , we wanted to test if this solution can be potentially measured using ACTIS. Therefore, this Fe solution was injected into ICP-MS through ACTIS setup and the corresponding separagram is presented in Figure 23A. In addition to this, the same stock solution was diluted with sub-boiled H_2O to reach the same concentration and injected via ACTIS (Figure 23B). Notable, in all ACTIS runs, the 30 mmol L^{-1} NH_4Ac with $\text{pH}=7.2$ was employed as an ARS.

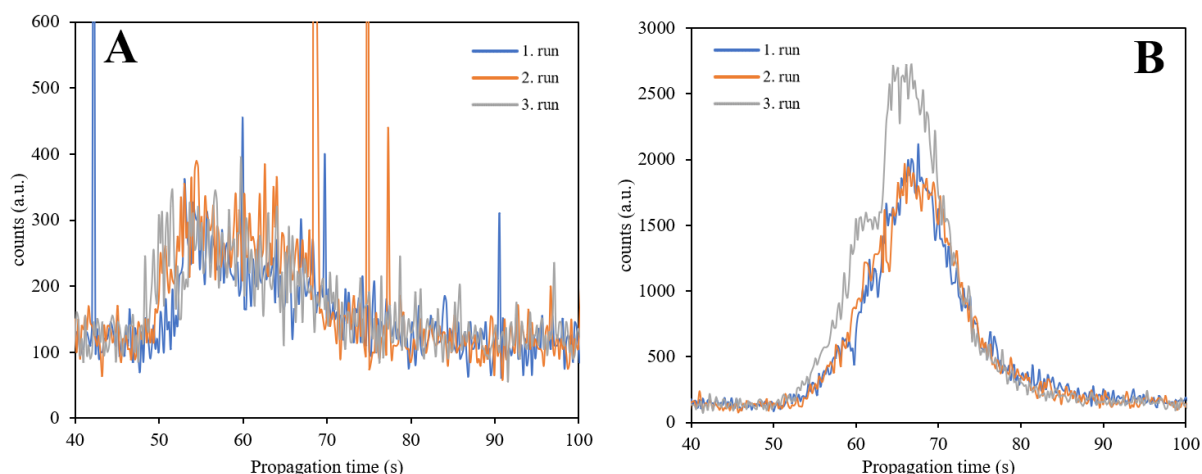


Figure 25: Three ACTIS runs of $5 \mu\text{mol L}^{-1}$ Fe solution, made by diluting Fe stock solution in sub-boiled H_2O , 2% HNO_3 and 0.1% HCl with the NH_4Ac (A). Due to high signal fluctuations, the y-axis is reduced here to better observe the signals. The whole signals are given in appendix, section 8; Three ACTIS runs of the $5 \mu\text{mol L}^{-1}$ Fe solution made by diluting Fe stock solution in sub-boiled H_2O , 2 % HNO_3 and 0.1 % HCl with the sub-boiled H_2O (B) The corresponding noise levels are given in Figure 22

The ACTIS-ICP-MS measurement presented in Figure 25 revealed that not only the solvent in the stock solution but also the solvent used for preparing of working solutions affects outcoming signals strongly. We see that the NH_4Ac suppress the signals up to 5 times compared to signals of solutions made with sub-boiled H_2O . Beside the lower intensity, the NH_4Ac solution exhibits much more single distinct peaks, which potentially suggest the presence of Fe agglomerates. The noise is similar in both cases (Figure 22), but the signal-to-noise level is much better in the second case.

In all ACTIS-ICP-MS runs in the time range when the rinsing step occurs, including valve switching, we see that the distinct peaks are more frequent. This appearance is analogous to the signals in purge steps observed in ACTIS-FLD and ACTIS-TOF-MS techniques. However, good repeatability of the measurements supports the idea that the chosen purge time is acceptable for this technique.

The conducted experiments have shown that the coupling of ACTIS to ICP-MS theoretically can be used for the assessment of the metal-protein binding. We found that the preparation of stock solution as well as choice of the solvent play a crucial role for the Fe signal intensity and signal-to-noise ratio. For instance, the Fe concentration of $5 \mu\text{mol L}^{-1}$ is too low for the accurate measurements if the NH_4Ac is used as a solvent. If the H_2O is used as a solvent instead, even lower Fe concentrations might be considered for the ACTIS working solutions. Our assumption is that the pH value causes the forming of the Fe polynuclear complexes, which further cause higher signal fluctuations. The solvent for our ACTIS experiments was done according to optimal conditions for BLG-FeQ₂ complex. However, the conditions needed for stabile iron in solutions are different. These are important parameters that need to be studied more thoroughly to adjust this model system for ACTIS-ICP-MS assessment. However, this was beyond the scope of this study.

ACTIS-ICP-AES

To test the applicability of ICP-AES as a detector for ACTIS measurements, we first analysed the NH_4Ac solution (30 mmol L^{-1} ; $\text{pH}=7.2$). The initial measurement performed to test this technique was the ICP-AES measurement of the pure NH_4Ac solution. The obtained Fe signals in NH_4Ac solution injected through ACTIS injections into ICP-AES are presented in Figure 26.

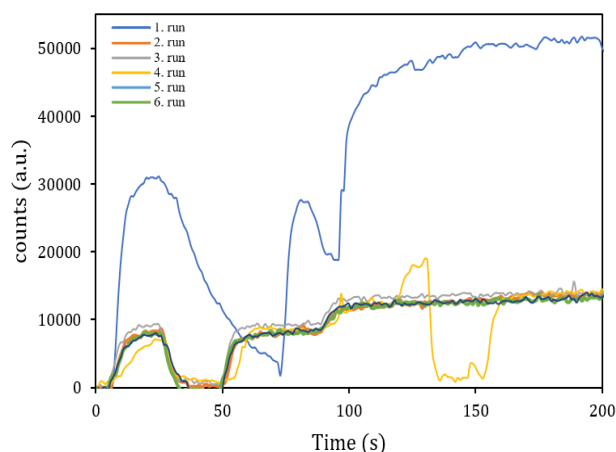


Figure 26: Six ACTIS-ICP-AES runs of NH_4Ac solution injected as a sample. The wavelength was set to 238.204 nm for Fe

Among the six measurements, two showed variations in forms and intensity, namely the first and the fourth run. It is important to highlight that during these measurements a syringe pump was used instead of pressure pump and no flow sensor was utilized. Consequently, these deviations may have been caused due to potential flow rate problems.

Even if we ignore the repeatability issue, it becomes evident that the signal intensity is significantly influenced by the flow rate of injected solution. With the flow rate of about $68 \mu\text{L min}^{-1}$, the background signal stabilizes at around 10,000 counts. With the constant flow rate, the signals are steady but when the flow rate is changed, the signal also changes immediately. For example, after valve switch between sample loading and separation step, the signal takes 6 seconds to reach its stable value.

Despite the low repeatability of the Fe signals, we decided to explore the effects of Fe concentration on them. Therefore, Fe solutions of $0.01 \mu\text{mol L}^{-1}$, $1 \mu\text{mol L}^{-1}$, and $10 \mu\text{mol L}^{-1}$ were injected into ACTIS-ICP-AES. The repeatability of these measurements was poor. Three of four runs of $10 \mu\text{mol L}^{-1}$ solutions and only four of six runs of $1 \mu\text{mol L}^{-1}$ solutions showed similar signal intensity. In contrast to this, all four measurements of $0.01 \mu\text{mol L}^{-1}$ Fe solutions were similar.

To be able to compare the effects of different Fe concentrations, we decided to consider only the measurements which resulted in similar intensity and shape ($\pm 10\%$ variations). The similarity was checked after normalisation of each separagram. All normalised measurements are added in appendix, section 10. The separation step was cut and normalised to surface of 1. Due to high dependency of the signal on the flow rate, an alignment of the base lines became necessary. We used a linear function

defined by the points marking the start and the end of the separation peak for the alignment. More precisely, the y-values calculated from the resulting function were subtracted from the signal values. The averages of aligned separation peaks are presented in Figure 27.

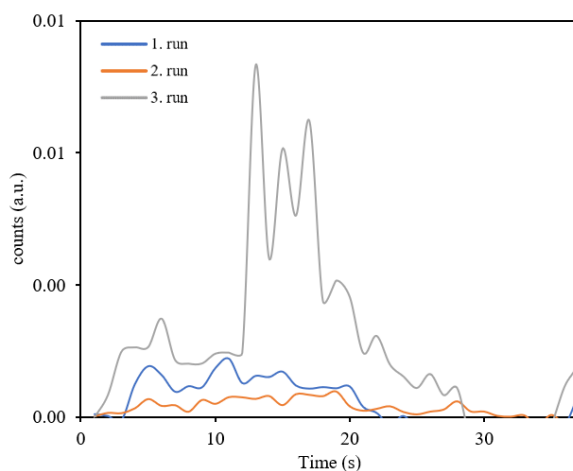


Figure 27: Average signals of normalized separations steps of similar $0.01 \mu\text{mol L}^{-1}$, $1 \mu\text{mol L}^{-1}$, and $10 \mu\text{mol L}^{-1}$ measurements

In contrast to $0.01 \mu\text{mol L}^{-1}$ and $1 \mu\text{mol L}^{-1}$, $10 \mu\text{mol L}^{-1}$ Fe solution exhibit peaks during the separation step (Figure 25). Three peaks observed in $10 \mu\text{mol L}^{-1}$ Fe solution are very narrow and consist of only few signals, but the peak shape resembles to the flow injection peaks observed in ICP-MS. Namely, the sharp rise and flatter descending are characteristic for ACTIS-ICP-MS injection peaks (Figure 25). However, it is very complicated to determine the time length of this signal.

To check if the Fe binding in BLG-FeQ₂ complex will affect the ACTIS separagrams, we decided to measure BLG-FeQ₂ working solutions. Fe concentration of $1 \mu\text{mol L}^{-1}$ was selected for BLG-FeQ₂ working solutions. Even though no Fe signals were observed when injected into ACTIS-ICP-AES, using this concentration enabled us to directly assess whether binding to Q or BLG would alter the absence of Fe signals.

10 working solutions of BLG-FeQ₂ were prepared and only one run per mixture was performed. All the aligned peaks were normalized to the surface value of one. The Figure 28 displays peaks gained by correction of whole separation step with the linear function. The solutions with [BLG]₀ of $0.25 \mu\text{mol L}^{-1}$ and $50 \mu\text{mol L}^{-1}$ exhibited separagrams with significant deviations. They are not presented here to allow for a clearer observation of other separagrams, but they are given in the appendix, section 10.

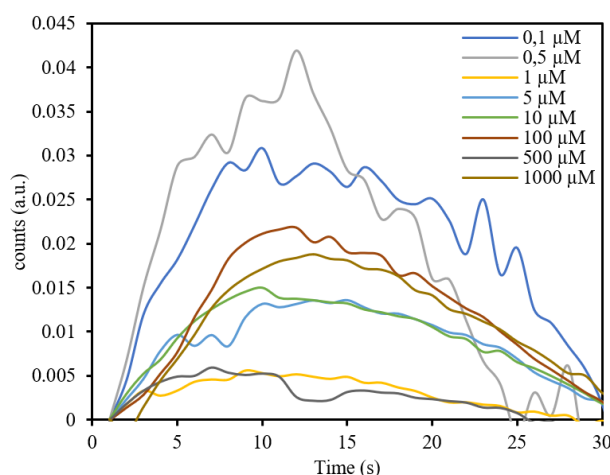


Figure 28: Aligned and normalized separagrams of 8 different working solutions measured using ACTIS-ICP-AES

The different $[BLG]_0$ in working solutions caused different slopes of the separation peak. Since the same flow rate was used for all performed runs, the changes of the slope implicate that the binding of FeQ_2 to BLG affects it.

The increased stability of the Fe in ASR caused by the binding to Q may explain this appearance. It is known that the complexation of Fe in extraction process with chelating agents having a high affinity for Fe can improve its determination [54]. To the best of our knowledge, there have been no studies investigating how the binding of iron to another molecule can affect its quantification by ICP based techniques. Based on performed experiments, the binding to Q and BLG improves iron detection. However, further studies are necessary to validate this observation and more importantly to eliminate the potential influence of flow rate on the signals.

It is evident that the increasing of the $[BLG]_0$ caused the general reduction in maximal signal intensity and changed separagram forms (Figure 28). This pattern is not the same across all mixtures. For instance, the maximum of working solution with $[BLG]_0 = 0.5 \mu\text{mol L}^{-1}$ is higher than the maximum of working solution with $[BLG]_0 = 0.1 \mu\text{mol L}^{-1}$ mixture, yet the trend remains evident.

The prACTISed evaluation of gained separagrams yielded K_d of $0.208 \pm 0.5 \mu\text{mol L}^{-1}$. This value is in the same range as K_d yielded from ACTIS-TOF-MS measurements for this model system. However, since only one run per working solution was performed and by strong signal dependence on flow rate, we would not consider gained results as accurate and precise. Despite that, the reduced signal intensity with increased $[BLG]_0$ proves the possibility of K_d assessment using this method. The evaluation data is given in appendix (section 10).

The fluctuations in the Fe signal, even at the constant flow rate, cannot be explained by the apparent impact of the flow rate. This leads us to consider the potential influence of the nebulizer configuration. As already mentioned, μ flow nebulizer was used for both ACTIS-ICP-MS and ACTIS-ICP-AES methods.

As the nebulizer is positioned between the separation capillary and the actual detection, the length and geometry of the nebulizer may affect the characteristic flow profile. In order to further explore the impact of the transfer capillary on the characteristic flow profile and consequently the accuracy of the K_d , computer simulations were performed.

3.5 Exploring the detector transfer capillary effects

One of the key advantages of ACTIS is its foundation in a deterministic process. The deterministic process can be computer-simulated, which allows the assessing of K_d in silico. These simulations can be used to evaluate the accuracy of performed ACTIS measurements, but also to examine the influence of physical factors on K_d accuracy. In order to understand the complexity of coupling ACTIS to ICP-AES, computer-simulations provide a valuable opportunity.

The linkage of ACTIS to a detection system is carried out through direct connection of the separation capillary to the detection system. The form of the detector injection system (nebulizer transfer capillary) can possibly have an influence on the K_d accuracy. Depending on the length and the width of the transfer capillary, the form of flow profiles may change after the transition of sample from separation capillary to detector. For example, introduction of the sample from ACTIS to ICP-AES includes the transition from separation capillary through the connector into a nebulizer. The inner radius of nebulizer capillary as well as its length can vary depending on a model used. In order to explore if the sample flow profile and consequently the K_d accuracy are affected by the transfer capillary inner radius, the computer simulations were employed.

Nine different inner radius of transfer capillary were tested using computer simulations. Alignment of the obtained separagrams was necessary due to variations in the starting time points. The shift in peak start positions is emerged due to lower mesh and time resolution with increasing nebulizer radius. The aligned and normalized separagrams of pure PC complex and pure C are displayed in Figure 29.

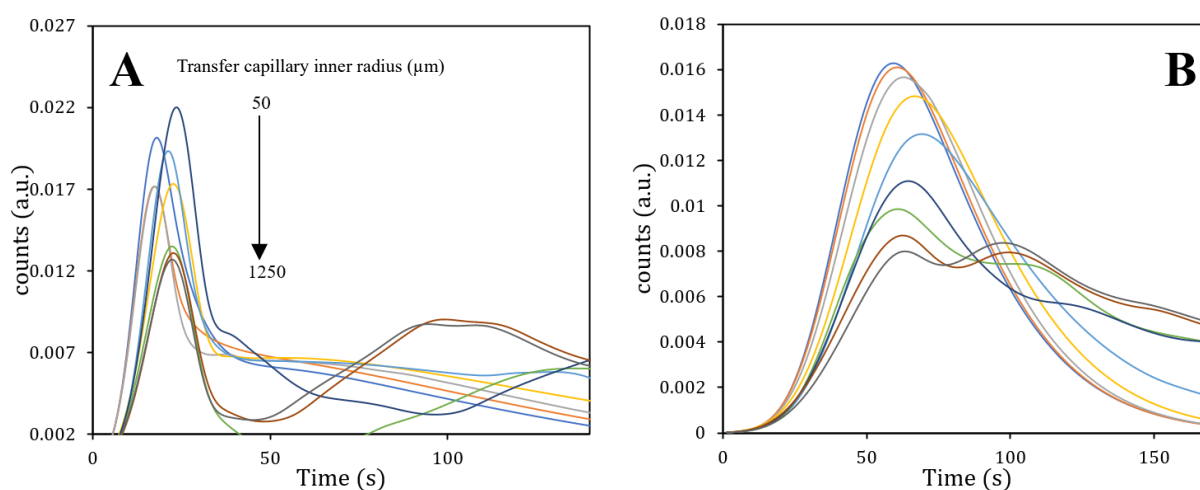


Figure 29: Separagrams made by computer simulations for PC (A) and C (B)

The lower diffusivity of PC complex caused more narrow peaks which arise earlier compared to the low diffusive C peaks. In the simulated separagrams an observable effect is that an increased inner radius decreases peak intensity while simultaneously raising post-peak signals. This signal changes suggest that the later portions of the PC flow profile spent more time in the wider nebulizer and therefore elute later. This caused lower intensity of the initially eluted molecules. The similar trend is observed in the separagrams for high diffusive C.

Let's examine the appearance of the separagrams of systems with both PC and C. Figure 30 represents the separagrams of both extremes, 50 and 1250 μm nebulizer diameter. These separagrams illustrate the negative effects of the wider transfer capillary. Due to higher signals of later portions of molecules in a flow profile, the diffusive peak is strongly reduced and the new, third peak is formed. Additionally, the dynamic range is reduced about 30% with wider transfer capillary.

Furthermore, a wider nebulizer results in a broader and more intense PC peak at the front of the flow profile. The black arrows clearly show how the working range is reduced in the wider transfer capillary.

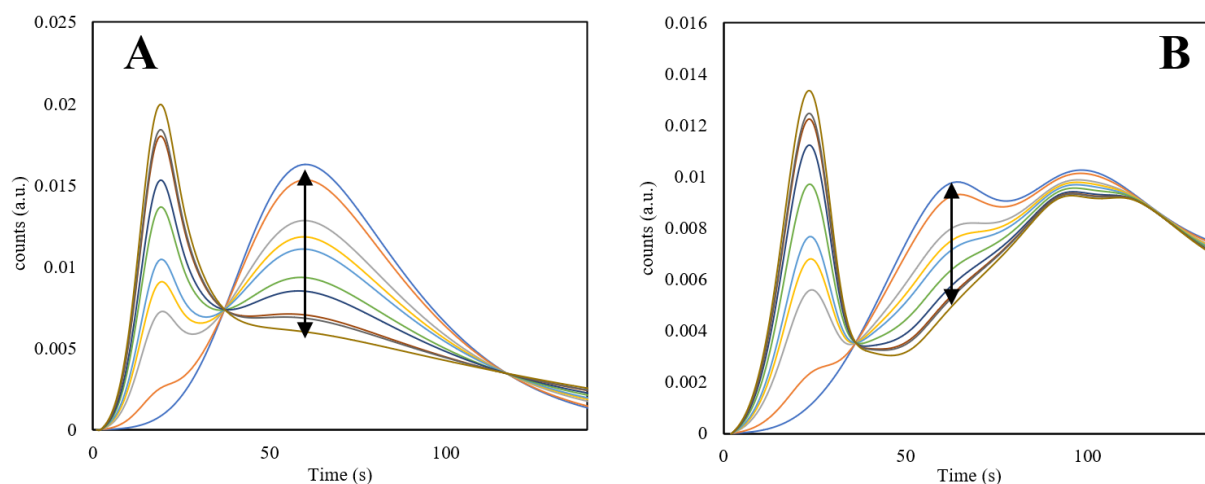


Figure 30: Normalized separagrams for transfer capillary inner radius of 50 μm (A), and 1250 μm (B) and corresponding working range

To estimate the influence of transfer capillary inner radius, the normalized separagrams for each tested nebulizer inner diameter, were put into the prACTISes for the assessing of the K_d values. The assessed K_d values as well as respective standard deviations are displayed in Figure 31. Separagrams and corresponding binding isotherms are given in appendix, section 11.

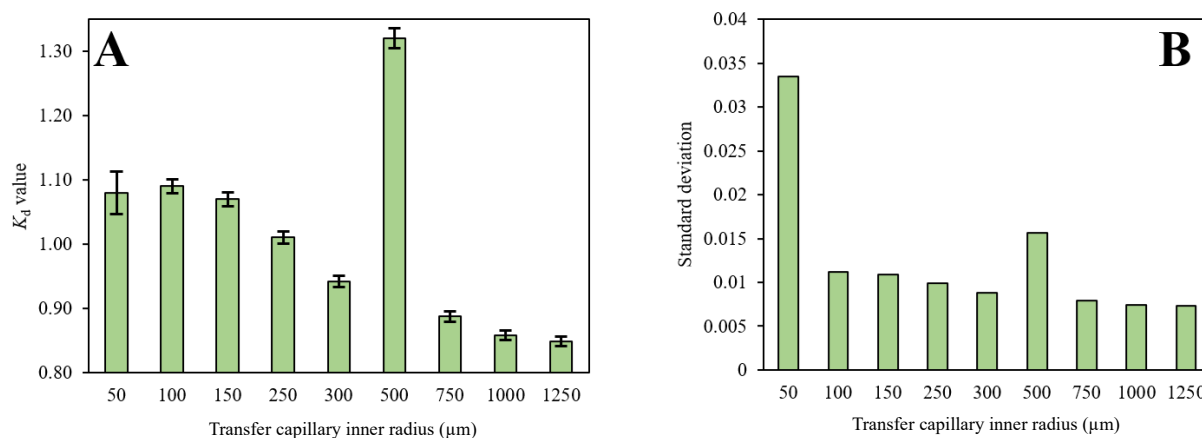


Figure 31: K_d values (A) and respective standard deviations (B) resulted from computer simulations.

K_d value which was used to calculate the R and the separagrams was set to 1 $\mu\text{mol L}^{-1}$. Therefore, the simulations of ideal transfer capillary inner radius should result in this value. Notably, the nebulizer inner radius of 250 μm gave the closest value to the expected one. The inner radius of the separation capillary was set to 250 μm in all simulations. This implicates, that the most accurate K_d value can be assessed if the nebulizer inner radius matches the separation capillary inner radius. With the exception of the 500 μm transfer capillary radius, assessed K_d values as well as corresponding standard deviations decrease with increasing the nebulizer inner radius (Figure 31). This result is in agreement with the observation of the separagrams, which showed lower values and lower changes of the diffusive peak intensity with wider transfer capillary radius.

In order to explore the effects of noise on resulting K_d values, we added noise to the separagrams of 50, 250 and 1250 μm simulations. The added noise (10-15 s/n) was comparable to the noise observed in conducted ICP-AES and ICP-MS measurements (14 s/n). A random number in range from -0.001 to 0.001 was added to every signal in each simulated separagram. Subsequently, separagrams were normalized and evaluated using prACTISed. The resulting K_d values and corresponding standard deviations are given in Figure 32. Further data is given in appendix, section 12.

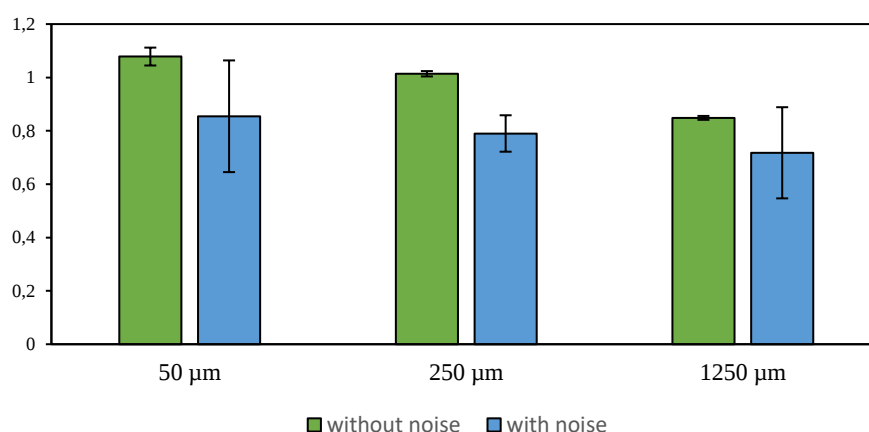


Figure 32: K_d values and corresponding standard deviations of noise-modified and original separagrams for transfer capillary inner radius of 50, 250, and 1250 μm

We see that noise greatly affected the accuracy of gained results independently of transfer capillary inner radius. On the other hand, the standard deviation is lowest for the inner radius of transfer capillary matching the inner radius of separation capillary (250 μm). A requirement for accurate K_d assessment is a high s/n ratio. Based on these simulations, we recommend at least 10 s/n ratio. The computer simulations have shown that the matching inner radii of separation and transfer capillary yield in the most accurate K_d .

3.6 Limitations and challenges

While our ACTIS experiments yielded compelling results, we found different limitation and challenges that we want to discuss here. These challenges and limitations can be categorized as instrumental or as methodological.

In all conducted experiments, we identified a technical challenge related to introduction of air bubbles into ACTIS capillary system. This problem was very characteristic for initial runs following a change of working solutions. Due to air bubble introduction into the injection capillary, the resulting signal was either lost or significantly changed compared to signals from other runs. Consequently, first runs yielded much lower or much higher signal intensity. To address this instrumentation issue, the employing of isopropanol between each sample change can be beneficial. Due to its lower viscosity, compared to aqueous solution of NH_4Ac , it could push air bubbles out of the capillary [55]. In addition

to this, a pump which can set higher pressure to the setup can be also helpful in terms of air bubble reduction.

The methodological limitations refer to the coupling of ACTIS to a detection system. The main limitation of ACTIS-FLD is its applicability on systems which have fluorescence active compound only. Furthermore, the flow cell volume affects the precision of transient measurement. To improve the precision, the FLD with lower flow cell volume should be used.

Even though very low K_d values can be assessed using ACTIS-TOF-MS, we are aware that this method may have few limitations. The investigation of lower binding affinities is limited by the protein concentration. The protein concentration that can be introduced into the TOF-MS device is limited. The protein fragment ions are masking the ligand ions and affects negatively the ion extracting process. The signal-masking effects can be compensated during the evaluation process. Nevertheless, the protein concentration range for working solutions should be selected so, to ensure that no signal overlapping occurs. The investigation of less complex PC system of only two molecules would also greatly improve the process of finding specific m/z values for the extracting of ion chromatograms.

By coupling the ACTIS to ICP based detection systems (ICP-MS and ICP-AES), few points need to be considered. The concentrations of metals are limited by the $[C]/K_d$ ratio in order to achieve accurate K_d values. The injected metal quantity is additionally diluted by the ARS in the separation capillary. Thus, in regard to the BLG-FeQ₂ model system, more sensitive Fe detection would be of advantage.

In the ACTIS-AES, the strong influence of the flow rate on signal represents the main challenge. This can compromise the sensitivity and accuracy of the measurement. Therefore, future experiments on this technique should reduce flow rates in separation steps. Moreover, the assessing of K_d using ACTIS-ICP-MS is strongly affected by the chosen stock solution. The preparation of freshly made Fe solutions in NH₄Ac and the preparation of Fe stock using sub-boiled H₂O in 2% HNO₃ and 0.1% HCl greatly improve the signals intensity and stability.

Since ACTIS is a novel method, it is currently under-explored within the research community, resulting in a limited pool of researchers actively investigating it. This may be challenging in terms of exchange of experiences. On the other hand, the research of this novel method can stimulate innovation and creativity.

4 Summary and conclusion

In conclusion, this work showed that assessing the K_d of metal-protein systems is possible using ACTIS. The conducted ACTIS-FLD measurements on HSA-FLC model system validated the capability of our setup to conduct ACTIS experiments. K_d values in $\mu\text{mol L}^{-1}$ range found in both ACTIS-FLD experiments align with literature value for BSA-FLC model system. This showed that the chosen ACTIS instrumentation is suitable for further experiments.

The validated ACTIS-FLD system was subsequently employed to explore the feasibility of assessing K_d of a specific metal-protein system (BLG-FeQ₂). Challenges related to solubility and signal intensity were effectively addressed during this stage. Although the ability of K_d estimation of this model system using ACTIS-FLD was verified, the necessity for a more sensitive detection system became evident.

To our knowledge, the assessment of BLG-FeQ₂ binding using ACTIS-TOF-MS represents the lowest K_d values found for this complex. K_d value assessed in both ACTIS-TOF-MS experiments were in nmol L^{-1} range. Despite the relatively high standard deviations, these values highlight the potential of the ACTIS method to assess low K_d values. Additionally, we found that it is crucial to perform one experiment within a single day, to eliminate potential variations in device properties that can greatly impact the results.

Coupling of ACTIS to ICP-MS showed promising results when investigating higher K_d values where higher iron concentrations need to be measured. We found that the pH value and the solvent used influence the obtained Fe signal. Transient measurements of Fe concentrations in nmol L^{-1} to $\mu\text{mol L}^{-1}$ range are the base for the assessing accurate K_d of BLG-FeQ₂ model system. The present capability of ICP-MS was not sufficient for this. Therefore, the method optimization through systematic studies is required.

Exploration of ACTIS-ICP-AES system revealed issues caused by flow rate - dependent signal change in transient Fe signal. Additionally, the binding of Fe to Q and BLG affected changes in Fe signal compared to signals of pure Fe solutions. This indicates that the complexation of iron positively affects its detection with this technique. More precise transient metal detection would allow assessing of metal-protein binding affinities using this method.

We must note that the chosen protein-metal model system posed challenges for the ACTIS exploration. The main reason for this is the strong binding that requires low metal concentrations for working solutions. In the separation step of an ACTIS run, this concentration is additionally diluted. Therefore, very low LOQ of detection method is required. Additionally, having three compounds in this model makes the assessment even more complicated.

Finally, we made additional important discoveries by employing computer simulations. In silico simulating of ACTIS experiments with different transfer capillary inner radius proved that the same capillary inner radii of separation and transfer capillary yield the most accurate K_d values. Moreover, the increasing of transfer capillary inner radius induces more turbulence of molecules and destroys the characteristic flow profiles. Additionally, we found that the noise about 15 counts can greatly affects the accuracy of the gained results independently of transfer capillary inner radius. On the other hand, best precision was found for the inner radius of transfer capillary matching the inner radius of separation capillary. A high signal-to-noise ratio is an important requirement for accurate K_d assessment. Based on these simulations, we recommend at least 10 signal-to-noise.

ACTIS proved to be a challenging method to handle. The estimated time for one ACTIS experiment is about 8 h, and the experimenter must be present the whole time. Automated valve and pump switching between the steps, greatly reduces the need of the experimenter to be present, but it is still necessary for sample injection and tracking the sample loading. We found the evaluation of the results also demanding. The actual evaluation using prACTISed take only few seconds, but the preparation of the results for the evaluation is time-consuming since the cut of the separation peaks and their normalization must be done manually in Excel or related software before input into prACTISed.

In summary, the ACTIS method shows great promise for accurately determining K_d of protein-metal complexes. It can assess a wide range of K_d values, depending on the detection system used. By implementing the recommendations given in the next section and addressing the minor technical issues, ACTIS has the potential to become a widely accepted standard for K_d assessment. Additionally, the method's capability for computer simulations is a significant advantage.

5. Outlook

This work is the first step towards enhancing the assessing of metal-protein binding constants. The present findings may help to better design the future ACTIS experiments. Therefore, here are few recommendations for this purpose.

The applying of ACTIS-TOF-MS has a great potential to become main ACTIS detector for assessing PC binding, especially when C is an organic molecule. To further investigate this method, few interesting model systems can be used. For example, binding of an anti-cholesterol drug Rosuvastatin (ROS) to HSA was recently investigated using SPR and K_d value of $1.55 \times 10^{-2} \mu\text{mol L}^{-1}$ was found [56]. If we assume that the real value is in this scale, the $[\text{ROS}]_0$ for working solution should be around $1.55 \times 10^{-4} \mu\text{mol L}^{-1}$. Even though very low concentrations needed for this experiment, the molecule structure of ROS might have a characteristic sulfur containing fragment that represents a specific m/z value for tracking [ROS] over the time [57]. Furthermore, the binding of BSA to Acetazolamide (AZA) was also investigated using SPR and K_d of $67.72 \mu\text{mol L}^{-1}$ was assessed [58]. K_d in this range enables higher compound concentrations for ACTIS experiments. Since the AZA is a small organic molecule of mass of $222.25 \text{ g mol}^{-1}$ with ESI as a soft ionization technique, theoretically the intact molecules could be used for tracking [AZA] over time.

The employing of MS devices with higher resolution compared to TOF devices, such as Orbitrap, could also improve ACTIS. More specifically, the typical TOF-MS resolution is in the range of 10,000-100,000 compared to Orbitrap which possesses resolutions of 100,000 up to 1,000,000 [59]. Lower resolution may be challenging in evaluation of ACTIS measurements, especially in complex mixtures with higher protein content.

Future experiments of ACTIS coupling to ICP techniques should consider protein-metal model systems including less abundant metals than Fe. Theoretically, precious metals such as Gold (Au), Platinum (Pt), Palladium (Pd) or heavy metals Cadmium (Cd), Lead (Pb), Mercury (Hg) can be effectively and more precisely determined using ICP-MS. HSA and hemoglobin (HG) have a high affinity to Hg with K_d of about $1 \times 10^{-7} \mu\text{mol L}^{-1}$ [60]. Moreover, the investigation of Pt binding peptides would be also suitable for further experiments [61].

5 References

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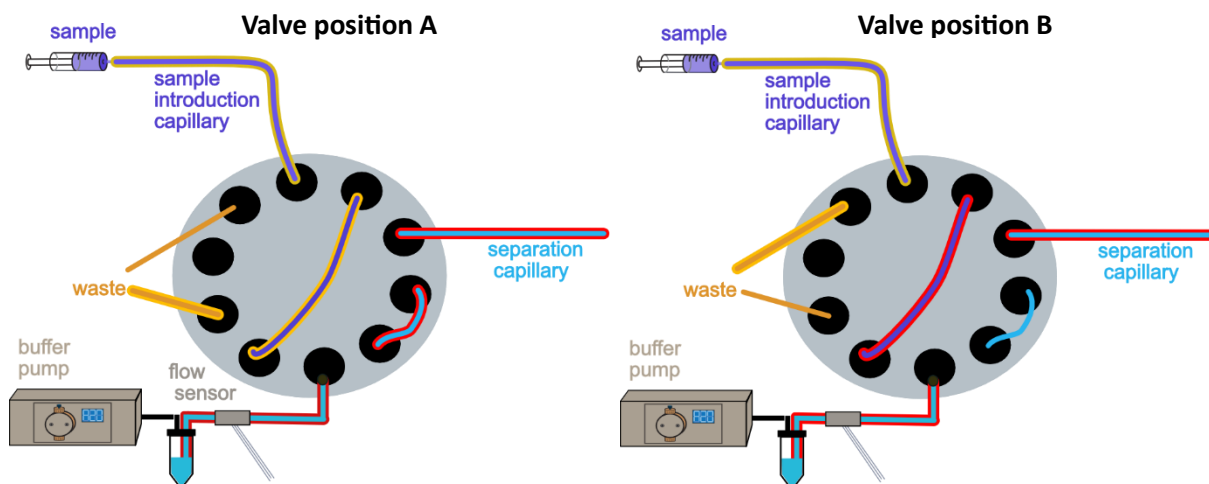
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Appendix

Section 1: Scheme of valve position



Section 2: Python script “automACTIS”

```
#!/usr/bin/env python3
# -*- coding: utf-8 -*-
# Imports
import random
import serial
import time
import win32con
import win32api
import win32ui
# Parameters
# -----
pump_device = "COM5"
valve_device = "COM1"
chrom_button_ID = 2
no_clean_switches = 10
time_preflush = 10 # s
time_plugpush = 20 # s
time_acquisition = 180 # s
time_clean_switch = 5 # s
time_clean = 60 # s
pressure_main = 135.0 # mbar
pressure_plug = 230.0 # mbar
pressure_clean = 2000.0 # mbar

# Init
# -----
# Setup and open serial connection for the pump
pump_ser = serial.Serial(port=pump_device,
                          baudrate=115384,
                          bytesize=serial.EIGHTBITS,
                          parity=serial.PARITY_NONE,
                          stopbits=serial.STOPBITS_ONE,
                          rtscts=True,
                          dsrdtr=True,
                          timeout=2
                          )
# Setup and open serial connection for the valve
valve_ser = serial.Serial(port=valve_device,
                           baudrate=9600,
```

```

        bytesize=serial.EIGHTBITS,
        parity=serial.PARITY_NONE,
        stopbits=serial.STOPBITS_ONE,
        rtscts=False,
        dsrdtr=False,
        timeout=2
    )
def pump_send(ser, text):
    sendbytes = (text + "\n").encode()
    ser.write(sendbytes)

def valve_send(ser, text):
    sendbytes = (text + "\r").encode()
    ser.write(sendbytes)

def recv(ser):
    readbytes = ser.read_until()
    return readbytes.decode(errors='replace')

def chrom_start_acquisition():
    try:
        pyCWnd = win32ui.FindWindow("#32770", "Chromeleon")
    except Exception as a:
        print("Error finding Chromeleon window", a)

    print("Chromeleon window found:", pyCWnd, "0x%x" % (pyCWnd.GetSafeHwnd()))

    try:
        # Control ID for the "OK"-Button in the Chromeleon dialog box is "2"
        pyCWnd.SendMessage(win32con.WM_COMMAND, chrom_button_ID, 0)
    except Exception as a:
        print("Error sending Chromeleon the OK-command", a)

# Pre-program
# -----
# Valve: set to initial position A
print("Set valve position to A...")
valve_send(valve_ser, "lGOA")

# Pump
print("Initialising pump...")
pump_send(pump_ser, "/startpcmode")
pump_send(pump_ser, "/getpid")
pid = recv(pump_ser)
print("Pump ID:", pid)
pump_send(pump_ser, "/setp1 %.2f" % pressure_main)
time.sleep(time_preflush)
pump_send(pump_ser, "/ping")
print("Pump pong:", recv(pump_ser))

# Program
# -----
# Push plug into capillary
print("Pushing plug into separation capillary...")
valve_send(valve_ser, "lGOB")
pump_send(pump_ser, "/setp1 %.2f" % pressure_plug)
time.sleep(time_plugpush)
pump_send(pump_ser, "/ping")
print("Pump pong:", recv(pump_ser))

# Acquisition (main part)
print("Starting acquisition...")
valve_send(valve_ser, "lGOA")
chrom_start_acquisition()
pump_send(pump_ser, "/setp1 %.2f" % pressure_main)
time.sleep(time_acquisition)
pump_send(pump_ser, "/ping")
print("Pump pong:", recv(pump_ser))

# Post-program
# -----
print("Cleaning valve...")
pump_send(pump_ser, "/setp1 %.2f" % pressure_clean)
for i in range(no_clean_switches):
    valve_send(valve_ser, "lTO")
    time.sleep(time_clean_switch)
pump_send(pump_ser, "/ping")
print("Pump pong:", recv(pump_ser))

```

```

pump_send(pump_ser, "/setp1 %.2f" % pressure_main)
pump_send(pump_ser, "/ping")
print("Pump pong:", recv(pump_ser))

# Push plug into capillary
print("Cleaning valve...")
valve_send(valve_ser, "1GOA")
pump_send(pump_ser, "/setp1 %.2f" % pressure_clean)
time.sleep(time_clean)
pump_send(pump_ser, "/ping")
print("Pump pong:", recv(pump_ser))
print("Program finished.")
pump_ser.close()
valve_ser.close()

```

Section 3: The “hack” script for the extraction of ICP-AES transient Fe signals

```

# This is the handle you want to check
$handle = 0x205BA
# Maximum points you want to collect
$maxpoints = 5000

# Import GetWindowText
Add-Type @"
    using System;
    using System.Runtime.InteropServices;
    public class UserWindows {
        [DllImport("user32.dll")]
        public static extern IntPtr GetWindowText(IntPtr hWnd, System.Text.StringBuilder text, int
count);
    }
"@

$str = New-Object System.Text.StringBuilder 256

$n = 0
"Time (s)\tValue"
for($i = 0; $i -le $maxpoints; $i++) {
    # Receive Window-Text
    $ret = [UserWindows]::GetWindowText($handle, $str, 256)

    "$($i+1)\t$($str.ToString())"

    # Sleep one second

```

Section 4: Text file for capillary geometry

```

/*****
Geometry for a 2D cross section of two capillaries for ACTIS.
Geometry includes a plug-region in the beginning for propagation
of (non-)diffusive species.
Created by Dr. Sven Kochmann, 2023.07.20
Modified by ...
Manual: https://gmsh.info/doc/texinfo/gmsh.html#Geometry-scripting-commands
*****/

/* Definitions: all sizes are in mm */
cap_length = 3.8;
cap_radius = 0.25;
plug_length = 0.3;

/* Mesh size should be a bit smaller than the smallest
dimension above */
mesh_size = 0.01;

/* Points { x, y, z, mesh } */
Point(1) = { 0.0, -cap_radius, 0.0, mesh_size };
Point(2) = { 0.0, +cap_radius, 0.0, mesh_size };

```

```

Point(3) = { plug_length, -cap_radius, 0.0, mesh_size };
Point(4) = { plug_length, +cap_radius, 0.0, mesh_size };

Point(5) = { cap_length, -cap_radius, 0.0, mesh_size };
Point(6) = { cap_length, +cap_radius, 0.0, mesh_size };

/* Curves { p1, p2 } */
Line(1) = {1, 2};
Line(2) = {2, 4};
Line(3) = {4, 3};
Line(4) = {3, 1};

Line(5) = {3, 5};
Line(6) = {5, 6};
Line(7) = {4, 6};

/* Loops: first one for the plug; second one for the capillaries */
Curve Loop(1) = {1, 2, 3, 4};
Curve Loop(2) = {3, 5, 6, -7};

/* Will be grouped boundaries for Elmer */
Physical Curve("walls") = {2, 4, 7, 5};
Physical Curve("inlet") = {1};
Physical Curve("outlet") = {6};

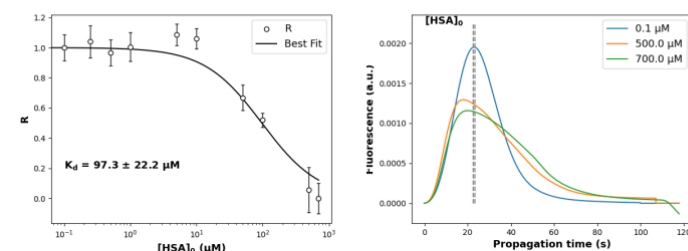
/* Surfaces: Plug + capillaries */
Plane Surface(1) = { 1 };
Plane Surface(2) = { 2 };

Physical Surface("plug") = { 1 };
Physical Surface("capillary") = { 2 };

```

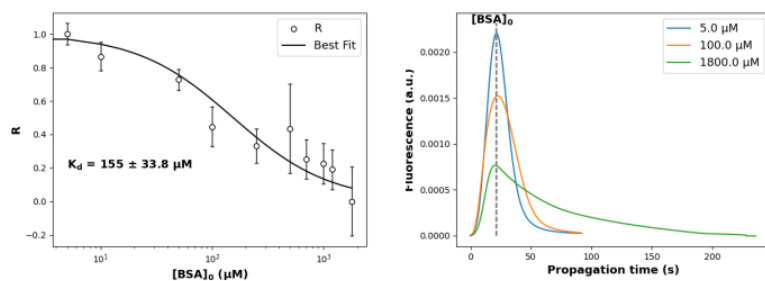
Section 5: Assessing of HSA-FLC binding; ACTIS-FLD experiments

HSA-FLC first experiment normalized



Propagation flow rate	68	Conc	Avg Sig (S)	S Std Dev	S Rel Std Dev	R value	R Std Dev	R Rel Std Dev
Injection flow rate	0	0.1 μM	0.002015706	4.88266e-05	2.422308	1	0.08656556	8.656556
Injection time (s)	0	0.25 μM	0.002047313	6.765785e-05	3.304714	1.039625	0.1060751	10.20321
Separation capillary length	60	0.5 μM	0.001989812	5.020637e-05	2.523171	0.9675384	0.08645506	8.935569
Separation capillary diameter	127	1.0 μM	0.002020157	6.000851e-05	2.970487	1.00558	0.0972025	9.666308
Injection loop length	13	5.0 μM	0.002083888	1.740985e-05	0.8354503	1.085476	0.07020513	6.467681
Injection loop diameter	50	10.0 μM	0.002063197	1.178047e-05	0.5709812	1.059537	0.066653	6.290768
Protein name	HSA	50.0 μM	0.00175138	5.464571e-05	3.120152	0.6686297	0.08327541	12.45464
Ligand name	Fluorescein	100.0 μM	0.001632537	8.248854e-06	0.5052782	0.5196433	0.04805605	9.247892
Number of Concentrations	10	500.0 μM	0.001262834	0.0001064515	8.429573	0.05616821	0.149727	266.569
Initial Ligand concentration [L]₀ (μM)	0.05	700.0 μM	0.00121803	5.73012e-05	4.704416	0	0.1015903	10159030
Type of Data	F	Kd: 97.3094 ± 22.1817 μM						
Compensation procedure	N	R²: 0.9547						
[P]₀ reference for MS normalization (μM)	nan	Chi²: 0.2410						
Window width (%)	2							
Determination of peak	P							
Manually determined peaks	nan							
[P]₀ to programmatically determine peak	0.1							

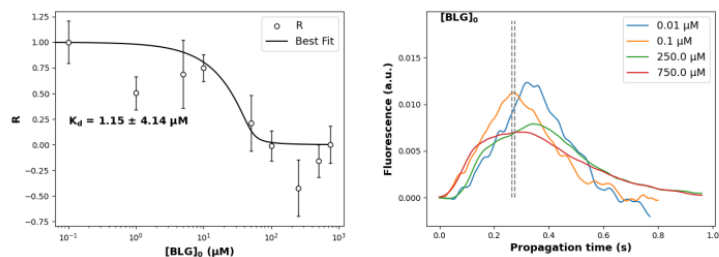
HSA-FLC second experiment -prACTISed



Propagation flow rate	68	Conc	Avg Sig (S)	S Std Dev	S Rel Std Dev	R value	R Std Dev	R Rel Std Dev
Injection flow rate	0	5.0 μM	0.002125833	5.300003e-05	2.493142	1	0.0634706	6.34706
Injection time (s)	0	10.0 μM	0.001967858	8.576207e-05	4.358144	0.8662263	0.08466273	9.773743
Separation capillary length	60	50.0 μM	0.001803558	4.260265e-05	2.362144	0.7270974	0.06290515	8.651544
Separation capillary diameter	127	100.0 μM	0.001471877	0.0001019834	6.928798	0.4462296	0.1200373	26.90034
Injection loop length	13	250.0 μM	0.001335575	2.73844e-05	2.050383	0.3308083	0.1016019	30.71322
Injection loop diameter	50	500.0 μM	0.001457729	0.0002985591	20.4811	0.4342492	0.26671	61.41866
Protein name	BSA	700.0 μM	0.001243637	4.44489e-05	3.574104	0.2529558	0.1160402	45.87371
Ligand name	Fluorescein	1000.0 μM	0.001211006	4.651478e-05	3.841003	0.2253236	0.1202978	53.38889
Number of Concentrations	10	1200.0 μM	0.00117033	1.979912e-05	1.691755	0.1908792	0.1197392	62.73038
Initial Ligand concentration [L]₀ (μM)	0.05	1800.0 μM	0.0009449182	0.0001725859	18.26464	0	0.2066816	20668160
Type of Data	F	Kd: 154.5953 ± 33.7676 μM						
Compensation procedure	N	R²: 0.8913						
[P]₀ reference for MS normalization (μM)	nan	Chi²: 0.4453						
Window width (%)	2							
Determination of peak	P							
Manually determined peaks	nan							
[P]₀ to programmatically determine peak	5							

Section 6: Assessing of BLG-FeQ₂ binding; ACTIS-FLD experiment

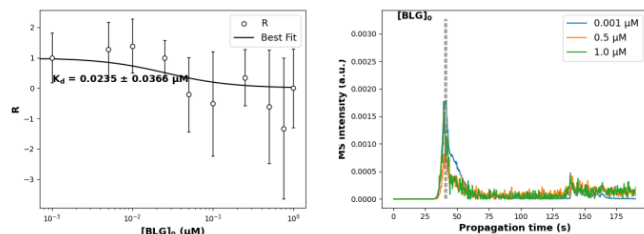
BLGFeQ2 ACTIS-FLD experiment - normalized



Propagation flow rate	68	Conc	Avg Sig (S)	S Std Dev	S Rel Std Dev	R value	R Std Dev	R Rel Std Dev
Injection flow rate	0	0.01 μM	0.01002703	0.0005412547	5.397955	nan	nan	nan
Injection time (s)	0	0.1 μM	0.01080434	0.0004523885	4.187101	1	0.2068942	20.68942
Separation capillary length	60	1.0 μM	0.009274103	0.0003980184	4.291718	0.5051426	0.1613164	31.93483
Separation capillary diameter	127	5.0 μM	0.00984067	0.0009703127	9.86023	0.6883627	0.3319446	48.22234
Injection loop length	13	10.0 μM	0.01003413	0.0001994242	1.987457	0.7509266	0.1313003	17.4851
Injection loop diameter	50	50.0 μM	0.00836311	0.0007803746	9.331153	0.2105399	0.2734992	129.9037
Protein name	BLG	100.0 μM	0.007684859	0.0002273405	2.958291	-0.008797125	0.1483466	14834660
Ligand name	Quercetin	250.0 μM	0.006401801	0.0006089892	9.512779	-0.4237205	0.2751203	27512030
Number of Concentrations	10	500.0 μM	0.007227641	0.0001775533	2.456587	-0.1566552	0.1601401	16014010
Initial Ligand concentration [L] ₀ (μM)	50	750.0 μM	0.007712062	0.0003949383	5.121047	0	0.18062	18062000
Type of Data	F							
Compensation procedure	N	Kd: 1.1544 ± 4.1424 μM						
[P] ₀ reference for MS normalization (μM)	nan	R ² : 0.7291						
Window width (%)	2	Chi ² : 42.4552						
Determination of peak	P							
Manually determined peaks	nan							
[P] ₀ to programmatically determine peak	0.1							

Section 7: Assessing of BLG-FeQ₂ binding; first ACTIS-TOF-MS experiment

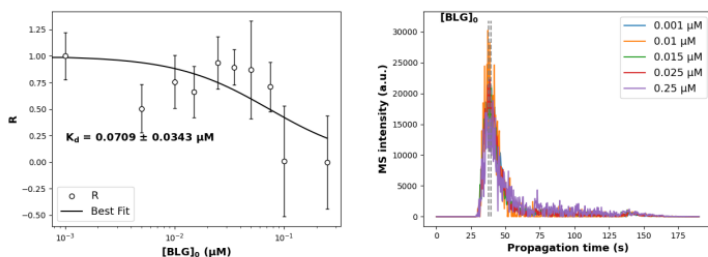
BLG-FeQ₂ first ACTIS-TOF-MS experiment



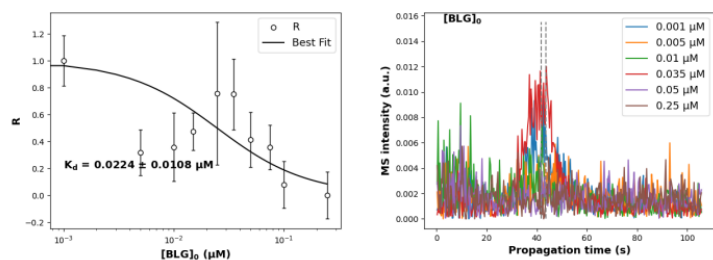
Propagation flow rate	70	Conc	Avg Sig (S)	S Std Dev	S Rel Std Dev	R value	R Std Dev	R Rel Std Dev
Injection flow rate	20	0.001 μM	0.001971899	0.0001768508	8.968554	1	0.8142459	81.42459
Injection time (s)	20	0.005 μM	0.002054572	0.0001508738	7.34332	1.269153	0.914276	72.0383
Separation capillary length	60	0.01 μM	0.002091095	4.426416e-05	2.116793	1.388058	0.8863364	63.85444
Separation capillary diameter	127	0.025 μM	0.00196764	5.750024e-05	2.922296	0.9861326	0.5979736	60.63825
Injection loop length	13	0.05 μM	0.001600418	0.0001577062	9.854064	-0.2094017	1.226051	122605100
Injection loop diameter	50	0.1 μM	0.001508243	0.000299154	19.83461	-0.5094883	1.71552	171552000
Protein name	BLG	0.25 μM	0.001772	0.0002077742	11.7254	0.3492059	0.9234279	264.4365
Ligand name	Quercetin	0.5 μM	0.001476923	0.0003397163	23.00163	-0.6114541	1.876725	187672500
Number of Concentrations	10	0.75 μM	0.001256223	0.0001540226	12.26077	-1.329969	2.320493	232049300
Initial Ligand concentration [L] ₀ (μM)	0.005	1.0 μM	0.001664738	0.0002811082	16.88603	0	1.294261	129426100
Type of Data	MS	Kd: 0.0235 ± 0.0366 μM						
Compensation procedure	Compensated	R ² : 0.4712						
[P] ₀ reference for MS normalization (μM)	1.0	Chi ² : 75.6142						
Window width (%)	2							
Determination of peak	P							
Manually determined peaks	nan							
[P] ₀ to programmatically determine peak	0.001							

Section 8: Assessing of BLG-FeQ₂ binding; second ACTIS-TOF-MS experiment

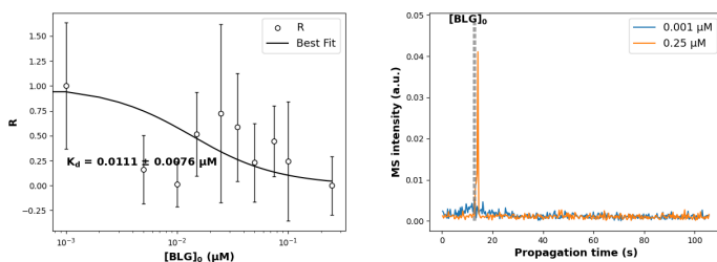
BLG-FeQ₂ second ACTIS-TOF-MS experiment - all ions



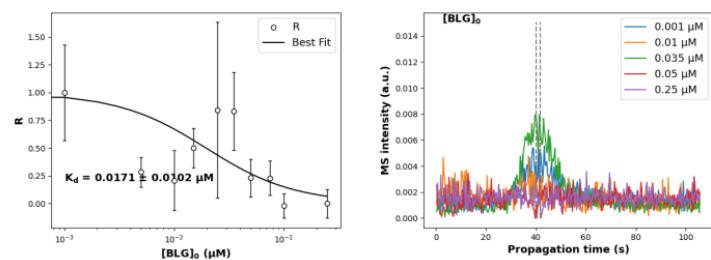
Propagation flow rate	70	Conc	Avg Sig (S)	S Std Dev	S Rel Std Dev	R value	R Std Dev	R Rel Std Dev
Injection flow rate	20	0.001 μM	20244.59	740.9369	3.659925	1	0.221256	22.1256
Injection time (s)	20	0.005 μM	17901.95	707.8993	3.954315	0.5053415	0.2285744	45.23168
Separation capillary length	60	0.01 μM	19097.37	975.0428	5.105639	0.75776	0.2492293	32.89027
Separation capillary diameter	254	0.015 μM	18642.31	908.4146	4.872866	0.6616715	0.242021	36.57722
Injection loop length	13	0.025 μM	19947.01	944.3866	4.734477	0.9371642	0.2482821	26.49291
Injection loop diameter	113	0.035 μM	19746.96	413.9084	2.096061	0.8949232	0.1682532	18.80086
Protein name	BLG	0.05 μM	19632.91	2067.461	10.53059	0.8708411	0.4590783	52.71665
Ligand name	Quercetin	0.075 μM	18872.49	868.1272	4.599961	0.710275	0.2325177	32.7363
Number of Concentrations	10	0.1 μM	15544.85	1997.503	12.84994	0.00763096	0.522585	6848.221
Initial Ligand concentration [L] ₀ (μM)	0.005	0.25 μM	15508.71	1472.432	9.494228	0	0.4396924	43969240
Type of Data	MS	Kd: 0.0709 ± 0.0343 μM						
Compensation procedure	Compensated	R ² : 0.4439						
[P] ₀ reference for MS normalization (μM)	0.001	Chi ² : 1.2193						
Window width (%)	2							
Determination of peak	P							
Manually determined peaks	nan							
[P] ₀ to programmatically determine peak	0.001							



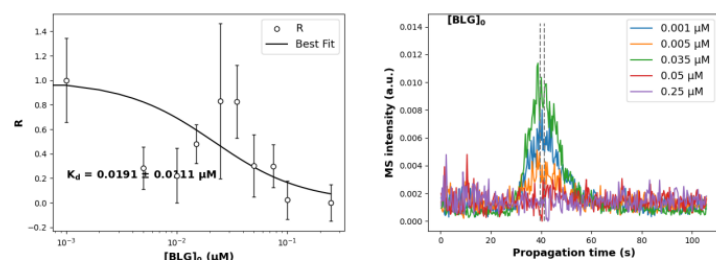
Propagation flow rate	70	Conc	Avg Sig (S)	S Std Dev	S Rel Std Dev	R value	R Std Dev	R Rel Std Dev
Injection flow rate	20	0.001 μM	0.007013881	0.0007145604	10.1878	1	0.1875582	18.75582
Injection time (s)	20	0.005 μM	0.003335934	0.0007667657	22.98503	0.3173665	0.1709106	53.85276
Separation capillary length	60	0.01 μM	0.003558158	0.001275519	35.84774	0.3586117	0.2542654	70.90271
Separation capillary diameter	254	0.015 μM	0.004186239	0.0005758489	13.75576	0.4751847	0.1401498	29.49376
Injection loop length	13	0.025 μM	0.005700669	0.002804639	49.19843	0.7562655	0.5309841	70.21134
Injection loop diameter	113	0.035 μM	0.005674356	0.001314162	23.15966	0.7513817	0.2652846	35.30624
Protein name	BLG	0.05 μM	0.003861037	0.0009805807	25.39682	0.4148266	0.2035443	49.06734
Ligand name	FeQ2	0.075 μM	0.003548103	0.0007298464	20.57005	0.3567454	0.1642219	46.03337
Number of Concentrations	10	0.1 μM	0.002043893	0.0006994131	34.21965	0.07756138	0.1734312	223.605
Initial Ligand concentration [L]₀ (μM)	0.005	0.25 μM	0.001626002	0.0006690662	41.14794	0	0.1756169	17561690
Type of Data	MS	Kd: 0.0224 ± 0.0108 μM						
Compensation procedure	N	R²: 0.2417						
[P]₀ reference for MS normalization (μM)	1.0	Chi²: 1.1967						
Window width (%)	2							
Determination of peak	P							
Manually determined peaks	nan							
[P]₀ to programmatically determine peak	0.001							



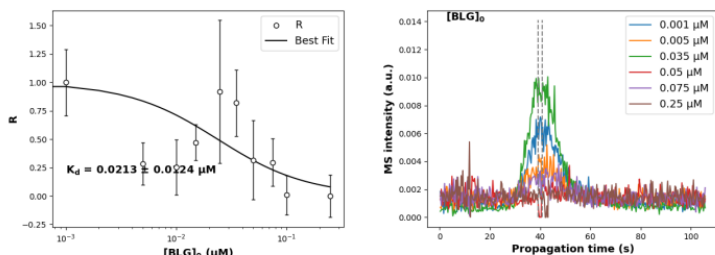
Propagation flow rate	70	Conc	Avg Sig (S)	S Std Dev	S Rel Std Dev	R value	R Std Dev	R Rel Std Dev
Injection flow rate	20	0.001 μM	0.003869331	0.001072301	27.71283	1	0.6330142	63.30142
Injection time (s)	20	0.005 μM	0.001863151	0.0006900058	37.03434	0.1625642	0.3442149	211.7409
Separation capillary length	60	0.01 μM	0.001502955	0.000229995	15.30285	0.01220816	0.2265071	1855.375
Separation capillary diameter	254	0.015 μM	0.002711025	0.0008023769	29.59681	0.5164907	0.4191719	81.15769
Injection loop length	13	0.025 μM	0.003209053	0.0019896	61.99959	0.7243815	0.8933985	123.3326
Injection loop diameter	113	0.035 μM	0.002880586	0.001116523	38.76028	0.58727	0.5419053	92.27532
Protein name	BLG	0.05 μM	0.00202749	0.0008269423	40.78651	0.2311637	0.3941333	170.4997
Ligand name	FeQ2	0.075 μM	0.002542723	0.0006407905	25.20095	0.4462367	0.3530746	79.12271
Number of Concentrations	10	0.1 μM	0.002059386	0.001363676	66.2176	0.2444781	0.6005082	245.6286
Initial Ligand concentration [L]₀ (μM)	0.005	0.25 μM	0.001473709	0.0004973694	33.7495	0	0.2936134	29361340
Type of Data	MS	Kd: 0.0111 ± 0.0076 μM						
Compensation procedure	N	R²: -0.1220						
[P]₀ reference for MS normalization (μM)	1.0	Chi²: 2.8223						
Window width (%)	2							
Determination of peak	P							
Manually determined peaks	nan							
[P]₀ to programmatically determine peak	0.001							



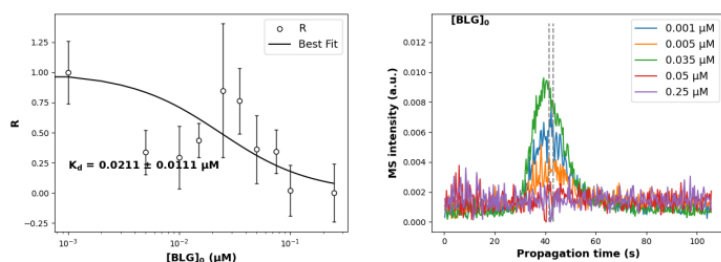
Propagation flow rate	70	Conc	Avg Sig (S)	S Std Dev	S Rel Std Dev	R value	R Std Dev	R Rel Std Dev
Injection flow rate	20	0.001 μM	0.0053372	0.0010866	20.35993	1	0.4308392	43.08392
Injection time (s)	20	0.005 μM	0.0027792	0.0002878	10.3578	0.2828605	0.1344353	47.52707
Separation capillary length	60	0.01 μM	0.0025162	0.0008996	35.7551	0.2091315	0.2696452	128.9357
Separation capillary diameter	254	0.015 μM	0.0035554	0.0002817	7.923989	0.5004639	0.1774546	35.45803
Injection loop length	13	0.025 μM	0.0047721	0.0026657	55.85951	0.8415902	0.7902328	93.89757
Injection loop diameter	113	0.035 μM	0.0047351	0.0008645	18.25797	0.8312054	0.3508561	42.21052
Protein name	BLG	0.05 μM	0.0025947	0.0004998	19.26436	0.2311411	0.1713161	74.11752
Ligand name	FeQ2	0.075 μM	0.0025895	0.0004244	16.38921	0.2296753	0.1543459	67.20178
Number of Concentrations	10	0.1 μM	0.0017006	0.0002276	13.38434	-0.019540	0.1116346	111.63460
Initial Ligand concentration [L]0 (μM)	0.005	0.25 μM	0.0017703	0.0003197	18.06345	0	0.1267873	126.78730
Type of Data	MS	Kd: 0.0171 ± 0.0102 μM						
Compensation procedure	N	R²: 0.2207						
[P]0 reference for MS normalization (μM)	1.0	Chi²: 1.9824						
Window width (%)	2							
Determination of peak	P							
Manually determined peaks	nan							
[P]0 to programmatically determine peak	0.001							



Propagation flow rate	70	Conc	Avg Sig (S)	S Std Dev	S Rel Std Dev	R value	R Std Dev	R Rel Std Dev
Injection flow rate	20	0.001 μM	0.0075281	0.0013099	17.40044	1	0.3442461	34.42461
Injection time (s)	20	0.005 μM	0.0036684	0.0007518	20.49535	0.2827663	0.1734319	61.33401
Separation capillary length	60	0.01 μM	0.0033450	0.0010768	32.19118	0.2226774	0.2231933	100.2317
Separation capillary diameter	254	0.015 μM	0.0047216	0.0004940	10.46425	0.4784862	0.1583451	33.09293
Injection loop length	13	0.025 μM	0.0066089	0.0032304	48.87926	0.8291959	0.6335809	76.40907
Injection loop diameter	113	0.035 μM	0.0065876	0.0011827	17.95398	0.8252387	0.2983346	36.15131
Protein name	BLG	0.05 μM	0.0037759	0.0012408	32.86151	0.3027498	0.2531781	83.62618
Ligand name	FeQ2	0.075 μM	0.0037583	0.0007653	20.36455	0.2994709	0.1763368	58.88278
Number of Concentrations	10	0.1 μM	0.0022709	0.0006280	27.65498	0.0230835	0.156367	677.3972
Initial Ligand concentration [L]0 (μM)	0.005	0.25 μM	0.0021467	0.0005724	26.66503	0	0.150434	1504.3400
Type of Data	MS	Kd: 0.0191 ± 0.0111 μM						
Compensation procedure	N	R²: 0.1752						
[P]0 reference for MS normalization (μM)	1.0	Chi²: 1.7638						
Window width (%)	2							
Determination of peak	P							
Manually determined peaks	nan							
[P]0 to programmatically determine peak	0.001							

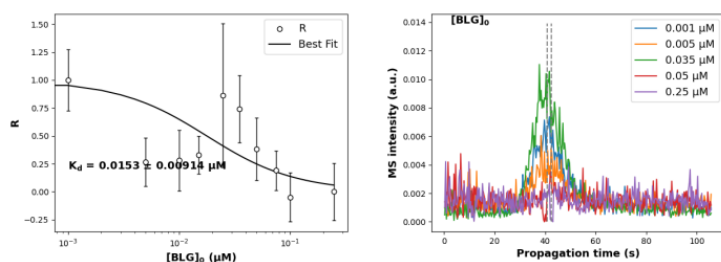


Propagation flow rate	70	Conc	Avg Sig (S)	S Std Dev	S Rel Std Dev	R value	R Std Dev	R Rel Std Dev
Injection flow rate	20	0.001 μM	0.0074114 15	0.0010417 33	14.05579	1	0.291627	29.1627
Injection time (s)	20	0.005 μM	0.0038013 69	0.0007484 805	19.68976	0.2853899	0.1855187	65.00536
Separation capillary length	60	0.01 μM	0.0036386 86	0.0010942 18	30.0718	0.2531866	0.2438714	96.32082
Separation capillary diameter	254	0.015 μM	0.0047444 88	0.0005155 318	10.86591	0.4720806	0.1574917	33.36119
Injection loop length	13	0.025 μM	0.0069903 6	0.0030351 13	43.41855	0.916652	0.629933	68.72106
Injection loop diameter	113	0.035 μM	0.0065018 92	0.0011942 74	18.3681	0.8199594	0.2916323	35.56668
Protein name	BLG	0.05 μM	0.0039591 51	0.0016716 5	42.22245	0.3166228	0.3492742	110.3124
Ligand name	FeQ2	0.075 μM	0.0038486 38	0.0008946 851	23.2468	0.2947467	0.20935	71.02709
Number of Concentrations	10	0.1 μM	0.0024023 3	0.0005536 696	23.04719	0.0084494 27	0.1713065	2027.434
Initial Ligand concentration [L]₀ (μM)	0.005	0.25 μM	0.0023596 45	0.0006707 173	28.4245	0	0.1877634	18776340
Type of Data	MS	Kd: 0.0213 ± 0.0124 μM						
Compensation procedure	N	R²: 0.1908						
[P]₀ reference for MS normalization (μM)	1.0	Chi²: 1.7812						
Window width (%)	2							
Determination of peak	P							
Manually determined peaks	nan							
[P]₀ to programmatically determine peak	0.001							



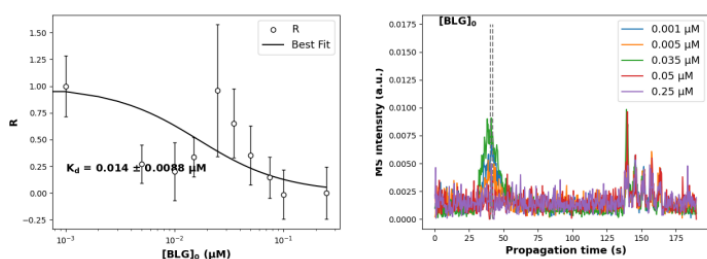
Propagation flow rate	70	Conc	Avg Sig (S)	S Std Dev	S Rel Std Dev	R value	R Std Dev	R Rel Std Dev
Injection flow rate	20	0.001 μM	0.0069176 98	0.0008842 301	12.78214	1	0.2604111	26.04111
Injection time (s)	20	0.005 μM	0.0037401 76	0.0006260 604	16.7388	0.33829	0.1829938	54.09375
Separation capillary length	60	0.01 μM	0.0035358 93	0.0010720 68	30.31958	0.2957486	0.2590186	87.58064
Separation capillary diameter	254	0.015 μM	0.0042144 94	0.0003402 549	8.073446	0.4370655	0.1436078	32.85728
Injection loop length	13	0.025 μM	0.0061957 08	0.0025475 83	41.1185	0.8496477	0.5537032	65.16857
Injection loop diameter	113	0.035 μM	0.0057816 12	0.0011005 72	19.03573	0.7634133	0.2718479	35.60954
Protein name	BLG	0.05 μM	0.0038534 47	0.0012110 51	31.42774	0.3618783	0.2824357	78.04715
Ligand name	FeQ2	0.075 μM	0.0037748 78	0.0006189 351	16.39616	0.3455165	0.1816471	52.57263
Number of Concentrations	10	0.1 μM	0.0022226 6	0.0006241 479	28.08112	0.0222715 1	0.2108047	946.5217
Initial Ligand concentration [L]₀ (μM)	0.005	0.25 μM	0.0021157 12	0.0008148 693	38.51513	0	0.2399839	23998390
Type of Data	MS	Kd: 0.0211 ± 0.0111 μM						
Compensation procedure	N	R²: 0.2326						
[P]₀ reference for MS normalization (μM)	1.0	Chi²: 1.4899						
Window width (%)	2							
Determination of peak	P							
Manually determined peaks	nan							
[P]₀ to programmatically determine peak	0.001							

BLG-FeQ2 second ACTIS-TOF-MS experiment - 508.9935 - single ion extractions



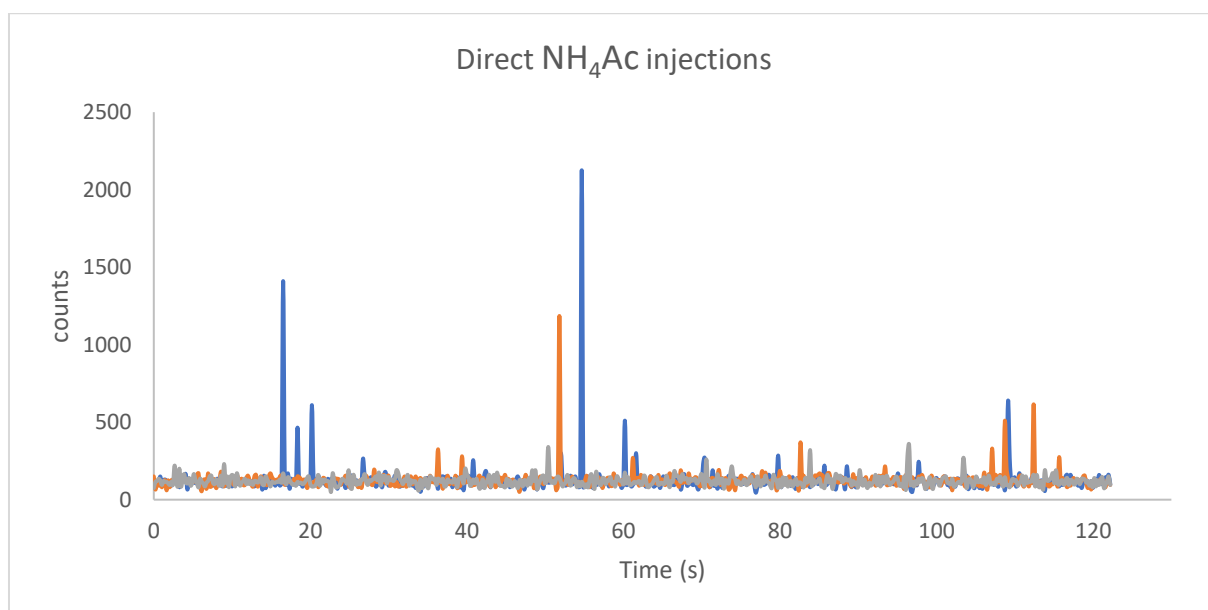
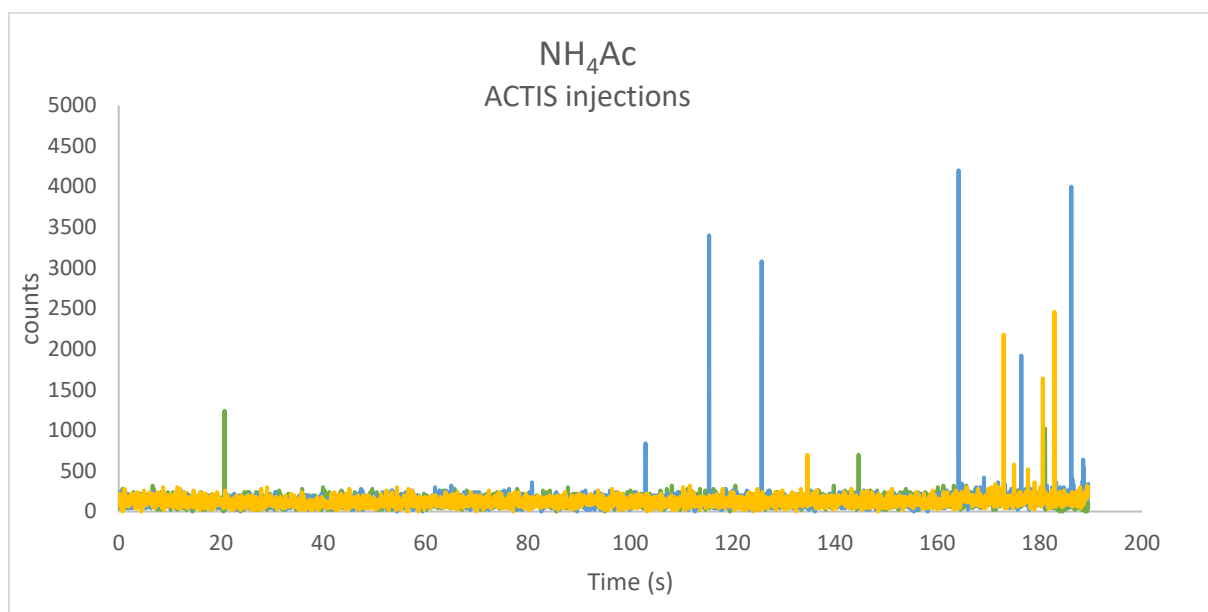
Propagation flow rate	70	Conc	Avg Sig (S)	S Std Dev	S Rel Std Dev	R value	R Std Dev	R Rel Std Dev
Injection flow rate	20	0.001 μM	0.00744512	0.00095319	12.80288	1	0.2753861	27.53861
Injection time (s)	20	0.005 μM	0.003839961	0.0007974402	20.76688	0.2635013	0.2163595	82.10945
Separation capillary length	60	0.01 μM	0.00391965	0.001141707	29.12778	0.279781	0.2724645	97.38493
Separation capillary diameter	254	0.015 μM	0.004169447	0.0004825711	11.57398	0.3308119	0.1686148	50.96998
Injection loop length	13	0.025 μM	0.006766146	0.003038658	44.90973	0.8612922	0.643512	74.71472
Injection loop diameter	113	0.035 μM	0.006180533	0.001280384	20.71641	0.7416572	0.3024014	40.77375
Protein name	BLG	0.05 μM	0.004418828	0.001190263	26.93617	0.3817581	0.2776365	72.72577
Ligand name	FeQ2	0.075 μM	0.003483533	0.0004537511	13.0256	0.1906865	0.1768359	92.73648
Number of Concentrations	10	0.1 μM	0.002303367	0.0005374511	23.33328	-0.05040993	0.2191609	21916090
Initial Ligand concentration [L]₀ (μM)	0.005	0.25 μM	0.002550123	0.0008827135	34.61455	0	0.2550247	25502470
Type of Data	MS	Kd: 0.0153 ± 0.0091 μM						
Compensation procedure	N	R²: 0.2064						
[P]₀ reference for MS normalization (μM)	1.0	Chi²: 2.0698						
Window width (%)	2							
Determination of peak	P							
Manually determined peaks	nan							
[P]₀ to programmatically determine peak	0.001							

BLG-FeQ2 second ACTIS-TOF-MS experiment - 590.9913 - single ion extractions



Propagation flow rate	70	Conc	Avg Sig (S)	S Std Dev	S Rel Std Dev	R value	R Std Dev	R Rel Std Dev
Injection flow rate	20	0.001 μM	0.006776436	0.0008602737	12.69508	1	0.2826478	28.26478
Injection time (s)	20	0.005 μM	0.003642913	0.0004928786	13.5298	0.2720074	0.1785145	65.62853
Separation capillary length	60	0.01 μM	0.003342569	0.0009849722	29.46752	0.2022304	0.2701333	133.577
Separation capillary diameter	254	0.015 μM	0.003925464	0.0005421553	13.81124	0.3376509	0.1830245	54.20523
Injection loop length	13	0.025 μM	0.006596412	0.002525758	38.28987	0.958176	0.6172947	64.42394
Injection loop diameter	113	0.035 μM	0.005285959	0.001248891	23.62657	0.6537265	0.3237761	49.52776
Protein name	BLG	0.05 μM	0.003996687	0.001049974	26.27112	0.3541977	0.2773968	78.31692
Ligand name	FeQ2	0.075 μM	0.003095398	0.0005236526	16.91713	0.1448067	0.1934989	133.6256
Number of Concentrations	10	0.1 μM	0.002416944	0.0006565984	27.16648	-0.01281451	0.232073	23207300
Initial Ligand concentration [L]₀ (μM)	0.005	0.25 μM	0.002472102	0.0007432035	30.06363	0	0.2441837	24418370
Type of Data	MS	Kd: 0.0140 ± 0.0088 μM						
Compensation procedure	N	R²: 0.1918						
[P]₀ reference for MS normalization (μM)	1.0	Chi²: 2.1885						
Window width (%)	2							
Determination of peak	P							
Manually determined peaks	nan							
[P]₀ to programmatically determine peak	0.001							

Section 9: ACTIS-ICP-MS measurements



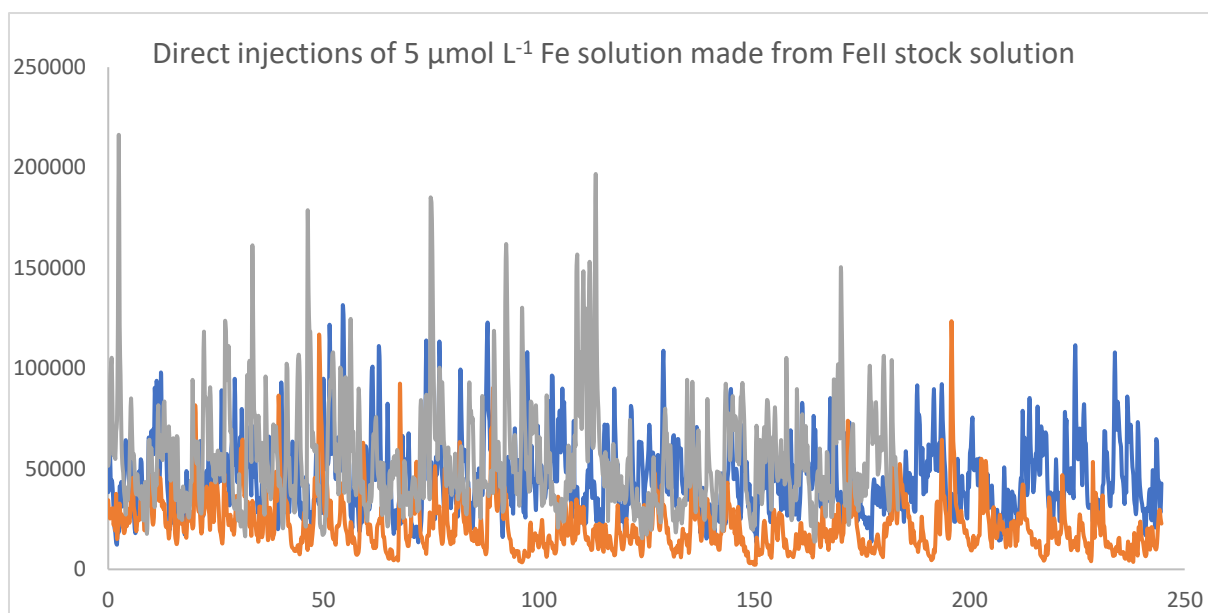
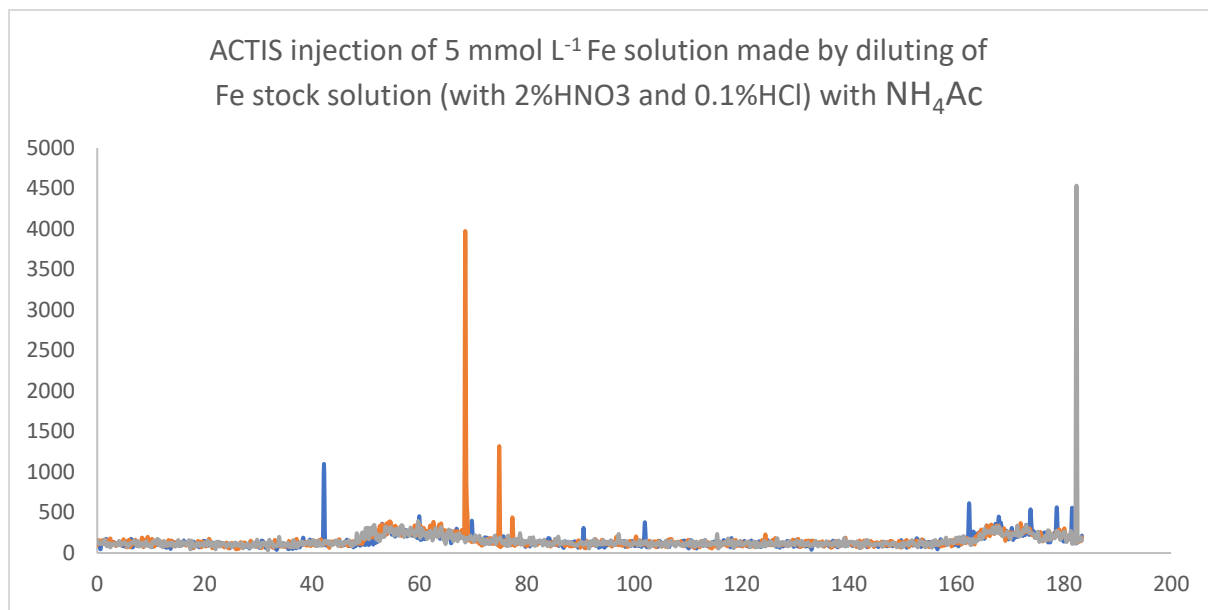
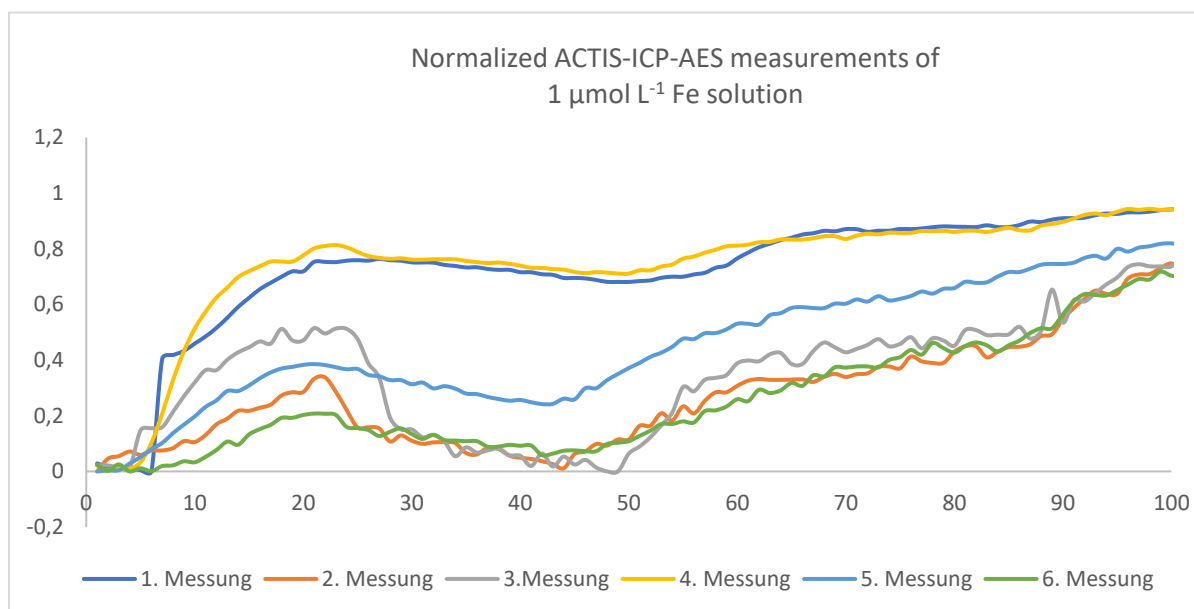
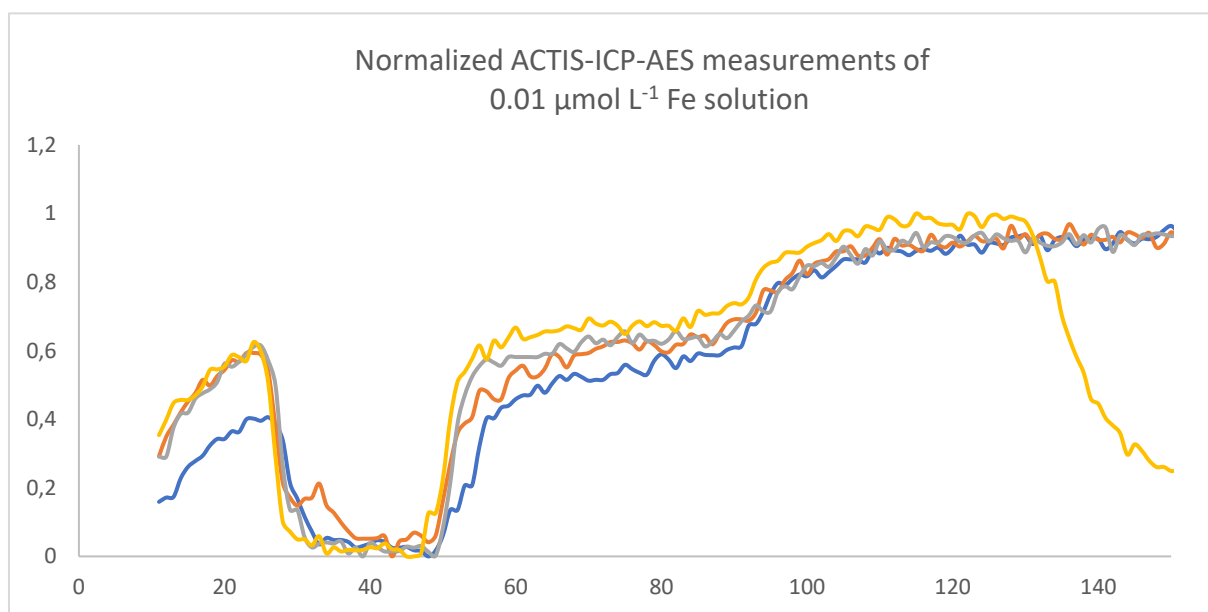


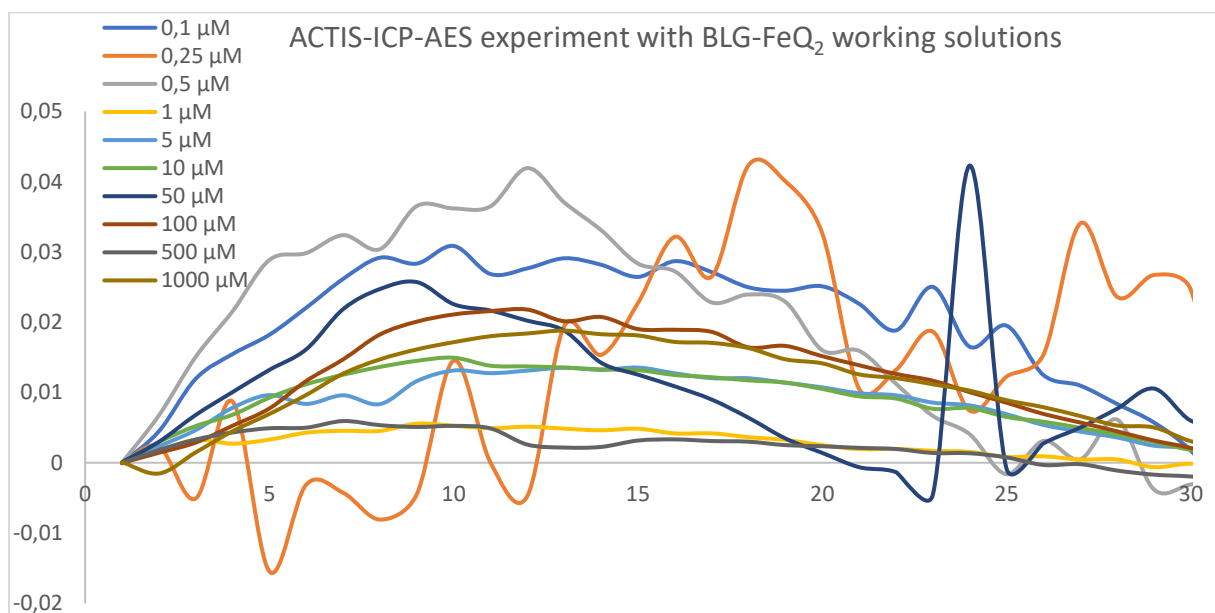
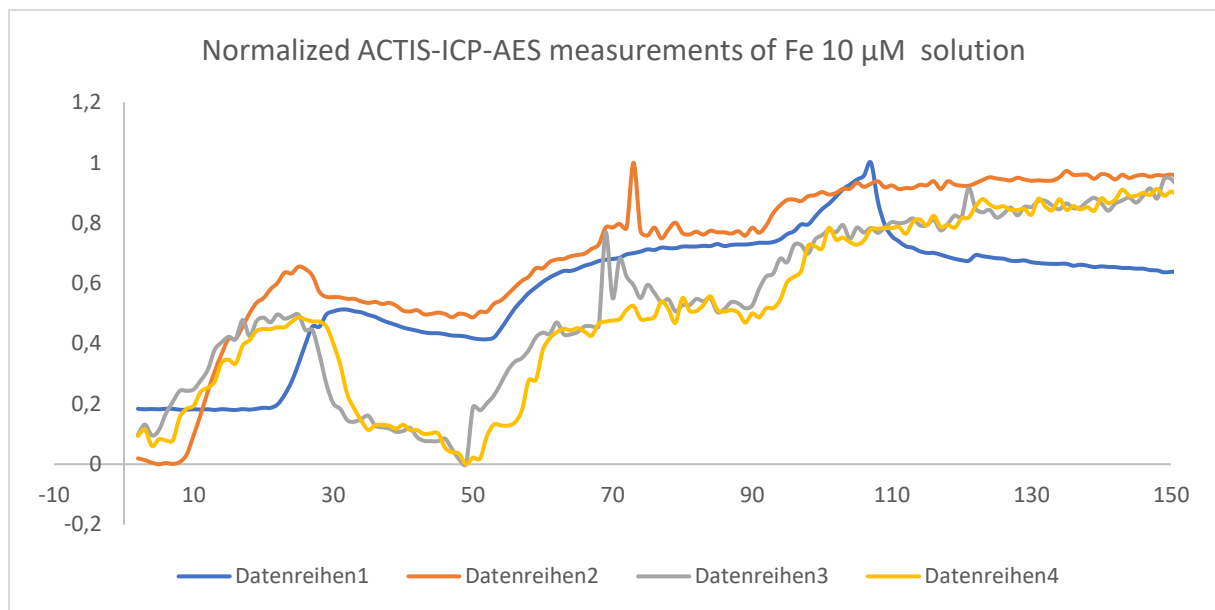
Table 18: Samples, injection methods, corresponding Std. dev, and noise level in ACTIS-ICP-MS measurements

Sample and injection method	Standard deviation	Noise level
direct injections of NH ₄ Ac solution	73.8	258.4
NH ₄ Ac injections through ACTIS	97.6	341.6
direct injections of 5 μM Fe made from Fe II stock solution	23968.4	81492.6
direct injections of 5 μM Fe made from stock solution in subb. H ₂ O with 2% HNO ₃ and 0.1 % HCl	376.0	1278.3
ACTIS injections of 5 μM Fe made from stock solution in subb, H ₂ O with 2% HNO ₃ and 0,1 % HCl (diluted with NH ₄ Ac)	127.7	447.2
ACTIS injections of 5 μM Fe made from stock solution in subb, H ₂ O with 2% HNO ₃ and 0,1 % HCl (diluted with subb, H ₂ O)	291.4	1019.9



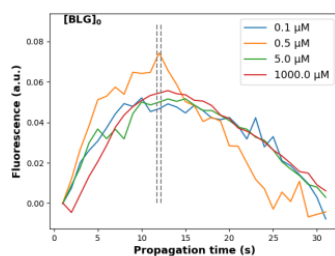
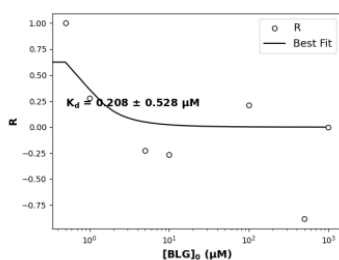
Section 10: ACTIS-ICP-AES measurements





[BLG]₀

BLG-FeQ2 prACTISed evaluation - without 0.25 and 50 μM



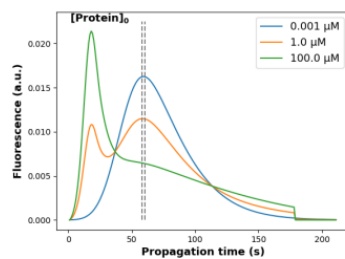
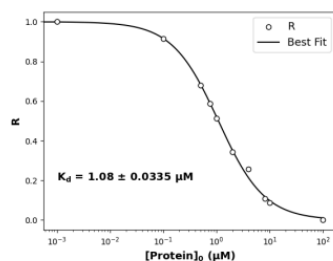
Propagation flow rate	68
Injection flow rate	0
Injection time (s)	0
Separation capillary length	60
Separation capillary diameter	127
Injection loop length	13
Injection loop diameter	50
Protein name	BLG
Ligand name	FeQ2
Number of Concentrations	8
Initial Ligand concentration [L]0 (μM)	1
Type of Data	F
Compensation procedure	N
[P]0 reference for MS normalization (μM)	nan
Window width (%)	2
Determination of peak	P
Manually determined peaks	nan
[P]0 to programmatically determine peak	0.5

Conc	Avg Sig (S)	S Std Dev	S Rel Std Dev	R value	R Std Dev	R Rel Std Dev
0.1 μM	0.04670018	0	0	nan	nan	nan
0.5 μM	0.07432935	0	0	1	0	0
1.0 μM	0.06004597	0	0	0.2807535	0	0
5.0 μM	0.04999841	0	0	-0.225196	0	0
10.0 μM	0.04921969	0	0	-0.264408	0	0
100.0 μM	0.05863858	0	0	0.209884	0	0
500.0 μM	0.0369122	0	0	-0.884158	0	0
1000.0 μM	0.05447053	0	0	0	0	0

$K_d: 0.2080 \pm 0.5279 \mu\text{M}$
$R^2: 0.4412$
$\chi^2: 1904.3568$

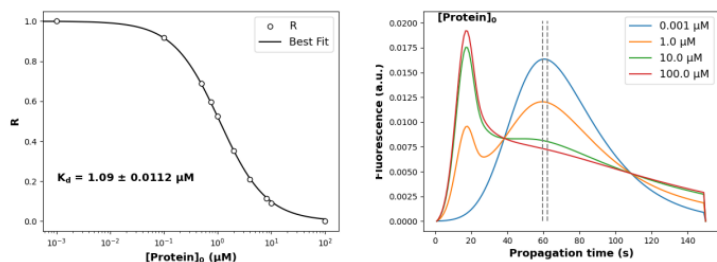
Section 12: Computer simulations results

50 μm



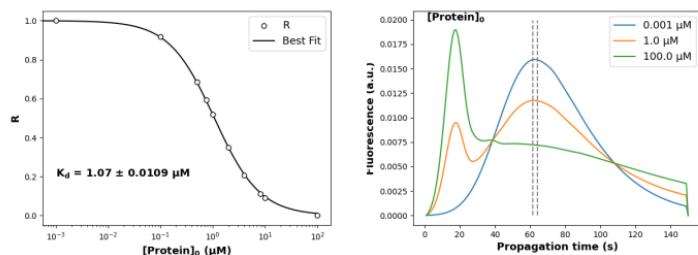
Propagation flow rate	68	Conc	Avg Sig (S)	S Std Dev	S Rel Std Dev	R value	R Std Dev	R Rel Std Dev
Injection flow rate	0	0.001 μM	0.01624896	0	0	1	0	0
Injection time (s)	0	0.1 μM	0.01541895	0	0	0.9153952	0	0
Separation capillary length	60	0.5 μM	0.01311756	0	0	0.6808096	0	0
Separation capillary diameter	127	0.75 μM	0.01218852	0	0	0.5861105	0	0
Injection loop length	13	1.0 μM	0.01148269	0	0	0.514163	0	0
Injection loop diameter	50	2.0 μM	0.009806103	0	0	0.3432647	0	0
Protein name	Protein	4.0 μM	0.008952563	0	0	0.2562613	0	0
Ligand name	Compound	8.0 μM	0.007508028	0	0	0.1090165	0	0
Number of Concentrations	10	10.0 μM	0.00729567	0	0	0.08737033	0	0
Initial Ligand concentration $[L]_0 (\mu\text{M})$	0.01	100.0 μM	0.00643853	0	0	0	0	0
Type of Data	F							
Compensation procedure	N	Kd: 1.0783 $\pm$ 0.0335 μM						
$[P]_0$ reference for MS normalization (μM)	nan	R ² : 0.9979						
Window width (%)	2	Chi ² : 0.0218						
Determination of peak	P							
Manually determined peaks	nan							
$[P]_0$ to programmatically determine peak	0.001							

100 μm



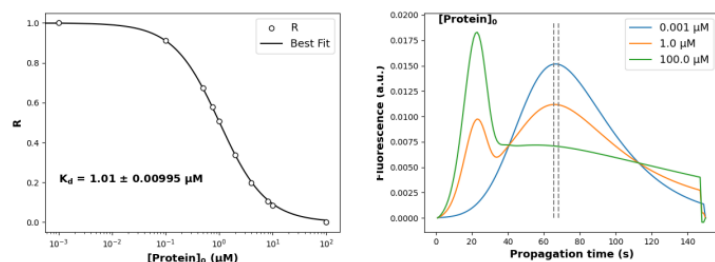
Propagation flow rate	68	Conc	Avg Sig (S)	S Std Dev	S Rel Std Dev	R value	R Std Dev	R Rel Std Dev
Injection flow rate	0	0.001 μM	0.01633113	0	0	1	0	0
Injection time (s)	0	0.1 μM	0.01559172	0	0	0.9183847	0	0
Separation capillary length	60	0.5 μM	0.01351606	0	0	0.6892746	0	0
Separation capillary diameter	127	0.75 μM	0.01266736	0	0	0.5955951	0	0
Injection loop length	13	1.0 μM	0.01201834	0	0	0.5239572	0	0
Injection loop diameter	50	2.0 μM	0.01046195	0	0	0.3521632	0	0
Protein name	Protein	4.0 μM	0.009174066	0	0	0.2100075	0	0
Ligand name	Compound	8.0 μM	0.008294181	0	0	0.1128863	0	0
Number of Concentrations	10	10.0 μM	0.008091821	0	0	0.09054988	0	0
Initial Ligand concentration $[\text{L}]_0$ (μM)	0.01	100.0 μM	0.00727147	0	0	0	0	0
Type of Data	F	Kd: $1.0852 \pm 0.0112 \mu\text{M}$ R²: 0.9998 Chi²: 0.0118						
Compensation procedure	N							
[P] ₀ reference for MS normalization (μM)	nan							
Window width (%)	2							
Determination of peak	P							
Manually determined peaks	nan							
[P] ₀ to programmatically determine peak	0.001							

150 μm



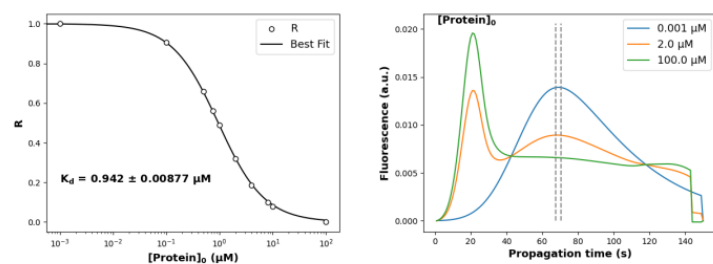
Propagation flow rate	68	Conc	Avg Sig (S)	S Std Dev	S Rel Std Dev	R value	R Std Dev	R Rel Std Dev
Injection flow rate	0	0.001 μM	0.01592857	0	0	1	0	0
Injection time (s)	0	0.1 μM	0.01520697	0	0	0.9172642	0	0
Separation capillary length	60	0.5 μM	0.0131907	0	0	0.6860838	0	0
Separation capillary diameter	127	0.75 μM	0.01237024	0	0	0.5920118	0	0
Injection loop length	13	1.0 μM	0.01174436	0	0	0.5202505	0	0
Injection loop diameter	50	2.0 μM	0.01024887	0	0	0.3487813	0	0
Protein name	Protein	4.0 μM	0.009017134	0	0	0.2075534	0	0
Ligand name	Compound	8.0 μM	0.008178581	0	0	0.1114071	0	0
Number of Concentrations	10	10.0 μM	0.007986067	0	0	0.08933389	0	0
Initial Ligand concentration $[\text{L}]_0$ (μM)	0.01	100.0 μM	0.007206929	0	0	0	0	0
Type of Data	F	Kd: $1.0694 \pm 0.0109 \mu\text{M}$ R²: 0.9998 Chi²: 0.0116						
Compensation procedure	N							
[P] ₀ reference for MS normalization (μM)	nan							
Window width (%)	2							
Determination of peak	P							
Manually determined peaks	nan							
[P] ₀ to programmatically determine peak	0.001							

250 μm



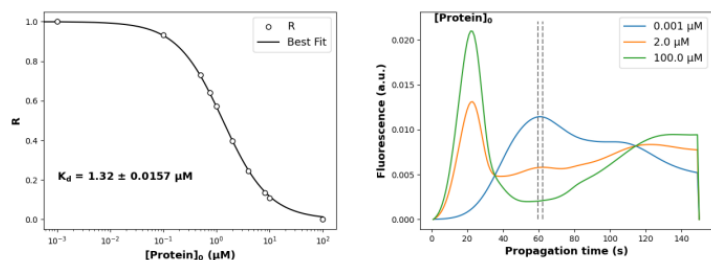
Propagation flow rate	68	Conc	Avg Sig (S)	S Std Dev	S Rel Std Dev	R value	R Std Dev	R Rel Std Dev
Injection flow rate	0	0.001 μM	0.01516081	0	0	1	0	0
Injection time (s)	0	0.1 μM	0.0144576	0	0	0.9130663	0	0
Separation capillary length	60	0.5 μM	0.01252638	0	0	0.6743207	0	0
Separation capillary diameter	127	0.75 μM	0.01175442	0	0	0.5788873	0	0
Injection loop length	13	1.0 μM	0.01117082	0	0	0.5067409	0	0
Injection loop diameter	50	2.0 μM	0.009794551	0	0	0.3366003	0	0
Protein name	Protein	4.0 μM	0.008679873	0	0	0.198799	0	0
Ligand name	Compound	8.0 μM	0.007930552	0	0	0.1061648	0	0
Number of Concentrations	10	10.0 μM	0.007759599	0	0	0.08503083	0	0
Initial Ligand concentration [L]₀ (μM)	0.01	100.0 μM	0.007071783	0	0	0	0	0
Type of Data	F	Kd: 1.0138 $\pm$ 0.0100 μM						
Compensation procedure	N	R²: 0.9998						
[P]₀ reference for MS normalization (μM)	nan	Chi²: 0.0111						
Window width (%)	2							
Determination of peak	P							
Manually determined peaks	nan							
[P]₀ to programmatically determine peak	0.001							

300 μm



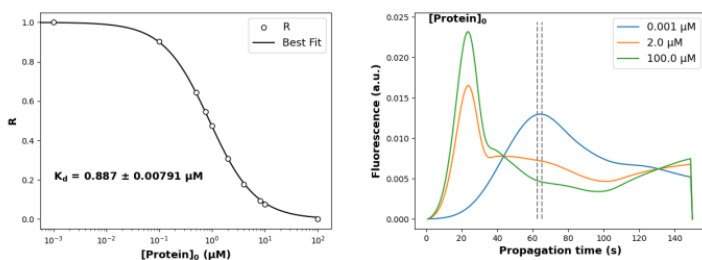
Propagation flow rate	68	Conc	Avg Sig (S)	S Std Dev	S Rel Std Dev	R value	R Std Dev	R Rel Std Dev
Injection flow rate	0	0.001 μM	0.01391486	0	0	1	0	0
Injection time (s)	0	0.1 μM	0.01323294	0	0	0.9069609	0	0
Separation capillary length	60	0.5 μM	0.01140622	0	0	0.6577334	0	0
Separation capillary diameter	127	0.75 μM	0.01069433	0	0	0.5606065	0	0
Injection loop length	13	1.0 μM	0.01016288	0	0	0.4880977	0	0
Injection loop diameter	50	2.0 μM	0.00893194	0	0	0.3201539	0	0
Protein name	Protein	4.0 μM	0.007957353	0	0	0.1871858	0	0
Ligand name	Compound	8.0 μM	0.007313138	0	0	0.09929234	0	0
Number of Concentrations	10	10.0 μM	0.007167374	0	0	0.07940494	0	0
Initial Ligand concentration [L]₀ (μM)	0.01	100.0 μM	0.006585376	0	0	0	0	0
Type of Data	F	Kd: 0.9417 $\pm$ 0.0088 μM						
Compensation procedure	N	R²: 0.9998						
[P]₀ reference for MS normalization (μM)	nan	Chi²: 0.0103						
Window width (%)	2							
Determination of peak	P							
Manually determined peaks	nan							
[P]₀ to programmatically determine peak	0.001							

500 μm



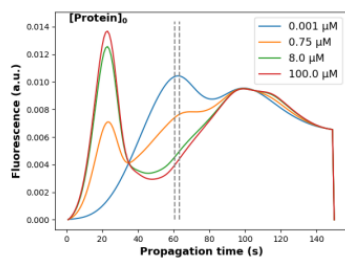
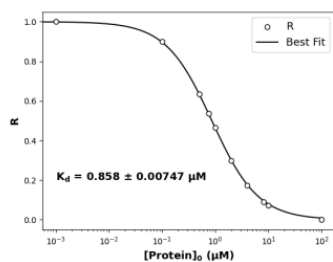
Propagation flow rate	68	Conc	Avg Sig (S)	S Std Dev	S Rel Std Dev	R value	R Std Dev	R Rel Std Dev
Injection flow rate	0	0.001 μM	0.0114304	0	0	1	0	0
Injection time (s)	0	0.1 μM	0.01079336	0	0	0.9319456	0	0
Separation capillary length	60	0.5 μM	0.008900153	0	0	0.7296992	0	0
Separation capillary diameter	127	0.75 μM	0.008078041	0	0	0.641875	0	0
Injection loop length	13	1.0 μM	0.007429114	0	0	0.5725517	0	0
Injection loop diameter	50	2.0 μM	0.005796568	0	0	0.3981506	0	0
Protein name	Protein	4.0 μM	0.004357662	0	0	0.2444356	0	0
Ligand name	Compound	8.0 μM	0.003324779	0	0	0.1340952	0	0
Number of Concentrations	10	10.0 μM	0.003081193	0	0	0.1080735	0	0
Initial Ligand concentration $[L]_0$ (μM)	0.01	100.0 μM	0.002069531	0	0	0	0	0
Type of Data	F							
Compensation procedure	N	Kd: 1.3168 $\pm$ 0.0157 μM						
[P]0 reference for MS normalization (μM)	nan	R ² : 0.9997						
Window width (%)	2	Chi ² : 0.0141						
Determination of peak	P							
Manually determined peaks	nan							
[P]0 to programmatically determine peak	0.001							

750 μm



Propagation flow rate	68	Conc	Avg Sig (S)	S Std Dev	S Rel Std Dev	R value	R Std Dev	R Rel Std Dev
Injection flow rate	0	0.001 μM	0.01296747	0	0	1	0	0
Injection time (s)	0	0.1 μM	0.0121512	0	0	0.9017272	0	0
Separation capillary length	60	0.5 μM	0.01001032	0	0	0.6439833	0	0
Separation capillary diameter	127	0.75 μM	0.009193535	0	0	0.5456499	0	0
Injection loop length	13	1.0 μM	0.008590032	0	0	0.4729932	0	0
Injection loop diameter	50	2.0 μM	0.007212319	0	0	0.3071283	0	0
Protein name	Protein	4.0 μM	0.006141015	0	0	0.1781525	0	0
Ligand name	Compound	8.0 μM	0.005442108	0	0	0.09401002	0	0
Number of Concentrations	10	10.0 μM	0.005284974	0	0	0.07509242	0	0
Initial Ligand concentration $[L]_0$ (μM)	0.01	100.0 μM	0.004661239	0	0	0	0	0
Type of Data	F							
Compensation procedure	N	Kd: 0.8870 $\pm$ 0.0079 μM						
[P]0 reference for MS normalization (μM)	nan	R ² : 0.9998						
Window width (%)	2	Chi ² : 0.0098						
Determination of peak	P							
Manually determined peaks	nan							
[P]0 to programmatically determine peak	0.001							

1000 μm

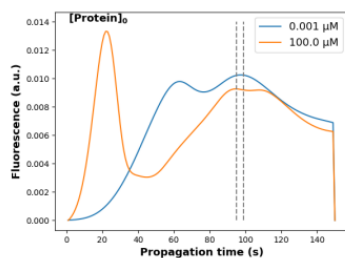
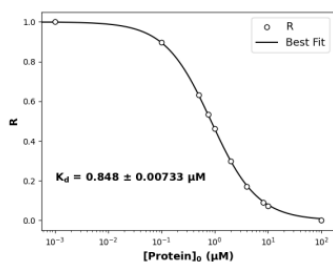


Propagation flow rate	68
Injection flow rate	0
Injection time (s)	0
Separation capillary length	60
Separation capillary diameter	127
Injection loop length	13
Injection loop diameter	50
Protein name	Protein
Ligand name	Compound
Number of Concentrations	10
Initial Ligand concentration [L]₀ (μM)	0.01
Type of Data	F
Compensation procedure	N
[P]₀ reference for MS normalization (μM)	nan
Window width (%)	2
Determination of peak	P
Manually determined peaks	nan
[P]₀ to programmatically determine peak	0.001

Conc	Avg Sig (S)	S Std Dev	S Rel Std Dev	R value	R Std Dev	R Rel Std Dev
0.001 μM	0.01042128	0	0	1	0	0
0.1 μM	0.009790658	0	0	0.8986847	0	0
0.5 μM	0.00815674	0	0	0.6361807	0	0
0.75 μM	0.007540904	0	0	0.5372409	0	0
1.0 μM	0.007088507	0	0	0.464559	0	0
2.0 μM	0.006064036	0	0	0.2999683	0	0
4.0 μM	0.005275281	0	0	0.1732474	0	0
8.0 μM	0.004764369	0	0	0.09116467	0	0
10.0 μM	0.004649897	0	0	0.07277364	0	0
100.0 μM	0.004196928	0	0	0	0	0

$K_d: 0.8577 \pm 0.0075 \mu\text{M}$
$R^2: 0.9998$
$\chi^2: 0.0095$

1250 μm



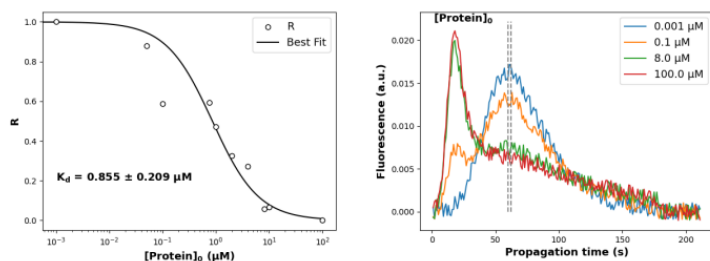
Propagation flow rate	68
Injection flow rate	0
Injection time (s)	0
Separation capillary length	60
Separation capillary diameter	127
Injection loop length	13
Injection loop diameter	50
Protein name	Protein
Ligand name	Compound
Number of Concentrations	10
Initial Ligand concentration [L]₀ (μM)	0.01
Type of Data	F
Compensation procedure	N
[P]₀ reference for MS normalization (μM)	nan
Window width (%)	2
Determination of peak	P
Manually determined peaks	nan
[P]₀ to programmatically determine peak	0.001

Conc	Avg Sig (S)	S Std Dev	S Rel Std Dev	R value	R Std Dev	R Rel Std Dev
0.001 μM	0.01024882	0	0	1	0	0
0.1 μM	0.01014512	0	0	0.8976748	0	0
0.5 μM	0.009877522	0	0	0.6336207	0	0
0.75 μM	0.009777065	0	0	0.5344941	0	0
1.0 μM	0.009703408	0	0	0.461813	0	0
2.0 μM	0.009537047	0	0	0.2976544	0	0
4.0 μM	0.009409374	0	0	0.1716713	0	0
8.0 μM	0.009326864	0	0	0.09025378	0	0
10.0 μM	0.009308397	0	0	0.07203194	0	0
100.0 μM	0.009235399	0	0	0	0	0

$K_d: 0.8484 \pm 0.0073 \mu\text{M}$
$R^2: 0.9998$
$\chi^2: 0.0094$

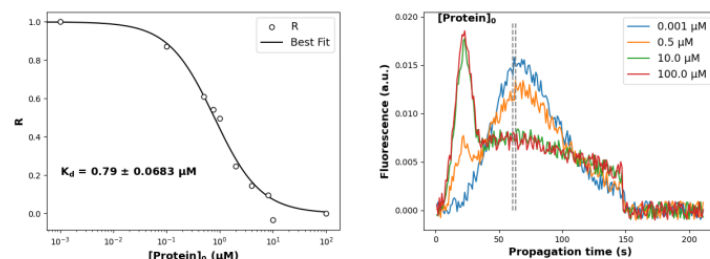
Section 12: Computer simulations with added noise

50 μm with noise



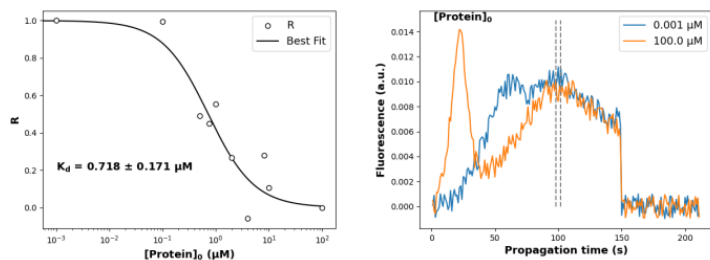
Propagation flow rate	68	Conc	Avg Sig (S)	S Std Dev	S Rel Std Dev	R value	R Std Dev	R Rel Std Dev
Injection flow rate	0	0.001 μM	0.01665028	0	0	1	0	0
Injection time (s)	0	0.05 μM	0.01538978	0	0	0.878497	0	0
Separation capillary length	60	0.1 μM	0.01237602	0	0	0.5879912	0	0
Separation capillary diameter	127	0.75 μM	0.01243601	0	0	0.5937741	0	0
Injection loop length	13	1.0 μM	0.01117995	0	0	0.4726988	0	0
Injection loop diameter	50	2.0 μM	0.00964154	0	0	0.3244067	0	0
Protein name	Protein	4.0 μM	0.009091877	0	0	0.271423	0	0
Ligand name	Compound	8.0 μM	0.006867206	0	0	0.0569804	0	0
Number of Concentrations	10	10.0 μM	0.006954099	0	0	0.0653563	0	0
Initial Ligand concentration $[L]_0$ (μM)	0.01	100.0 μM	0.00627608	0	0	0	0	0
Type of Data	F							
Compensation procedure	N	Kd: $0.8545 \pm 0.2093 \mu\text{M}$						
[P]₀ reference for MS normalization (μM)	nan	R²: 0.8932						
Window width (%)	2	Chi²: 0.1979						
Determination of peak	P							
Manually determined peaks	nan							
[P]₀ to programmatically determine peak	0.001							

250 μm ideal inputs - norm-short - noise



Propagation flow rate	68	Conc	Avg Sig (S)	S Std Dev	S Rel Std Dev	R value	R Std Dev	R Rel Std Dev
Injection flow rate	0	0.001 μM	0.01487314	0	0	1	0	0
Injection time (s)	0	0.1 μM	0.01394203	0	0	0.8725359	0	0
Separation capillary length	60	0.5 μM	0.01203475	0	0	0.6114401	0	0
Separation capillary diameter	127	0.75 μM	0.01152612	0	0	0.5418116	0	0
Injection loop length	13	1.0 μM	0.01118683	0	0	0.4953636	0	0
Injection loop diameter	50	2.0 μM	0.009365725	0	0	0.2460643	0	0
Protein name	Protein	4.0 μM	0.008619732	0	0	0.1439418	0	0
Ligand name	Compound	8.0 μM	0.008270943	0	0	0.09619445	0	0
Number of Concentrations	10	10.0 μM	0.007314457	0	0	-0.0347435	0	0
Initial Ligand concentration $[L]_0$ (μM)	0.01	100.0 μM	0.007568254	0	0	0	0	0
Type of Data	F							
Compensation procedure	N	Kd: $0.7899 \pm 0.0683 \mu\text{M}$						
[P]₀ reference for MS normalization (μM)	nan	R²: 0.9853						
Window width (%)	2	Chi²: 0.1833						
Determination of peak	P							
Manually determined peaks	nan							
[P]₀ to programmatically determine peak	0.001							

1250 μm with noise



Propagation flow rate	68	Conc	Avg Sig (S)	S Std Dev	S Rel Std Dev	R value	R Std Dev	R Rel Std Dev
Injection flow rate	0	0.001 μM	0.01024514	0	0	1	0	0
Injection time (s)	0	0.1 μM	0.01024131	0	0	0.9964631	0	0
Separation capillary length	60	0.5 μM	0.009692681	0	0	0.4895824	0	0
Separation capillary diameter	127	0.75 μM	0.009647809	0	0	0.4481248	0	0
Injection loop length	13	1.0 μM	0.009760439	0	0	0.552185	0	0
Injection loop diameter	50	2.0 μM	0.009451454	0	0	0.2667109	0	0
Protein name	Protein	4.0 μM	0.009098316	0	0	-0.05955647	0	0
Ligand name	Compound	8.0 μM	0.009466579	0	0	0.2806852	0	0
Number of Concentrations	10	10.0 μM	0.009278086	0	0	0.1065347	0	0
Initial Ligand concentration [L]₀ (μM)	0.01	100.0 μM	0.009162778	0	0	0	0	0
Type of Data	F	Kd: 0.7176 $\pm$ 0.1708 μM						
Compensation procedure	N	R²: 0.8954						
[P]₀ reference for MS normalization (μM)	nan	Chi²: 0.8814						
Window width (%)	2							
Determination of peak	P							
Manually determined peaks	nan							
[P]₀ to programmatically determine peak	0.001							

Table 19: K_d values and corresponding standard deviations (all values given in $\mu\text{mol L}^{-1}$) resulted in evaluation of separagrams with and without noise added. Simulated K_d was set to $1 \mu\text{mol L}^{-1}$.

Transfer capillary	Without noise		With noise	
inner diameter	K_d	Std. dev.	K_d	Std. dev.
50 μm	1.0783	0.0335	0.8545	0.2093
250 μm	1.0138	0.0100	0.7899	0.0683
1250 μm	0.8484	0.0073	0.7176	0.1708